TECHNICAL REPORT

IEC TR 60788

Second edition
2004-02

Medical electrical equipment –

Glossary of defined terms

Reference number
IEC/TR 60788:2004(E)

Publication numbering

As from 1 January 1997 all IEC publications are issued with a designation in the 60000 series. For example, IEC 34-1 is now referred to as IEC 60034-1.

Consolidated editions

The IEC is now publishing consolidated versions of its publications. For example, edition numbers 1.0, 1.1 and 1.2 refer, respectively, to the base publication, the base publication incorporating amendment 1 and the base publication incorporating amendments 1 and 2.

Further information on IEC publications

The technical content of IEC publications is kept under constant review by the IEC, thus ensuring that the content reflects current technology. Information relating to this publication, including its validity, is available in the IEC Catalogue of publications (see below) in addition to new editions, amendments and corrigenda. Information on the subjects under consideration and work in progress undertaken by the technical committee which has prepared this publication, as well as the list of publications issued, is also available from the following:

- **IEC Web Site (www.iec.ch)**

- **Catalogue of IEC publications**

  The on-line catalogue on the IEC web site (www.iec.ch/searchpub) enables you to search by a variety of criteria including text searches, technical committees and date of publication. On-line information is also available on recently issued publications, withdrawn and replaced publications, as well as corrigenda.

- **IEC Just Published**

  This summary of recently issued publications (www.iec.ch/online_news/ justpub) is also available by email. Please contact the Customer Service Centre (see below) for further information.

- **Customer Service Centre**

  If you have any questions regarding this publication or need further assistance, please contact the Customer Service Centre:

  Email: custserv@iec.ch
  Tel: +41 22 919 02 11
  Fax: +41 22 919 03 00

TECHNICAL REPORT

IEC TR 60788

Second edition
2004-02

Medical electrical equipment –

Glossary of defined terms

International Electrotechnical Commission, 3, rue de Varembé, PO Box 131, CH-1211 Geneva 20, Switzerland
Telephone: +41 22 919 02 11 Telefax: +41 22 919 03 00 E-mail: inmail@iec.ch Web: www.iec.ch

Commission Electrotechnique Internationale
International Electrotechnical Commission
Международная Электротехническая Комиссия

PRICE CODE XH

For price, see current catalogue

INTERNATIONAL ELECTROTECHNICAL COMMISSION

MEDICAL ELECTRICAL EQUIPMENT – GLOSSARY OF DEFINED TERMS

FOREWORD

1) The International Electrotechnical Commission (IEC) is a worldwide organization for standardization comprising all national electrotechnical committees (IEC National Committees). The object of IEC is to promote international co-operation on all questions concerning standardization in the electrical and electronic fields. To this end and in addition to other activities, IEC publishes International Standards, Technical Specifications, Technical Reports, Publicly Available Specifications (PAS) and Guides (hereafter referred to as "IEC Publication(s)"). Their preparation is entrusted to technical committees; any IEC National Committee interested in the subject dealt with may participate in this preparatory work. International, governmental and non-governmental organizations liaising with the IEC also participate in this preparation. IEC collaborates closely with the International Organization for Standardization (ISO) in accordance with conditions determined by agreement between the two organizations.
2) The formal decisions or agreements of IEC on technical matters express, as nearly as possible, an international consensus of opinion on the relevant subjects since each technical committee has representation from all interested IEC National Committees.
3) IEC Publications have the form of recommendations for international use and are accepted by IEC National Committees in that sense. While all reasonable efforts are made to ensure that the technical content of IEC Publications is accurate, IEC cannot be held responsible for the way in which they are used or for any misinterpretation by any end user.
4) In order to promote international uniformity, IEC National Committees undertake to apply IEC Publications transparently to the maximum extent possible in their national and regional publications. Any divergence between any IEC Publication and the corresponding national or regional publication shall be clearly indicated in the latter.
5) IEC provides no marking procedure to indicate its approval and cannot be rendered responsible for any EQUIPMENT declared to be in conformity with an IEC Publication.
6) All users should ensure that they have the latest edition of this publication.
7) No liability shall attach to IEC or its directors, employees, servants or agents including individual experts and members of its technical committees and IEC National Committees for any personal injury, property damage or other damage of any nature whatsoever, whether direct or indirect, or for costs (including legal fees) and expenses arising out of the publication, use of, or reliance upon, this IEC Publication or any other IEC Publications.
8) Attention is drawn to the Normative references cited in this publication. Use of the referenced publications is indispensable for the correct application of this publication.
9) Attention is drawn to the possibility that some of the elements of this IEC Publication may be the subject of patent rights. IEC shall not be held responsible for identifying any or all such patent rights.

The main task of IEC technical committees is to prepare International Standards. However, a technical committee may propose the publication of a technical report when it has collected data of a different kind from that which is normally published as an International Standard, for example "state of the art".

IEC 60788, which is a technical report, has been prepared by IEC TC 62: Electrical EQUIPMENT in medical practice.

This second edition cancels and replaces the first edition of IEC 60788 published in 1984. This second edition constitutes a technical revision.

The text of this technical report is based on the following documents:

Enquiry draft	Report on voting
62/137/DTR	62/140/RVC

Full information on the voting for the approval of this technical report can be found in the report on voting indicated in the above table.

This publication does not follow the rules for structuring International Standards as given in Part 2 of the ISO/IEC Directives.

The committee has decided that the contents of this publication will remain unchanged until 2005. At this date, the publication will be

- reconfirmed;
- withdrawn;
- replaced by a revised edition, or
- amended.

INTRODUCTION

Purpose

– To provide an actual mirror of defined terms for all steps in the development of IEC standards under the scope of "MEDICAL ELECTRICAL EQUIPMENT", IEC TC 62.

– To give guidance for harmonisation of the defined terms used in the IEC standards on "MEDICAL ELECTRICAL EQUIPMENT".

Contents

– All DEFINED TERMS used in the General, Particular and Collateral Standards recorded in the project files of the IEC for TC 62, SC 62A, 62B, 62C and 62D are mirrored.

– Recommendations to avoid existing redundancy are added as red text in the column "Definitions" in the table.

Maintenance

– An annual maintenance cycle for this TR is introduced. Closing date for the editorial input is the middle of December of a year.

– The annual editorial maintenance is done by the Secretaries of the IEC technical committee 62 and its subcommittees 62A, 62B, 62C and 62D.

– The compilation (addition of new terms and deletion of obsolete terms) is done by the Secretary of IEC TC 62.

Targets

– Represent the state-of-the-art in the definitions

– Harmonize the language of the IEC publications

– Ease translations of the IEC publications

– Enable self-control by the experts working in projects for MEDICAL ELECTRICAL EQUIPMENT.

Coded reference of the DEFINED TERMS

– In all cases – as appropriate – the reference codes "IEV xxx-xx-xx" of the International Electronic Vocabulary (IEV) are added in the "Reference" column of the table.

– For DEFINED TERMS used in RADIOLOGY the reference codes "rm-xx-xx" remain unchanged as initiated by IEC 60788 Ed.1.

– For main fields other than RADIOLOGY, the coded references will be generated in future annual editions.

Replacement

This technical report replaces IEC 60788 Ed.1, *Medical radiology – Terminology*.

MEDICAL ELECTRICAL EQUIPMENT – GLOSSARY OF DEFINED TERMS

1 Scope

This Technical report comprises all defined terms used in the IEC standards and technical reports which

– fall under the scope of MEDICAL ELECTRICAL EQUIPMENT, and
– are on the list of publications as stated in May 2003.

2 Normative references

The documents referenced in 2.2 are forming the sources for the defined terms in this document.

2.1 General

The defined terms listed in this glossary are mirrored as presented in the standards and technical reports. Only the recommendations are added for further harmonisation of multiple defined terms.

The glossary is prepared to ease the use of the electronic version by two search functions:

– Search in the alphabetic order, and
– Search by the technical and physical chapters in case of ionising radiation (rm-xx-xx).

2.2 List of the IEC publications mirrored in this edition 2004

The list of IEC Standards below comprises the defined terms as used in the latest consolidated version, comprising the amendments as applicable.

1	60336	1993-07
2	60522	1999-02
3	60526	1978-01
4	60580	2000-01
5	60601-1/A1+ A2	1988-12/ 1991-11/ 1995-03
6	60601-1-2	2001-09
7	60601-1-3	1994-07
8	60601-1-4 Ed.1.1	2000-04
9	60601-2-1 /A1	1998-06/ 2002-05
10	60601-2-2	1998-09
11	60601-2-3/A1	1991-06/ 1998-09
12	60601-2-4	2002-08
13	60601-2-5	2000-07
14	60601-2-6	1984-01
15	60601-2-7	1998-02
16	60601-2-8 Ed.1.1	1999-04
17	60601-2-9	1996-10
18	60601-2-10/A1	1987-12/ 2001-09
19	60601-2-11	1997-08
20	60601-2-12	2001-10
21	60601-2-13	2003-05
22	60601-2-16	1998-02
23	60601-2-17/A1	1989-09/ 1996-03
24	60601-2-18/A1	1996-08/ 2000-07
25	60601-2-19/A1	1990-12/ 1996-10
26	60601-2-20/A1	1990-12/ 1996-10
27	60601-2-21/A1	1994-02/ 1996-10
28	60601-2-23	1999-12
29	60601-2-24	1998-02
30	60601-2-25/A1	1993-03/ 1999-05
31	60601-2-26	2002-11
32	60601-2-27	1994-04
33	60601-2-28	1993-04
34	60601-2-29,	1999-01
35	60601-2-30	1999-12
36	60601-2-31/A1	1994-10/ 1998-01
37	60601-2-32	1994-03
38	60601-2-33	2002-05
39	60601-2-34	2000-10
40	60601-2-35	1996-11
41	60601-2-36	1997-03
42	60601-2-37	2001-07
43	60601-2-38/A1	1996-10/ 1999-12
44	60601-2-39	1999-06
45	60601-2-40	1998-02
46	60601-2-41	2000-02
47	60601-2-43	2000-06
48	60601-2-44 Ed.2.1	2002-11
49	60601-2-45	2001-05
50	60601-2-46	1998-06

51	60601-2-47	2001-07
52	60601-2-49	2001-07
53	60601-2-50	2000-07
54	60601-2-51	2003-02
55	60601-2-55	To be published
56	60601-3-1	1996-08
57	60613	1989-05
58	60627	2001-08
59	60731/A1	1997-07/ 2002-06
60	60789	1992-02
61	60806	1984-01
62	60976/A1	1989-06/ 2000-07
63	60977/A1	1989-10/ 2000-04
64	61168	1993-12
65	61170	1993-12
66	61217 Ed.1.1	2002-03
67	61223-1	1993-07
68	61223-2-1	1993-07
69	61223-2-4	1994-03
70	61223-2-5	1994-03
71	61223-2-6	1994-04
72	61223-2-7	1999-09
73	61223-2-9	1999-09
74	61223-2-10	1999-09
75	61223-2-11	1999-09
76	61223-3-1	1999-03
77	61223-3-2	1996-11
78	61223-3-3	1996-11
79	61223-3-4	2000-03
80	61262-1	1994-07
81	61262-2	1994-07
82	61262-3	1994-07
83	61262-4	1994-07
84	61262-5	1994-08
85	61262-6	1994-07
86	61262-7	1995-09
87	61267	1994-10
88	61303	1994-10
89	61331-1	1994-10
90	61331-2	1994-10
91	61331-3	1998-11
92	61674/A1	1997-10/ 2002-06
93	61675-1	1998-02
94	61675-2	1998-01
95	61675-3	1998-02
96	61676	2002-09
97	61852	1998-04
98	61859	1997-05
99	61948-1, TR	2001-02
100	61948-2, TR	2001-02
101	62083	2000-11
102	62266, TR	2002-03
103	ISO 14971	2000-11

Glossary of DEFINED TERMS used for MEDICAL ELECTRICAL EQUIPMENT – Edition 2004

Search...

...via chapters for imaging EQUIPMENT ***...by alphabetic index for all medical EQUIPMENT*** A B-C D E-F G-I K-M N-O P-Q R S T-V W-Z

Physics	General	Ionizing RADIATION	Interactions	Quantities, units and related concepts				
Generation and emission of ionizing RADIATION	General	HIGH VOLTAGE generators	X-RAY TUBE assemblies	PARTICLE ACCELERATORS	Beam therapy, RADIONUCLIDE sources	Therapy EQUIPMENT with SEALED RADIOACTIVE SOURCES		
RADIOLOGICAL EQUIPMENT using ionizing RADIATION	General	EQUIPMENT for medical diagnostics	Images: Reception, transfer, recording	EQUIPMENT for RADIOTHERAPY	EQUIPMENT for nuclear medicine	Accessories	Operation of EQUIPMENT	Geometry of RADIATION BEAM
Medical RADIOLOGICAL techniques	General	Diagnosis using beams	Therapy using beams	Nuclear medicine				
Dosimetry	General	RADIATION DETECTORS	PHANTOMS					
Protection against ionizing RADIATION	General	Limits and factors	Groups of persons	Areas	Means of protection			
Testing of RADIOLOGICAL EQUIPMENT	General	Test EQUIPMENT	VERIFICATION of characteristics	Concepts in mathematics, metrics, statistics	Obligation & statement of compliance			
Technology	General	Docu-mentation	EQUIPMENT	Operation of EQUIPMENT	Persons			
Magnetic resonance EQUIPMENT	General							
ULTRASOUND EQUIPMENT	General							

PHYSICS
General rm-10
RADIATION TYPE

PHYSICS
Ionizing RADIATION rm-11
DOSE PROFILE
EXTRA-FOCAL RADIATION
FOCAL RADIATION
INTRINSIC ENERGY RESOLUTION
INTRINSIC ENERGY SPECTRUM
IONIZING RADIATION
LEAKAGE RADIATION
MAXIMUM ENERGY
NEUTRON
PHOTON
PRIMARY RADIATION
RADIATION
RADIONUCLIDE
RESIDUAL RADIATION
SCATTERED RADIATION
STRAY RADIATION

PHYSICS
Interactions rm-12
ABSORPTION
BACK-SCATTERING
BUILD UP
FILTRATION
INDUCED RADIOACTIVITY
IRRADIATION
RADIOACTIVITY
TRANSMISSION

PHYSICS
Quantities, units and related concepts rm-13
ABSORBED DOSE
ABSORBED DOSE RATE
ABSORBED DOSE RATE TO WATER
ABSORBED DOSE TO WATER
ACTIVITY
ADDITIONAL FILTRATION
AIR KERMA
AIR KERMA LENGTH
AIR KERMA RATE
ATTENUATION
ATTENUATION COEFFICIENT
ATTENUATION EQUIVALENT
ATTENUATION RATIO
AUTOMATIC CONTROL SYSTEM
AUTOMATIC EXPOSURE CONTROL
AUTOMATIC EXPOSURE RATE CONTROL
AUTOMATIC INTENSITY CONTROL
BUILD UP FACTOR
DEPTH DOSE
DOSE AREA PRODUCT
DOSE AREA PRODUCT RATE
DOSE EQUIVALENT
DOSE MONITOR UNIT
ELECTRON
ENERGY FLUENCE RATE
ENERGY RESOLUTION
EXPOSURE
EXPOSURE RATE
HALF-VALUE LAYER
INHERENT FILTRATION
KERMA
KERMA RATE
LEAD EQUIVALENT
NOMINAL ENERGY
QUALITY EQUIVALENT FILTRATION
RADIATION SPECTRUM
RADIATION CONDITION
RADIATION ENERGY
RADIATION OUTPUT
RADIATION QUALITY
RADIATION QUANTITIES AND UNITS
RADIATION QUANTITY
RADIOACTIVE HALF-LIFE
RELATIVE SURFACE DOSE
RESPONSE
RESPONSE TIME
SENSITIVITY PROFILE
TENTH-VALUE LAYER
TOTAL FILTRATION
TRANSMISSION KERMA (TRANSMISSION KERMA RATE)
TRANSMISSION OF PRIMARY RADIATION
TRANSMISSION OF SCATTERED RADIATION
TRANSMISSION OF TOTAL RADIATION
TRANSMISSION RATIO
UNATTENUATED BEAM
UNATTENUATED BEAM QUALITY
UNIFORMITY
UNSCATTERED TRUE COINCIDENCE
VARIATION
VOXEL
WATER KERMA

GENENERATION & EMISSION OF IONIZING RADIATION
General rm-20
ACTUAL FOCAL SPOT
BLOOMING VALUE
CAPSULE
EFFECTIVE FOCAL SPOT
EXAMINATION ROOM
FOCAL SPOT
NOMINAL FOCAL SPOT VALUE
RADIATION HEAD
RADIATION SOURCE
RADIATION SOURCE ASSEMBLY
RADIOACTIVE SOURCE
RADIOACTIVE SOURCE TRAIN
RADIOLOGICAL EQUIPMENT
RADIOLOGICAL INSTALLATION
SEALED RADIOACTIVE SOURCE
TARGET
TARGET ANGLE
TREATMENT ROOM
X-RAY EQUIPMENT
X-RAY GENERATOR
X-RAY IMAGING ARRANGEMENT
X-RAY TUBE HEAD

GENENERATION & EMISSION OF IONIZING RADIATION
HIGH VOLTAGE generators rm-21
CAPACITOR DISCHARGE HIGH-VOLTAGE GENERATOR
CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR
HIGH-VOLTAGE CABLE CONNECTION
HIGH-VOLTAGE GENERATOR
HIGH-VOLTAGE TRANSFORMER ASSEMBLY
NOMINAL SHORTEST IRRADIATION TIME
ONE-PEAK HIGH-VOLTAGE GENERATOR
PRIMARY TIMER
PRIMARY/SECONDARY (TIMER) COMBINATION
RADIATION QUANTITY FOR NOMINAL SHORTEST IRRADIATION TIME
SIX-PEAK HIGH-VOLTAGE GENERATOR
TWO-PEAK HIGH VOLTAGE GENERATOR

GENENERATION & EMISSION OF IONIZING RADIATION
X-RAY TUBE assemblies rm-22
ANODE
ANODE ANGLE
CATHODE
FOCAL TRACK

MAXIMUM PEAK VOLTAGE
MEAN PEAK VOLTAGE
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE
PERMANENT FILTRATION
PRACTICAL PEAK POTENTIAL (PPP)
TUBE VOLTAGE (X-RAY)
TWELVE-PEAK HIGH VOLTAGE GENERATOR
X-RAY TUBE
X-RAY TUBE ASSEMBLY
X-RAY TUBE HOUSING

GENENERATION & EMISSION OF IONIZING RADIATION
PARTICLE ACCELERATORS rm-23
PARTICLE ACCELERATOR
PRACTICAL RANGE
QUANTITY INDEX

GENENERATION & EMISSION OF IONIZING RADIATION
Beam therapy, RADIONUCLIDE sources rm-24
DELINEATED LIGHT FIELD
DELINEATED RADIATION BEAM
DELINEATED RADIATION FIELD
DELINEATOR
RADIONUCLIDE BEAM THERAPY EQUIPMENT
SHUTTER
SOURCE CARRIER

GENENERATION & EMISSION OF IONIZING RADIATION
Therapy EQUIPMENT with SEALED RADIOACTIVE SOURCES rm-25
CHANNEL
SOURCE APPLICATOR
SOURCE DRIVE MECHANISM
STORAGE CONTAINER

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION
General rm-30
ASSOCIATED EQUIPMENT
GANTRY
IRRADIATION SWITCH
PATIENT SUPPORT
QUALITY ASSURANCE
QUALITY ASSURANCE PROGRAMME
REFERENCE AIR KERMA

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION EQUIPMENT for medical diagnosis rm-31
CASSETTE CHANGER
CT SCANNER
EFFECTIVE LENGTH
EFFECTIVE RANGE (OF INDICATED VALUES)
FILM CHANGER
INTERVENTIONAL X-RAY EQUIPMENT
POSITRON EMISSION TOMOGRAPH
RADIOSCOPICALLY GUIDED INTERVENTIONAL PROCEDURE
SERIAL CHANGER
SPEED INDEX
SPOTFILM DEVICE

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION
Reception, recording and transfer of images rm-32
ANTI-SCATTER GRID
ARTEFACT
AXIAL FIELD OF VIEW
AXIAL POINT SPREAD FUNCTION
AXIAL RESOLUTION
AXIAL SLICE WIDTH
BEST FOCUS
CENTRAL AXIS
CENTRAL LINE INDICATION
CENTRAL MAGNIFICATION
CENTRE OF THE ENTRANCE FIELD
CENTRE OF THE OUTPUT IMAGE
COINCIDENCE DETECTION
COINCIDENCE WINDOW
CONTRAST IMPROVEMENT RATIO
CONTRAST INDEX
CONTRAST RATIO (ABBREVIATION CR)
CONVERSION FACTOR
CROSS GRID
CT DETECTOR
CT DOSIMETER
DAS CONTRAST SENSITIVITY
DAS VISUAL SPATIAL RESOLUTION
DECENTRING OF A FOCUSED GRID
DEFOCUSING OF A FOCUSED GRID
DETECTIVE QUANTUM EFFICIENCY (ABBREVIATION DQE)
DETECTOR ASSEMBLY
DETECTOR FIELD OF VIEW (FOV)
DIFFERENTIAL RADIAL IMAGE DISTORTION
DIRECT RADIOGRAM
DOUBLE EMULSION FILM
DYNAMIC RANGE
EDGE FILTER
EFFECTIVE IMAGE RECEPTION AREA
ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER
ENTRANCE FIELD
ENTRANCE FIELD SIZE
ENTRANCE PLANE
FLUORESCENT SCREEN
FOCUSED GRID
FOCUSING DISTANCE
GRID EXPOSURE FACTOR
GRID RATIO
GRID SELECTIVITY
IMAGE DISTORTION
IMAGE MATRIX
IMAGE RECEPTOR PLANE IN X-RAY
IMAGE INTENSIFIER TUBES
INPUT SCREEN
INTEGRAL IMAGE DISTORTION
INTEGRAL MAGNIFICATION
INTENSIFYING SCREEN
INTERRUPTION
LINEAR GRID
LINEAR RANGE
LINEARITY
LINE PAIR RESOLUTION
LOCAL RADIAL MAGNIFICATION
LOW CONTRAST RESOLUTION
LOW-FREQUENCY DROP (LFD)
LUMINANCE DISTRIBUTION
LUMINANCE NON-UNIFORMITY
MAMMOGRAPHIC ANTI-SCATTER GRID
MATRIX ELEMENT
MEAN CT NUMBER
MOVING GRID
NET OPTICAL DENSITY
NOMINAL ENTRANCE FIELD SIZE
NOMINAL FOCAL SPOT VALUE
NOMINAL IMAGE SIZE
NOMINAL TOMOGRAPHIC SECTION THICKNESS
NOMINAL TOMOGRAPHIC SLICE THICKNESS
NON-SCREEN FILM
OBJECT SLICE
OBLIQUE CROSS GRID
ORTHOGONAL CROSS GRID
OUTPUT IMAGE
OUTPUT SCREEN
PARALLEL GRID

TRANSVERSE TOMOGRAPHY
TREATMENT FIELD
TREATMENT PARAMETER
TREATMENT PLAN/ TREATMENT PLANNING
TRUE COINCIDENCE
TRUE COUNT RATE
VOLUME SENSITIVITY
WELL-COUNTER
WELL-TYPE DETECTOR
WHOLE BODY COUNTER
WHOLE BODY IMAGING DEVICE

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION
Accessories rm-35

ADDED FILTER
BACK POINTER
BEAM SCATTERING FILTER
COMPRESSION DEVICE
CORE BIOPSY GUN
EFFECTIVE APERTURE
FIELD FLATTENING FILTER
FILTER
FRONT POINTER
IONIZING RADIATION SHIELD
MAMMOGRAPHIC STEREOTACTIC DEVICE
RADIOGRAM
TISSUE EQUIVALENT MATERIAL
WEDGE FILTER
ZERO FILTER

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION
Operation of EQUIPMENT rm-36

ANODE COOLING CURVE
ANODE HEAT CONTENT
ANODE HEATING CURVE
ANODE INPUT POWER
ANODE SPEED
APPARENT RESISTANCE OF SUPPLY MAINS
CATHODE EMISSION CHARACTERISTIC
CONTINUOUS MODE
CONTROLLED AREA
CT CONDITIONS OF OPERATION
CT PITCH FACTOR
CURRENT TIME PRODUCT
DECREASING INPUT POWER RATING
DEFAULT SETTING
EQUIVALENT ANODE INPUT POWER
FILAMENT CURRENT
INDIRECT RADIOGRAM
INITIAL X-RAY TUBE VOLTAGE
INITIATION
INTERMITTENT MODE
IRRADIATION TIME
LIMITED X-RAY TUBE VOLTAGE
LOADING
LOADING FACTOR
LOADING STATE
LOADING TIME
MAXIMUM ANODE HEAT CONTENT
MAXIMUM CONTINUOUS HEAT DISSIPATION
MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT
MODES OF OPERATION WITH CONTINUED DISPLAY
NOMINAL ANODE INPUT POWER
NOMINAL ELECTRIC POWER
NOMINAL X-RAY TUBE VOLTAGE
NON- ISOCENTRIC
OBJECT PROGRAMMED CONTROL
PERCENTAGE RIPPLE
PERCENTAGE RIPPLE IN CONSTANT
POTENTIAL HIGH-VOLTAGE GENERATORS
PRUDENT USE STATEMENT
RADIOGRAPHIC RATING
SERIAL LOAD RATING
SINGLE LOAD RATING
TREATMENT TIME
X-RAY TUBE ASSEMBLY COOLING CURVE
X-RAY TUBE ASSEMBLY HEAT CONTENT
X-RAY TUBE ASSEMBLY HEATING CURVE
X-RAY TUBE ASSEMBLY INPUT POWER
X-RAY TUBE CURRENT
X-RAY TUBE LOAD
X-RAY TUBE VOLTAGE

RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION
Geometry of RADIATION BEAM rm-37

BEAM APPLICATOR
BEAM LIMITING DEVICE
BEAM LIMITING SYSTEM
BOUNDARY AND DIMENSIONS OF THE X-RAY FIELD
BROAD BEAM
BROAD BEAM CONDITION
DETECTOR HEAD TILT
DIAPHRAGM
ENTRANCE SURFACE
FOCAL SPOT TO IMAGE RECEPTOR DISTANCE
FOCAL SPOT TO SKIN DISTANCE
GEOMETRICAL FIELD SIZE
GEOMETRICAL RADIATION FIELD
IMAGE PLANE
IMAGE RECEPTION AREA
IMAGE RECEPTION PLANE
INPUT APERTURE
IRRADIATION FIELD SIZE
ISOCENTRE
ISOCENTRIC
LIGHT DETECTOR
LIGHT FIELD
LIGHT FIELD -INDICATOR
NARROW BEAM
NARROW BEAM CONDITION
OUTPUT BEAM AREA
OUTPUT BEAM DIMENSIONS (NON-UNIFORM EXCITATION)
PATIENT SURFACE
PENUMBRA
RADIATION SOURCE TO SKIN DISTANCE
RADIATION APERTURE
RADIATION BEAM
RADIATION BEAM AXIS
RADIATION FIELD
RATED FIELD SIZE
RATED RANGE
REFERENCE AXIS
REFERENCE DIRECTION
REFERENCE PLANE
SOURCE TO ENTRANCE PLANE DISTANCE (SED)
TARGET VOLUME
TREATMENT VOLUME
USEFUL BEAM
USEFUL FIELD
VIRTUAL SOURCE

MEDICAL RADIOLOGICAL TECHNIQUES
General rm-40

MEDICAL DIAGNOSTIC RADIOLOGY
MEDICAL RADIOLOGICAL EXAMINATION
MEDICAL RADIOLOGY
NUCLEAR MEDICINE
RADIOLOGICAL RADIOLOGY

RADIOTHERAPY
TREATMENT

MEDICAL RADIOLOGICAL TECHNIQUES
Diagnosis using beams rm-41
CINERADIOGRAPHY
COMPUTED TOMOGRAPHY
DENTAL PANORAMIC RADIOGRAPHY
DIRECT RADIOGRAPHY
DIRECT RADIOSCOPY
INDIRECT RADIOGRAPHY
INDIRECT RADIOSCOPY
RADIOGRAPHY
RADIOSCOPY
RADIOSCOPICALLY GUIDED INVASIVE PROCEDURE
RECONSTRUCTIVE TOMOGRAPHY
SERIAL RADIOGRAPHY
SINGLE PHOTON EMISSION COMPUTED TOMOGRAPHY (SPECT)
TOMOGRAPHIC PLANE
TOMOGRAPHIC SECTION
TOMOGRAPHIC SECTION THICKNESS
TOMOGRAPHIC VOLUME
TOMOGRAPHY
TOTAL FIELD OF VIEW

MEDICAL RADIOLOGICAL TECHNIQUES
Therapy using beams rm-42
ANNIHILATION RADIATION
BEAM OFF
BEAM ON
BRACHYRADIOTHERAPY
BRACHYTHERAPY SOURCE MODEL / BRACHYTHERAPY SOURCE MODELING
INTERSTITIAL RADIOTHERAPY
INTRACAVITARY RADIOTHERAPY
MOVING BEAM RADIOTHERAPY
STATIONARY RADIOTHERAPY
SUPERFICIAL RADIOTHERAPY
TELERADIOTHERAPY
X-RAY THERAPY

MEDICAL RADIOLOGICAL TECHNIQUES
Nuclear medicine rm-43

DOSIMETRY
General rm-50
DOSEMETER
DOSEMETER (PATIENT CONTACT)
DOSIMETER (DIAGNOSTIC)
DOSIMETER (RADIOTHERAPY)
RADIATION METER

DOSIMETRY
RADIATION DETECTORS rm-51
CHAMBER (IONIZATION)
CHAMBER ASSEMBLY
DOSE AREA PRODUCT METER
EFFECTIVE RANGE
EXPOSURE METER
IONIZATION CHAMBER
LEAKAGE CURRENT (CHAMBER ASSEMBLY)
RADIATION DETECTOR
SENSITIVE VOLUME
TRANSMISSION CHAMBER

DOSIMETRY
PHANTOMS rm-52
PHANTOM

PROTECTION AGAINST IONIZING RADIATION
General rm-60
RADIATION PROTECTION
RADIOLOGICAL PROTECTION

PROTECTION AGAINST IONIZING RADIATION
Limits and factors rm-61
DOSE EQUIVALENT LIMIT
WORKLOAD

PROTECTION AGAINST IONIZING RADIATION
Groups of persons rm-62

PROTECTION AGAINST IONIZING RADIATION
Areas rm-63
PROTECTED AREA
SIGNIFICANT ZONE OF OCCUPANCY

PROTECTION AGAINST IONIZING RADIATION
Means of protection rm-64
OVARY SHIELD
PROTECTIVE BARRIER
PROTECTIVE DEVICE
PROTECTIVE GLASS PLATE
PROTECTIVE GLASS PLATE TYPE SC
PROTECTIVE GLASS PLATE TYPE VI
PROTECTIVE GONAD APRON
PROTECTIVE MITTEN
PRIMARY PROTECTIVE SHIELDING
PROTECTIVE SHIELDING
SCROTUM SHIELD
SHADOW SHIELD
STRUCTURAL SHIELDING

TESTING OF RADIOLOGICAL EQUIPMENT
General rm-70
ACCEPTANCE TEST
CONSTANCY TEST
FILM ILLUMINATOR
FILM PROCESSOR
HYDRAULIC TEST PRESSURE
INSTRUMENT PARAMETER
INVASIVE MEASUREMENT
QUALITY ASSURANCE
QUALITY ASSURANCE PROGRAMME
QUALITY CONTROL
REFERENCE CONDITIONS
REFERENCE DATA
REFERENCE INDICATED VALUE
REFERENCE SCALE READING
REFERENCE VOLUME
SITE TEST
SPEED INDEX
STANDARD TEST CONDITIONS
STATUS TEST
TYPE TEST
VALIDATION
VERIFICATION

TESTING OF RADIOLOGICAL EQUIPMENT
Test EQUIPMENT rm-71
AIR-DENSITY CHARACTERISTIC
BASE DEPTH
CALIBRATION FACTOR
CERTIFIED RADIOACTIVE STANDARD SOURCE
COMPOSITION OF REFERENCE MATERIALS
EFFECTIVE RADIATED POWER (ERP)
FIELD-CLASS DOSIMETER
HALF VALUE LAYER TEST DEVICE
INITIAL CONSTANCY TEST FILM

INITIAL REFERENCE FILM
INSTRUMENT ACCURACY
IONIZATION CHAMBER TEST SOURCE
MEASURING ASSEMBLY
MTF ANALYZER
MULTI-DETECTOR COUNTER
NON-INVASIVE MEASUREMENT
NON-IRRADIATED CONSTANCY TEST FILM
PINHOLE CAMERA
RADIOACTIVE IMPURITY
RADIOACTIVE STANDARD SOURCE
RADIONUCLIDE CALIBRATOR
RADIONUCLIDE FACTOR
RATED LENGTH (OF USE)
REFERENCE POINT (OF A CHAMBER)
REFERENCE POINT (OF A RADIATION DETECTOR)
REFERENCE-CLASS DOSIMETER
SAMPLE VOLUME CHARACTERISTIC
SLIT CAMERA
STANDARD TEST VALUES
STAR PATTERN CAMERA
TEST DEVICE
TRACEABLE RADIOACTIVE STANDARD SOURCE
UNIFORM CONSTANCY TEST FILM

TESTING OF RADIOLOGICAL EQUIPMENT
VERIFICATION of characteristics rm-72
ENERGY CALIBRATION
FILM BASE PLUS FOG DENSITY
FOCAL SPOT PINHOLE RADIOGRAM
FOCAL SPOT SLIT RADIOGRAM
FOCAL SPOT STAR RADIOGRAM
INTRINSIC LINE SPREAD FUNCTION
INTRINSIC NON-UNIFORMITY OF RESPONSE
INTRINSIC SPATIAL NON-LINEARITY
IMMUNITY LEVEL
IMMUNITY TEST LEVEL
MINIMUM EFFECTIVE RANGE
MINIMUM RATED RANGE
ROUTINE TEST
SPATIAL RESOLUTION (IN CT EQUIPMENT)
SPECIFIED ENERGY RESPONSE
STABILITY CHECK DEVICE
STABILIZATION TIME
STANDARD
STANDARD MEASUREMENT DEPTH
STAR PATTERN RESOLUTION LIMIT
SYSTEM LINEARITY
ZERO DRIFT (MEASURING ASSEMBLY)
ZERO SHIFT (MEASURING ASSEMBLY)

TESTING OF RADIOLOGICAL EQUIPMENT
Concepts in mathematics, metrics and statistics rm-73
BASELINE VALUE
COEFFICIENT OF VARIATION
COMBINED STANDARD UNCERTAINTY
COMPUTED TOMOGRAPHY DOSE INDEX (CTDI)
COMPUTED TOMOGRAPHY DOSE INDEX 100 (CTDI100)
COMPUTED TOMOGRAPHY NUMBER (CT NUMBER)
CONVENTIONAL TRUE VALUE
COORDINATE SYSTEM OF PROJECTION
CORRECTION FACTOR
ERROR OF MEASUREMENT
EXPANDED UNCERTAINTY
FULLWIDTH AT HALF MAXIMUM (FWHM)
FULL WIDTH AT TENTH MAXIMUM (FWTM)
HAZARD ANALYSIS
INDICATED VALUE
INTERVENTIONAL REFERENCE POINT
INTRINSIC ERROR
ISOPLANATIC REGION
LIMITS OF VARIATION
LINE SOURCE
LINE SPREAD FUNCTION (LSF)
MAXIMUM TOLERABLE RISK
MEASURED VALUE
MODULATION TRANSFER FUNCTION (MTF)
NOISE
NOMINAL (VALUE)
NON- LINEARITY
OPTICAL TRANSFER FUNCTION (OTF)
OVERALL UNCERTAINTY
RANDOM UNCERTAINTY
REFERENCE VALUE
RELATIVE INTRINSIC ERROR
RESIDUAL RISK
RISK
SAFETY
SAFETY FACTOR
SAFETY HAZARD
SAFETY INTEGRITY
SCALE READING
SEVERITY
SINGLE FAULT CONDITION
TRUE VALUE

TESTING OF RADIOLOGICAL EQUIPMENT
Obligation and statement of compliance rm-74
COMPLIANCE LEVEL or IMMUNITY COMPLIANCE LEVEL
SPECIFIC
SPECIFIED

TECHNOLOGY
General rm-80
DESIGNED FOR DEVELOPMENT LIFE-CYCLE
EMERGENCY TROLLEY EQUIPMENT
HAND-HELD EQUIPMENT
HARD COPY CAMERA
HIGH VOLTAGE
IEC 60601 TEST LEVEL
IMAGE DISPLAY DEVICE
INFORMATION TECHNOLOGY EQUIPMENT (ITE)
LIFE SUPPORTING EQUIPMENT OR SYSTEM
LOW VOLTAGE
MEDICAL ELECTRICAL EQUIPMENT (REFERRED TO AS EQUIPMENT)
MEDICAL ELECTRICAL SYSTEM
MOBILE EQUIPMENT
MODEL OR TYPE REFERENCE
NATIONAL STANDARD
PASSWORD
PERFORMANCE CHARACTERISTIC
PROGRAMMABLE ELECTRICAL MEDICAL SYSTEM (PEMS)
PROGRAMMABLE ELECTRONIC SUBSYSTEM (PESS)
PROGRAMMABLE ELECTRONIC SYSTEM (PES)
PROPERLY INSTALLED
PUBLIC MAINS NETWORKS
RATED (VALUE)
RADIO FREQUENCY (RF)
TOOL
VOLTAGE RIPPLE

TECHNOLOGY
Documentation rm-82

ACCOMPANYING DOCUMENTS
ASSEMBLING INSTRUCTIONS
ESTABLISHED CRITERIA
INSTRUCTIONS FOR USE
NORMAL USE
RISK MANAGEMENT FILE
RISK MANAGEMENT SUMMARY
WORKING STANDARD

TECHNOLOGY
EQUIPMENT rm-83

ACCESS COVER
ACCESSIBLE CONDUCTIVE PARTS
ACCESSIBLE METAL PART
ACCESSIBLE PART
ACCESSIBLE SURFACE
ACCESSORY
ADDRESS PILE UP
AIR CLEARANCE
BASIC INSULATION
CATEGORY AP EQUIPMENT
CATEGORY APG EQUIPMENT
CLASS I EQUIPMENT
CLASS II EQUIPMENT
COLD CONDITION
CONDUCTIVE CONNECTION
CONTINUOUS OPERATION
CONTINUOUS OPERATION WITH INTERMITTENT LOADING
CONTINUOUS OPERATION WITH SHORT-TIME LOADING
CONTROL PANEL
CONTROLLING TIMER
CREEPAGE DISTANCE
DEFIBRILLATION-PROOF APPLIED PART
DETACHABLE POWER SUPPLY CORD
DIRECT CARDIAC APPLICATION
DISINFECTABLE EQUIPMENT
DOUBLE INSULATION
EARTH LEAKAGE CURRENT
ELECTROMAGNETIC COMPATIBILITY (ABBREVIATION EMC)
ELECTROMAGNETIC DISTURBANCE
ELECTROMAGNETIC EMISSION
ELECTROMAGNETIC ENVIRONMENT
ELECTROMAGNETIC NOISE
ELECTROSTATIC DISCHARGE: (ESD)
EMISSION (ELECTROMAGNETIC)
ENCLOSURE
ENCLOSURE LEAKAGE CURRENT
EXTERNAL TERMINAL DEVICE
EXCLUSION BAND
FIXED EQUIPMENT
FIXED MAINS SOCKET OUTLET
FIXED SETTING (OF A CONTROL OR LIMITING DEVICE)
FLAMMABLE ANAESTHETIC MIXTURE WITH AIR
FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE
F-TYPE ISOLATED (FLOATING) APPLIED PART (F-TYPE APPLIED PART)
FUNCTION (OF AN EQUIPMENT AND/OR SYSTEM)
FUNCTIONAL EARTH CONDUCTOR
FUNCTIONAL EARTH TERMINAL
HARD-WIRED
IMMUNITY (TO A DISTURBANCE)
INTERCONNECTION TERMINAL DEVICE
INTERLOCK
INTERNAL ELECTRICAL POWER SOURCE
INTERNALLY POWERED EQUIPMENT
LARGE EQUIPMENT AND/OR SYSTEM
LEAKAGE CURRENT
LIVE
MAINS CONNECTOR
MAINS PART
MAINS PLUG
MAINS TERMINAL DEVICE
OVER-CURRENT RELEASE
OPERATING FREQUENCY
PATIENT AUXILIARY CURRENT
PATIENT CIRCUIT
PATIENT CONNECTION
PATIENT ENVIRONMENT
PATIENT LEAKAGE CURRENT
PERMANENTLY INSTALLED EQUIPMENT
PHYSIOLOGICAL SIMULATION FREQUENCY
PORTABLE EQUIPMENT
POTENTIAL EQUALIZATION CONDUCTOR
POWER SUPPLY CORD
PRESSURE (OVERPRESSURE)
PROTECTIVE COVER
PROTECTIVE EARTH CONDUCTOR
PROTECTIVE EARTH TERMINAL
PROTECTIVELY EARTHED
QUENCH
REINFORCED INSULATION
SAFETY DEVICE
SAFETY EXTRA-LOW VOLTAGE (SELV)
SAFETY EXTRA-LOW VOLTAGE TRANSFORMER
SECONDARY TIMER
SELF-RESETTING THERMAL CUT-OUT
SEPARATION DEVICE
SERIAL NUMBER
SHORT-TIME OPERATION
SIGNAL INPUT PART
SIGNAL OUTPUT PART
STATIC LOAD
STATIONARY EQUIPMENT
STERILIZABLE EQUIPMENT
SUPPLEMENTARY INSULATION
SUPPLY EQUIPMENT
SUPPLY MAINS
SURFACE DOSE
TERMINAL DEVICE
THERMAL CUT-OUT
THERMOSTAT
TIMING DEVICE
TOTAL LOAD
TRANSPORTABLE EQUIPMENT
TYPE B APPLIED PART
TYPE BF APPLIED PART
TYPE CF APPLIED PART

TECHNOLOGY
Operation of
EQUIPMENT rm-84

ADJUSTABLE SETTING (OF A CONTROL OR LIMITING DEVICE)
APPLIED PART
AUXILIARY MAINS SOCKET-OUTLET
DEGRADATION (OF PERFORMANCE)
DISPLAY
DUTY CYCLE
INFLUENCE QUANTITY
INTERMITTENT OPERATION
MAXIMUM PERMISSIBLE WORKING PRESSURE
MEDICAL SUPERVISION
MODE OF OPERATION
PREPARATORY STATE
READY STATE
SAFE WORKING LOAD
STAND-BY STATE
TRANSFER

TECHNOLOGY
Persons rm-85

MANUFACTURER
OPERATOR

PATIENT
QUALIFIED PERSON
USER

MAGNETIC RESONANCE
General rm-90
COMPLIANCE VOLUME
CONTROLLED ACCESS AREA
EFFECTIVE STIMULATION DURATION (TS)
EMERGENCY FIELD SHUT DOWN UNIT
FIRST LEVEL CONTROLLED OPERATING MODE
GRADIENT OUTPUT
GRADIENT UNIT
HEAD RF TRANSMIT COIL
HEAD SAR
LOCAL RF TRANSMIT COIL
LOCAL SAR
MAGNETIC RESONANCE (MR)
MAGNETIC RESONANCE EQUIPMENT (MR EQUIPMENT)
MAGNETIC RESONANCE EXAMINATION (MR EXAMINATION)
MAGNETIC RESONANCE SYSTEM (MR SYSTEM)
NORMAL OPERATING MODE
PARTIAL BODY SAR
ROUTINE MONITORING
SEARCH COIL
SECOND LEVEL CONTROLLED OPERATING MODE
SPECIAL PURPOSE GRADIENT SYSTEM
SPECIFIC ABSORPTION RATE(SAR)
TIME RATE OF CHANGE OF THE MAGNETIC FIELD (dB/dt)
TRANSVERSE FIELD MAGNET
VOLUME RF TRANSMIT COIL
WHOLE BODY GRADIENT SYSTEM
WHOLE BODY MAGNET
WHOLE BODY MAGNETIC RESONANCE EQUIPMENT (WHOLE BODY MR EQUIPMENT)
WHOLE BODY RF TRANSMIT COIL
WHOLE BODY SAR

ULTRASOUND
General rm-100
-12 dB OUTPUT BEAM AREA
-12 dB OUTPUT BEAM DIMENSIONS
ACOUSTIC ATTENUATION COEFFICIENT
ACOUSTIC WORKING FREQUENCY
APPLIANCE COUPLER
APPLIANCE INLET
APPLICATION DISTANCE
APPLICATION LIMITS
APPLICATION PLANE
ATTENUATED BEAM
ATTENUATED BEAM QUALITY
ATTENUATED OUTPUT POWER
ATTENUATED PEAK-RAREFACTIONAL ACOUSTIC PRESSURE
ATTENUATED PULSE-AVERAGE INTENSITY
ATTENUATED PULSE-INTENSITY INTEGRAL
ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY
ATTENUATED TEMPORAL-AVERAGE INTENSITY
BEAM ALIGNMENT AXIS
BEAM AREA
BONE THERMAL INDEX
BOUNDED OUTPUT POWER
BREAK-POINT DEPTH
COMBINED-OPERATING MODE
CRANIAL-BONE THERMAL INDEX
DEPTH FOR TIB
DEPTH FOR TIS
DEPTH OF DOSE MAXIMUM
DISCRETE-OPERATING MODE
EQUIVALENT BEAM DIAMETER
EQUIVALENT APERTURE DIAMETER
EQUIVALENT BEAM AREA
FULL SOFTWARE CONTROL OF ACOUSTIC OUTPUT
MAXIMUM GRADIENT SLEW RATE
MECHANICAL INDEX
MULTI-PURPOSE ULTRASONIC EQUIPMENT
NON-SCANNING MODE
OUTPUT POWER
PEAK-RAREFACTIONAL ACOUSTIC PRESSURE
PULSE AVERAGE INTENSITY
PULSE BEAM-WIDTH
PULSE DURATION
PULSE-INTENSITY INTEGRAL
PULSE REPETITION RATE
PULSE-PRESSURE-SQUARED INTEGRAL
SCANNING MODE
SOFT TISSUE THERMAL IINDEX
SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY
THERMAL INDEX
TRANSDUCER ASSEMBLY
TRANSMIT PATTERN
ULTRASONIC DIAGNOSTIC EQUIPMENT
ULTRASONIC TRANSDUCER

S

T

U

V

W

X

Z

Term	Definition	Reference	Used in IEC
–12 dB OUTPUT BEAM AREA	Area of the ultrasonic beam derived from the –12 dB OUTPUT BEAM DIMENSIONS. Symbol: A_{aprt}. Unit: centimetre squared, cm^2.		IEC 60601-2-37:2001
–12 dB OUTPUT BEAM DIMENSIONS	Dimensions of the ultrasonic beam (–12 dB PULSE BEAM WIDTH) in specified directions normal to the BEAM ALIGNMENT AXIS and at the TRANSDUCER output face. NOTE 1 For reasons of measurement accuracy the –12 dB OUTPUT BEAM DIMENSIONS can be derived from measurements at a distance chosen to be as close as possible to the face of the TRANSDUCER, and if possible no more than 1 mm from the face. NOTE 2 For contact TRANSDUCERS, these dimensions can be taken as the dimensions of the radiating element. Symbol: *X, Y*. Unit: centimetres, cm.		IEC 60601-2-37:2001
ABSORBED DOSE	Letter symbol: *D*. Mean energy imparted by IONIZING RADIATION to matter. ABSORBED DOSE is determined as the quotient of $d\bar{\varepsilon}$ by d*m*, where $d\bar{\varepsilon}$ is the mean energy imparted by IONIZING RADIATION to matter of mass d*m*: $D = \frac{d\bar{\varepsilon}}{dm}$ The unit of ABSORBED DOSE is the joule per kilogram ($J.kg^{-1}$). The special name of the unit of ABSORBED DOSE is the gray (Gy). The earlier unit of ABSORBED DOSE was the rad, 1 rad being equal to 10^{-2} $J.kg^{-1}$.	rm-13-08	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976/ A1:2000 IEC 62083:2000
ABSORBED DOSE RATE	Letter symbol: $\dot{D}$. ABSORBED DOSE per unit time. ABSORBED DOSE RATE is determined as the quotient of d*D* by d*t*, where d*D* is the increment of ABSORBED DOSE in the time interval d*t*: $\dot{D} = \frac{dD}{dt}$ A unit of ABSORBED DOSE RATE is any quotient of the gray or its multiples or submultiples by a suitable unit of time ($Gy{\cdot}s^{-1}$, $mGy{\cdot}h^{-1}$, etc.).	rm-13-09	60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60976/ A1:2000 IEC 62083:2000
ABSORBED DOSE RATE TO WATER	Letter symbol: $\dot{D}$. Following the definition in C.5 of ICRU 33, ABSORBED DOSE RATE to water is the quotient of d*D* by d*t*, where d*D* is the increment of ABSORBED DOSE to water in the time interval d*t*. The unit of ABSORBED DOSE RATE to water is $Gy \cdot s^{-1}$ ($Gy \cdot min^{-1}$; $Gy \cdot h^{-1}$).		IEC 60731/A1:2002
ABSORBED DOSE TO WATER	Letter symbol: *D*. Following the definition in C.4 of ICRU 33, ABSORBED DOSE to water is the quotient of $d\bar{\varepsilon}$ by d*m* where $d\bar{\varepsilon}$ is the mean energy imparted by IONIZING RADIATION to water of mass d*m*. The unit of ABSORBED DOSE to water is Gy (where 1 Gy = 1 J · kg^{-1}).		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
ABSORPTION	Phenomenon in which incident RADIATION transfers to the matter which it traverses some or all its energy. NOTE SCATTERING accompanied by energy loss, for example the compton effect and NEUTRON slowing down, is considered to be ENERGY ABSORPTION.	rm-12-05	IEC 61223-3-1:1999
ACCEPTANCE TEST	TEST carried out after new EQUIPMENT has been installed, or major modifications have been made to existing EQUIPMENT, in order to verify compliance with contractual specifications.	rm-70-01	IEC 60627:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61267:1994 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000
ACCEPTANCE TEST	TEST carried out at the request and with the participation of the user or his representative to ascertain by determination of proper performance parameters that the instrument meets the specifications claimed by the vendor. NOTE An ACCEPTANCE TEST should be carried out at the time of installation and when appropriate after major service. During or immediately after ACCEPTANCE TESTING, REFERENCE DATA are collected to be used as a standard for comparison with future ROUTINE TESTS.		IEC 61948-1:2001 IEC 61948-2:2001
ACCESS COVER	Part of an ENCLOSURE or guard providing the possibility of access to EQUIPMENT parts for the purpose of adjustment, inspection, replacement or repair.	NG.01.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
ACCESSIBLE CONDUCTIVE PARTS	Conducting parts of EQUIPMENT which can be touched without the use of a TOOL.		IEC 60601-2-9:1996
ACCESSIBLE METAL PART	Metal part of EQUIPMENT which can be touched without the use of a TOOL. See also NG.01.22.	NG.01.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60731/A1:2002 IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
ACCESSIBLE PART	Part of EQUIPMENT which can be touched without the use of a TOOL.	NG.01.22	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-26:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
ACCESSIBLE SURFACE	Surface of EQUIPMENT or of an EQUIPMENT part that can be easily or accidentally touched by persons without the use of a TOOL.	rm-84-07	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-33:2002
ACCESSORY	Additional component for use with an EQUIPMENT in order: – to perform its intended use; – to adapt the EQUIPMENT to some special use; – to facilitate the use of the EQUIPMENT; – to enhance the performance of the EQUIPMENT; – to enable the functions of the EQUIPMENT to be integrated with those of other EQUIPMENT.	rm-83-06	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61267:1994

Term	Definition	Reference	Used in IEC
ACCESSORY	Additional component for use with an EQUIPMENT in order: – to perform its intended use; – to adapt the EQUIPMENT to some special use; – to facilitate the use of the EQUIPMENT; – to enhance the performance of the EQUIPMENT; – to enable the functions of the EQUIPMENT to be integrated with those of other EQUIPMENT. Separate programmers are regarded as accessories and therefore a component part of the EQUIPMENT.		IEC 60601-2-24:1998
ACCESSORY	Optional component necessary and/or suitable to be used with EQUIPMENT in order to enable, facilitate or improve the intended use of EQUIPMENT or to integrate additional functions.	NG.01.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-29:1999
ACCOMPANYING DOCUMENT	Document accompanying a medical device, or an ACCESSORY, and containing important information for the USER, OPERATOR, installer or assembler of the medical device particularly regarding SAFETY. NOTE Based on IEC 60601-1:1988, definition 2.1.4.		ISO 14971:2000

Term	Definition	Reference	Used in IEC
ACCOMPANYING DOCUMENTS	Documents provided with an installation, EQUIPMENT, ASSOCIATED EQUIPMENT or ACCESSORY and containing important information for the assembler, installer and USER, particularly regarding SAFETY.	rm-82-01	IEC 60336:1993 IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 60601-2-44: 2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60731/A1:2002 IEC 60976/ A1:2000 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61303:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61674/ A1:2002 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 62083:2000

Term	Definition	Reference	Used in IEC
ACCOMPANYING DOCUMENTS	Documents accompanying EQUIPMENT or an ACCESSORY and containing all important information for the USER, OPERATOR, installer or assembler of EQUIPMENT, particularly regarding SAFETY. Recommended replacement: rm-82-01	NG.01.04	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-4:2000 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-12:2001 IEC 60601-2-17/ A1: 1996 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
ACCOMPANYING DOCUMENTS	Documents provided with an installation, EQUIPMENT, ASSOCIATED EQUIPMENT or ACCESSORY, containing important information for the assembler, installer and USER, particularly regarding SAFETY (IEC 60788 rev., MR-128-01). Recommended replacement: NG.01.04		IEC 60580:2000
ACOUSTIC ATTENUATING COEFFICIENT	Coefficient intended to account for ultrasonic ATTENUATION of tissue between the source and a specified point. Symbol: α. Unit: decibels per centimetre per megahertz, dB cm^{-1} MHz^{-1}.		IEC 60601-2-37:2001
ACOUSTIC WORKING FREQUENCY	Arithmetic mean of the most widely separated frequencies f_1 and f_2 at which the amplitude of the pressure spectrum of the acoustic signal is 3 dB lower than the peak amplitude. Symbol: f_{awf}. Unit: megahertz, MHz.		IEC 60601-2-37:2001
ACOUSTIC WORKING FREQUENCY	Frequency of an acoustic signal based on the observation of the output of a hydrophone placed in an acoustic field. The signal is analysed using the zero-crossing frequency technique (see 3.4.1 of IEC 61102). [IEC 61689, definition 3.3]		IEC 60601-2-5:2000
ACTIVE ELECTRODE	Electrode intended to produce certain physical effects required in electrosurgery, for example CUTTING and coagulation.		IEC 60601-2-2:1998
ACTIVITY	Letter symbol: A. Quantitative indication of the RADIOACTIVITY of an amount of RADIONUCLIDE in a particular energy state at a given time. ACTIVITY is determined as the quotient of dN by dt, where dN is the expectation value of the number of spontaneous nuclear transitions from that energy state in the time interval dt: $A = \frac{dN}{dt}$ The unit of ACTIVITY is the reciprocal second (s^{-1}). The special name of the unit of ACTIVITY is the becquerel (Bq), 1 Bq being equal to one transition per second. The earlier unit of ACTIVITY was the curie (Ci), 1 Ci being equal to 3.7×10^{10} transitions per second.	rm-13-18	IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60789:1992 IEC 61262-5:1994 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-1:2001 IEC 61948-2:2001
ACTUAL FOCAL SPOT	Area on the surface of the TARGET that intercepts the beam of accelerated particles.	rm-20-12	IEC 60336:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
ADDED FILTER	Removable or irremovable FILTER positioned in the RADIATION BEAM to provide part or all of the ADDITIONAL FILTRATION.	rm-35-02	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60806:1984 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61267:1994
ADDITIONAL FILTRATION	QUALITY EQUIVALENT FILTRATION due to ADDED FILTERS and other removable materials in the RADIATION BEAM which are between the RADIATION SOURCE and the PATIENT or a specified plane.	rm-13-47	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-44:2002 IEC 60627:2001 IEC 60806:1984 IEC 61223-3-1:1999
ADDRESS PILE-UP	For imaging devices false address calculation of an artificial event which passes the PULSE amplitude analyzer window, but is formed from two or more events by the pile-up effect.		IEC 61675-1:1998
ADJUSTABLE SETTING (of a control or limiting device)	Setting which can be altered by the OPERATOR without the use of a TOOL.	NG.09.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
ADMINISTRATION SET	Device(s) that convey(s) liquid from the supply via the EQUIPMENT to the PATIENT.		IEC 60601-2-24:1998
ADMINISTRATION SET CHANGE INTERVAL	Time recommended by the MANUFACTURER of the EQUIPMENT for using the ADMINISTRATION SET.		IEC 60601-2-24:1998
AFTERLOADING	Manual or remotely-controlled transfer of one or more SEALED RADIOACTIVE SOURCES between a STORAGE CONTAINER and pre-positioned SOURCE APPLICATORS for BRACHYRADIOTHERAPY.	rm-42-54	IEC 60601-2-17 A1:1996

Term	Definition	Reference	Used in IEC
AIR CLEARANCE	Shortest path in air between two conductive parts.	NG.03.01	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-44: 2002 IEC 60601-2-45:2001
AIR CONTROLLED INCUBATOR	INCUBATOR in which the air temperature is automatically controlled by an air temperature sensor close to a value set by the USER.		IEC 60601-2-19 A1:1996
AIR CONTROLLED TRANSPORT INCUBATOR	TRANSPORT INCUBATOR in which the air temperature is automatically controlled by an air temperature sensor close to a value set by the USER.		IEC 60601-2-20 A1:1996
AIR KERMA	Letter symbol: K. Quotient of dE_{tr} by dm, where dE_{tr} is the sum of the initial kinetic energies of all the charged particles in a mass dm of air, thus $K = \frac{dE_{tr}}{dm}$. Unit: J kg^{-1}. The special name for the unit of AIR KERMA is gray (Gy) (ICRU 60).	rm-13-11	IEC 60580:2000
AIR KERMA	Letter symbol: K. Following the definition in C.6 of ICRU 33, AIR KERMA is the quotient of dE_{tr} by dm where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in air of mass dm. The unit of AIR KERMA is Gy (where 1 Gy = 1 J · kg^{-1}). **Recommended replacement: precise definition in IEC 60580 (2000)**		IEC 60731/A1:2002
AIR KERMA	KERMA measured in a mass of air. **Recommended replacement: precise definition in IEC 60580 (2000)**	rm-13-11	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17 /A1: 1996 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
AIR KERMA	Letter symbol: *K*. Quotient of dE_{tr} by d*m*, where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in air of mass d*m*. The unit of AIR KERMA is Gy (where 1 Gy = 1 J · kg^{-1}), (see C.6 of ICRU 33). **Recommended replacement: precise definition in IEC 60580 (2000)**		IEC 61674 /A1:2002
AIR KERMA LENGTH	Letter symbol: *K.l*. For any straight line passing through the cross sectional X-ray scan of a CT machine, AIR KERMA LENGTH is the infinite integral of the product of AIR KERMA and elemental length along this line. The unit of AIR KERMA LENGTH is Gy·m (mGy·m).		IEC 61674 /A1:2002
AIR KERMA RATE	Letter symbol: $\dot{K}$. Quotient of d*K* by d*t*, where d*K* is the increment of AIR KERMA in the time interval d*t*, thus $\dot{K} = \frac{dK}{dt}$. Unit: J kg^{-1} s^{-1}. If the special name gray is used, the unit of AIR KERMA RATE is gray per second (Gy s^{-1}) (ICRU).	rm-13-54	IEC 60580:2000
AIR KERMA RATE	Letter symbol: $\dot{K}$. Following the definition in C.7 of ICRU 33, AIR KERMA RATE is the quotient of d*K* by d*t*, where d*K* is the increment of AIR KERMA in the time interval d*t*. The unit of AIR KERMA RATE is Gy · s^{-1} (Gy · min^{-1}; Gy · h^{-1}). **Recommended replacement see IEC 60580 (2000)**		IEC 60731/A1:2002
AIR KERMA RATE	Letter symbol: $\dot{K}$. Quotient of d*K* by d*t*, where d*K* is the increment of AIR KERMA in the time interval d*t*. The unit of AIR KERMA RATE is Gy/s (Gy/min; Gy/h), (see C.7 of ICRU 33). **Recommended replacement see IEC 60580 (2000)**		IEC 61674/ A1:2002
AIR-DENSITY CHARACTERISTIC	Two-dimensional function relating the instrument reading with temperature and PRESSURE.		IEC 61303:1994
ALARM	Signal which indicates abnormal events occurring to the PATIENT or EQUIPMENT.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
ALARM CONDITION	A condition that occurs when a variable that is being monitored by an ALARM SYSTEM equals or falls outside the set ALARM LIMIT(S).		IEC 60601-2-13:2003
ALARM LIMIT	Value(s) which are set by the MANUFACTURER, the device, the USER or OPERATOR which define the threshold range of the ALARM CONDITION.		IEC 60601-2-13:2003
ALARM SIGNAL	A signal the purpose of which is to alert the OPERATOR to an abnormal condition in the PATIENT or the EQUIPMENT that may develop into a SAFETY HAZARD which requires OPERATOR awareness or action.		IEC 60601-2-13:2003
ALARM SYSTEM	A system that is intended to make the OPERATOR(s) aware of an ALARM CONDITION, in the PATIENT or EQUIPMENT, by means of its ALARM SIGNAL(S).		IEC 60601-2-13:2003
AMBULATORY ELECTROCARDIOGRAPHIC SYSTEM (EQUIPMENT)	AMBULATORY RECORDER and a PLAYBACK EQUIPMENT, both of which may contain an analysis function. NOTE This EQUIPMENT is often referred to as Holter monitoring EQUIPMENT after its inventor, Dr. Norman Holter.		IEC 60601-2-47:2001
AMBULATORY RECORDER	Recording EQUIPMENT worn or carried by the PATIENT including associated ELECTRODES and cables for recording or recording and analysing heart action potentials.		IEC 60601-2-47:2001

Term	Definition	Reference	Used in IEC
ANAESTHETIC GAS DELIVERY SYSTEM	Assembly of components which controls and delivers the fresh gas into the ANAESTHETIC BREATHING SYSTEM. NOTE It may include a flow control system, flow meters and/or a gas mixing system and ANAESTHETIC GAS DELIVERY SYSTEM PIPING.		IEC 60601-2-13:2003
ANAESTHETIC GAS DELIVERY SYSTEM PIPING	All pipework, including unions, from unidirectional valves in the pipeline inlets and from the outlets of the pressure regulator(s) to the flow control system, as well as the PIPING connecting the flow control system and the piping connecting the ANAESTHETIC VAPOUR DELIVERY DEVICE to the FRESH GAS OUTLET. It includes piping leading to and from pneumatic ALARM SYSTEM(s), pressure indicators, oxygen flush and gas power outlets.		IEC 60601-2-13:2003
ANAESTHETIC SYSTEM (ANAESTHETIC WORKSTATION)	Inhalational ANAESTHETIC SYSTEM that contains an ANAESTHETIC GAS DELIVERY SYSTEM, an ANAESTHETIC BREATHING SYSTEM and the required MONITORING DEVICE(S), ALARM SYSTEM(s), and PROTECTION DEVICES. NOTE The ANAESTHETIC SYSTEM may include, but is not limited to, ANAESTHETIC VAPOUR DELIVERY DEVICE(S) and ANAESTHETIC VENTILATOR(S) and their associated MONITORING DEVICE(S), ALARM SYSTEM(s) and PROTECTION DEVICE(S).		IEC 60601-2-13:2003
ANAESTHETIC VAPOUR DELIVERY DEVICE	Device which provides the vapour of an anaesthetic agent in a controllable concentration.		IEC 60601-2-13:2003
ANAESTHETIC VENTILATOR	Automatic device, which is connected via the ANAESTHETIC BREATHING SYSTEM to the PATIENT'S airway and is designed to augment or provide ventilation of the PATIENT during anaesthesia.		IEC 60601-2-13:2003
ANALYSING ELECTROCARDIOGRAPH	ELECTROCARDIOGRAPH capable of analysing heart action potentials, deriving measurements from them and/or making interpretative statements. These may be also capable of communicating ECGS and/or analysis results.		IEC 60601-2-51:2003
ANNIHILATION RADIATION	IONIZING RADIATION that is produced when a particle and its antiparticle interact and cease to exist.		IEC 61675-1:1998
ANNUNCIATION	Communication of ALARM SIGNALS to the OPERATOR.		IEC 60601-2-13:2003
ANODE	In an X-RAY TUBE, electrode to which ELECTRONS forming a beam are accelerated and which usually contains the TARGET.	rm-22-06	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996
ANODE COOLING CURVE	Curve showing the ANODE HEAT CONTENT as a function of time with zero ANODE INPUT POWER, beginning after a LOADING when the ANODE HEAT CONTENT is equal to the maximum ANODE HEAT CONTENT.	rm-36-29	IEC 60601-2-28:1993 IEC 60613:1989
ANODE ANGLE	TARGET ANGLE in an X-RAY TUBE or in an X-RAY TUBE ASSEMBLY.	rm-22-07	IEC 60336:1993
ANODE HEAT CONTENT	Momentary value of the heat contained in the ANODE of an X-RAY TUBE accumulated during, or retained after, LOADINGS.	rm-36-26	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989

Term	Definition	Reference	Used in IEC
ANODE HEATING CURVE	Curve showing the ANODE HEAT CONTENT as a function of LOADING TIME for specified ANODE INPUT POWER.	rm-36-28	IEC 60601-2-28:1993 IEC 60613:1989
ANODE INPUT POWER	Power applied to the ANODE of an X-RAY TUBE to produce X-radiation.	rm-36-22	IEC 60601-2-28:1993 IEC 60613:1989
ANODE SPEED	In a rotating ANODE X-RAY TUBE, angular velocity at which the ANODE rotates, usually expressed in revolutions per minute.	rm-36-35	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989
ANTI-SCATTER GRID	Device to be placed before the IMAGE RECEPTION AREA in order to reduce the incidence of SCATTERED RADIATION upon that area and thus increase the contrast in the X-RAY PATTERN.	rm-32-06	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
ANTI-SCATTER GRID	Device with a fixed periodic arrangement of materials with different X-RAY ATTENUATION properties to be placed in front of the IMAGE RECEPTION AREA in order to reduce the incidence of SCATTERED RADIATION upon that area and thus increase the contrast in the X-RAY PATTERN. **Recommended replacement: rm-32-06**		IEC 60627:2001
APPARENT RESISTANCE OF SUPPLY MAINS	For diagnostic X-RAY GENERATOR, resistance of the SUPPLY MAINS determined under specific load conditions.	rm-36-16	IEC 60601-2-7:1998 IEC 60601-2-44: 2002 IEC 60601-2-45:2001
APPLIANCE COUPLER	Means enabling the connection of a flexible cord to EQUIPMENT without the use of a TOOL, consisting of two parts: a MAINS CONNECTOR and an APPLIANCE INLET.	NG.07.01	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-13:2003

Term	Definition	Reference	Used in IEC
APPLIANCE INLET	Part of an APPLIANCE COUPLER incorporated in or fixed to EQUIPMENT.	NG.07.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
APPLICATION DISTANCE	Distance from the EFFECTIVE FOCAL SPOT to the APPLICATION PLANE.		IEC 61267:1994
APPLICATION LIMITS	Letter symbols: f_1, f_2; unit: cm. Lower, f_1, and upper, f_2, limits of the distance from the FOCAL SPOT to the incident face of a FOCUSED GRID or a PARALLEL GRID between which the obtained RADIOLOGICAL information can be considered acceptable for many purposes.		IEC 60627:2001
APPLICATION LIMITS	Letter symbols: lower limit: f_1; upper limit: f_2. For a FOCUSED GRID, limits of the distance from the FOCAL SPOT to the incident face between which the RADIOLOGICAL information obtained can generally be expected to be acceptable.	rm-32-19	IEC 60601-2-7:1998
APPLICATION PLANE	Plane perpendicular to the REFERENCE AXIS, where the standard RADIATION CONDITION is defined.		IEC 61267:1994
APPLICATOR	An ACCESSORY or part of the EQUIPMENT intended to be used to couple the r.f. power to the PATIENT, but excluding the associated connecting cables.		IEC 60601-2-3/ A1:1998
APPLICATOR	Radiator, i.e., an aerial with a directional effect, such as a dipole with reflector, a dipole array, open waveguide or dielectric radiator for local application of microwave energy to the PATIENT.		IEC 60601-2-6:1984
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT.	NG.01.05	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-17/A1:1996 IEC 60601-2-26:2002 IEC 60601-2-29:1999 IEC 60601-2-37:2001 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
APPLIED PART	A part of a DOSEMETER, the RADIATION DETECTOR (for example CHAMBER ASSEMBLY) together with any additional PROTECTIVE COVER provided by the MANUFACTURER, intended for physical contact (not electrical contact) with the PATIENT (for example for intracavitary use).		IEC 60601-2-9:1996
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. Accessible parts of APPLICATORS.		IEC 60601-2-3/ A1:1998

Term	Definition	Reference	Used in IEC
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. Accessible parts of APPLICATORS and their associated connecting cables or waveguides and their connectors.		IEC 60601-2-6:1984
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. The STIMULATOR ELECTRODES and all parts conductively connected to them.		IEC 60601-2-10 /A1: 2001
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT, or any part of the VENTILATOR intended to be connected to the breathing system.		IEC 60601-2-12:2001
APPLIED PART	The EXTRACORPOREAL CIRCUIT and the DIALYSING FLUID circuit and/or all parts permanently and conductively connected to it.		IEC 60601-2-16:1998
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. For some ENDOSCOPIC EQUIPMENT, the APPLIED PART extends, as seen from the PATIENT, into the SUPPLY UNIT(S) to the point(s) where the required separation is provided (see 17a) of the General Standard).		IEC 60601-2-18 /A1: 2000
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. For some ENDOSCOPIC EQUIPMENT, the APPLIED PART extends, as seen from the PATIENT, into the SUPPLY UNIT(S) to the point(s) where the required separation is provided (see 17a) and 17 c) of the General Standard).		IEC 60601-2-18/ A1: 2000
APPLIED PART	The definition of IEC 60601-1 (see amendment 2) applies.		IEC 60601-2-19 /A1: 1996 IEC 60601-2-20/ A1: 1996
APPLIED PART	TRANSDUCER and its connecting lead.		IEC 60601-2-23:1999

Term	Definition	Reference	Used in IEC
APPLIED PART	Entirety of all parts of the EQUIPMENT including the infusion liquid pathway that is intentionally in contact with the PATIENT being treated in NORMAL USE.		IEC 60601-2-24:1998
APPLIED PART	The occluding cuff and any integral TRANSDUCERS, their connecting leads and pressure tubes.		IEC 60601-2-30:1999
APPLIED PART	The TRANSDUCER, including any fluid filled system.		IEC 60601-2-34:2000
APPLIED PART	All parts of the BED which can intentionally or unintentionally come into contact with the PATIENT, are considered an APPLIED PART. (See Figure 111.)		IEC 60601-2-38 /A1: 1999
APPLIED PART	The part of the DIALYSING SOLUTION circuit that conveys DIALYSING SOLUTION from the EQUIPMENT to the peritoneal cavity of the PATIENT, and subsequently to a drainage bag or drain, or parts permanently and conductively connected to it, shall be considered as the APPLIED PART.		IEC 60601-2-39:1999
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. NOTE Except if intended for such purpose, a SURGICAL LUMINAIRE or LUMINAIRE FOR DIAGNOSIS has no APPLIED PART on the PATIENT.		IEC 60601-2-41:2000
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – needs to be touched by the PATIENT.		IEC 60601-2-49:2001
APPLIED PART INTERFACE	That portion of the APPLIED PART intended to come into contact with the PATIENT'S skin.		IEC 60601-2-23:1999
ARTERIAL PRESSURE	The PRESSURE measured in the EXTRACORPOREAL CIRCUIT between the PATIENT and the arterial blood pump.		IEC 60601-2-16:1998
ARTEFACT / ARTIFACT	Apparent structure visible in the image which does not represent a structure within the object and which cannot be explained by NOISE or the MODULATION TRANSFER FUNCTION of the system.	rm-32-67	IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996
ARTEFACT	Apparent structure visible in the image which does not represent a structure within the object.		IEC 61223-3-4:2000
ASSEMBLING INSTRUCTIONS	Those parts of ACCOMPANYING DOCUMENTS giving information enabling an assembler to observe necessary precautions with respect to SAFETY and functional performance when assembling EQUIPMENT, equipment parts or sub-assemblies according to their specified purpose.	rm-82-03	IEC 60601-1-3:1994

Term	Definition	Reference	Used in IEC
ASSOCIATED EQUIPMENT	In a RADIOLOGICAL INSTALLATION, EQUIPMENT other than those for the production and control of IONIZING RADIATION, but essential for its application.	rm-30-01	IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
ATTACHMENT HEAD	ACCESSORY intended to be attached to the TREATMENT HEAD for the purpose of modifying the ultrasonic beam characteristics.		IEC 60601-2-5:2000
ATTENUATED BEAM	X-ray beam exiting the PATIENT or PHANTOM.		IEC 61674 /A1:2002
ATTENUATED BEAM QUALITY	RADIATION QUALITY of the X-ray beam exiting the PATIENT or PHANTOM.		IEC 61674/ A1:2002
ATTENUATED OUTPUT POWER	Value of the acoustic OUTPUT POWER after ATTENUATION and at a specified distance from the TRANSDUCER, and given by: $P_a = P10^{(-azf_{awf}/10)}$ where α is the ACOUSTIC ATTENUATION COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; P_α is the ATTENUATED OUTPUT POWER in milliwatts; P is the OUTPUT POWER in milliwatts measured in water. Symbol: P_α. Unit: milliwatts, mW.		IEC 60601-2-37:2001
ATTENUATED PEAK-RAREFACTIONAL ACOUSTIC PRESSURE	Value of the PEAK-RAREFACTIONAL ACOUSTIC PRESSURE after ATTENUATION and at a specified point, and given by $p_{ra}(z) = p_r(z)10^{(-azf_{awf}/20)}$ where α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest, in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; $p_r(z)$ is the PEAK-RAREFACTIONAL ACOUSTIC PRESSURE measured in water. Symbol: p_{ra}. Unit: megapascals, MPa.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
ATTENUATED PULSE-AVERAGE INTENSITY	Value of the acoustic PULSE-AVERAGE INTENSITY after ATTENUATION and at a specified point, and given by $I_{\mathrm{pa},\alpha} = I_{\mathrm{pa}}(z)10^{(-azf_{\mathrm{awf}}/10)}$ where α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY, at distance z in megahertz; $I_{pa}(z)$ is the PULSE-AVERAGE INTENSITY measured in water, in milliwatts per centimetre squared. Symbol: $I_{pa\ \alpha}$. Unit: watts per centimetre squared, W cm^{-2}.		IEC 60601-2-37:2001
ATTENUATED PULSE-INTENSITY INTEGRAL	Value of the PULSE-INTENSITY INTEGRAL after ATTENUATION and at a specified point, and given by $I_{\mathrm{pi},\alpha} = I_{\mathrm{pi}}10^{(-azf_{awf}/10)}$ where α is the ACOUSTIC ATTENUATION COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; $I_{\mathrm{pi},\alpha}$ is the ATTENUATED PULSE-INTENSITY INTEGRAL in millijoules per centimetre squared; I_{pi} is the PULSE-INTENSITY INTEGRAL measured in water in millijoules per centimetre squared. Symbol: $I_{\mathrm{pi},\alpha}$. Unit: millijoules per centimetre squared, mJ/cm^2.		IEC 60601-2-37:2001
ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY	Value of the SPATIAL-PEAK TEMPORAL AVERAGE INTENSITY after ATTENUATION and at a specified distance z, and given by $I_{\mathrm{zpta},\alpha}(z) = I_{\mathrm{zpta}}(z)10^{(-azf_{awf}/10)}$ where α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; $I_{\mathrm{zpta}}(z)$ is the SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at a specified distance z in milliwatts per centimetre squared measured in water. Symbol: $I_{\mathrm{zpta},\alpha}(z)$. Unit: milliwatts per centimetre squared, mW cm^2.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
ATTENUATED TEMPORAL-AVERAGE INTENSITY	Value of the TEMPORAL-AVERAGE INTENSITY after ATTENUATION and at a specified point, and given by $I_{ta,\alpha}(z) = I_{ta}(z)10^{(-azf_{awf}/10)}$ where α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; $I_{ta,\alpha}(z)$ is the ATTENUATED TEMPORAL-AVERAGE INTENSITY in milliwatts per centimetre squared; $I_{ta}(z)$ is the TEMPORAL-AVERAGE INTENSITY measured in water in milliwatts per centimetre squared. Symbol: $I_{ta,\alpha}(z)$. Unit: milliwatts per centimetre squared, mW cm^2.		IEC 60601-2-37:2001
ATTENUATION	Reduction of a RADIATION QUANTITY upon passage of the RADIATION through matter resulting from all types of interaction with this matter. The RADIATION QUANTITY may be, for example, the particle flux density or the energy density. NOTE ATTENUATION does not include the geometric reduction of the RADIATION QUANTITY with distance from the RADIATION SOURCE.	rm-12-08	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17/ A1: 1996 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
ATTENUATION COEFFICIENT	Letter symbol: μ. For a material in a beam of uncharged ionizing particles, quotient $\frac{dN}{N}$ by d*l*, where $\frac{dN}{N}$ is the fraction of particles that experience interactions in traversing a distance d*l* in the material. $\mu = -\frac{1}{N}\frac{dN}{dl}$	rm-13-39	IEC 60601-1-3:1994 IEC 61267:1994
ATTENUATION EQUIVALENT	Letter symbol: δ. Thickness of a layer of reference material which, if substituted for the material under consideration in a beam of specified RADIATION QUALITY and under specified geometrical conditions, gives the same degree of ATTENUATION. The ATTENUATION EQUIVALENT is expressed in suitable submultiples of the metre together with the reference material and the RADIATION QUALITY of the incident beam.	rm-13-37	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 60601-2-45:2001 IEC 61262-1:1994 IEC 61262-4:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998
ATTENUATION RATIO	Ratio of the value of a specified RADIATION QUANTITY in the centre of a BROAD BEAM of specified RADIATION QUALITY with the attenuating material under consideration outside the beam, to the value at the same position and under the same conditions with this attenuating material placed in the beam.	rm-13-40	IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61331-1:1994
AUDITORY STIMULATOR	Parts of EQUIPMENT for the application of sound pressure from a TRANSDUCER (headphone, bone conductor or free-field) to the ear(s) of the PATIENT, for the evoking of biopotentials or other action.		IEC 60601-2-40:1998
AUTOMATED EXTERNAL DEFIBRILLATOR (AED)	A DEFIBRILLATOR that, once activated by the OPERATOR, analyses the ECG obtained from ELECTRODES placed on the chest surface, identifies shockable cardiac rhythms, and automatically operates the DEFIBRILLATOR when a shockable rhythm is detected, hereinafter referred to as an AED. NOTE AEDs may provide varying levels of automation and be referred to by various terms.		IEC 60601-2-4:2002
AUTOMATIC CONTROL SYSTEM	In an X-RAY GENERATOR, system in which the control or limitation of the electric energy delivered to an X-ray tub assembly depends upon the measurement of one or more radiation quantities or corresponding physical quantities.	rm-36-45	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999

Term	Definition	Reference	Used in IEC
AUTOMATIC CYCLING NON-INVASIVE BLOOD PRESSURE MONITORING EQUIPMENT	A device, or part of a physiological monitoring or measuring system, including its associated accessories used for intermittent assessment of a PATIENT'S blood pressure by an externally applied means.		IEC 60601-2-30:1999
AUTOMATIC CYCLING NON-INVASIVE BLOOD PRESSURE MONITORING EQUIPMENT	Stand alone measuring EQUIPMENT or part of a physiological monitoring or measuring system, including associated TRANSDUCERS, that is used for the internal measurement of circulatory system pressures.		IEC 60601-2-34:2000
AUTOMATIC EXPOSURE CONTROL	In an X-RAY GENERATOR, mode of operation in which one or more LOADING FACTORS are controlled automatically in order to obtain at a pre-selected location a desired quantity of RADIATION.	rm-36-46	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61267:1994
AUTOMATIC EXPOSURE RATE CONTROL	In an X-RAY GENERATOR, mode of operation in which the rate of emitted RADIATION is controlled automatically by control of one or more LOADING FACTORS in order to obtain at a pre-selected location and in a pre-selected LOADING TIME a desired quantity of RADIATION.	rm-36-47	IEC 61223-3-1:1999
AUTOMATIC INTENSITY CONTROL	In an X-RAY GENERATOR, mode of operation in which one or more LOADING FACTORS are controlled automatically in order to obtain at a pre-selected location a desired rate of a RADIATION QUANTITY.	rm-36-48	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-2-9:1999
AUXILIARY MAINS SOCKET-OUTLET	Socket-outlet with MAINS VOLTAGE on EQUIPMENT, accessible without the use of a TOOL and intended for provision of mains supply to other EQUIPMENT or to other separate parts of the EQUIPMENT.	NG.07.04	IEC 60601-1/A2:1995 IEC 60601-2-12:2001 IEC 60601-2-13:2003
AVERAGE INCUBATOR TEMPERATURE	The average of the INCUBATOR TEMPERATURE readings taken at regular intervals achieved during STEADY TEMPERATURE CONDITION (see Figure 101).		IEC 60601-2-19/A1:1996
AVERAGE TEMPERATURE	The average of temperature readings taken at regular intervals at any specified point in the BABY COMPARTMENT achieved during STEADY TEMPERATURE CONDITION.		IEC 60601-2-19/A1:1996
AVERAGE TEMPERATURE	The average of the maximum and minimum temperatures at any specified point in the BABY COMPARTMENT achieved during STEADY TEMPERATURE CONDITION.		IEC 60601-2-20/A1:1996
AVERAGE TRANSPORT INCUBATOR TEMPERATURE	The average of the maximum and minimum TRANSPORT INCUBATOR TEMPERATURES achieved during STEADY TEMPERATURE CONDITION (see Figure 101).		IEC 60601-2-20/A1:1996
AXIAL FIELD OF VIEW	Dimensions of a slice through the TOMOGRAPHIC VOLUME parallel to and including the SYSTEM AXIS. In practice it is specified only by its axial dimension given by the distance between the centres of the outermost defined IMAGE PLANES plus the average of the measured AXIAL SLICE WIDTH measured as EQUIVALENT WIDTH (EW).	rm-32-51	IEC 61675-1:1998 IEC 61675-2:1998
AXIAL POINT SPREAD FUNCTION	Profile passing through the peak of the PHYSICAL POINT SPREAD FUNCTION in a plane parallel to the SYSTEM AXIS.	rm-32-52	IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
AXIAL RESOLUTION	For tomographs with sufficiently fine axial sampling fulfilling the sampling theorem, SPATIAL RESOLUTION along a line parallel to the SYSTEM AXIS.	rm-32-53	IEC 61675-1:1998 IEC 61675-2:1998
AXIAL SLICE WIDTH	For tomographs, the width of the AXIAL POINT SPREAD FUNCTION.	rm-33-54	IEC 61675-1:1998 IEC 61675-2:1998
BABY COMPARTMENT	An environmentally-controlled ENCLOSURE intended to contain a baby and with transparent section(s) which allows for viewing of the baby.		IEC 60601-2-19/A1:1996
BABY CONTROLLED INCUBATOR	An AIR CONTROLLED INCUBATOR which has additional capability of automatically controlling the INCUBATOR air temperature in order to maintain the temperature as measured by a SKIN TEMPERATURE SENSOR close to a value set by the USER.		IEC 60601-2-19/A1:1996
BABY CONTROLLED MODE	A mode of operation in which the power output varies automatically in response to the temperature of the baby, to achieve a temperature close to a value set by the USER.		IEC 60601-2-21/A1:1996
BABY CONTROLLED TRANSPORT INCUBATOR	An air controlled TRANSPORT INCUBATOR which has the additional capability of automatically controlling the INCUBATOR air temperature in order to maintain the temperature as measured by a SKIN TEMPERATURE SENSOR close to a value set by the USER.		IEC 60601-2-20/A1:1996
BACK POINTER	Luminous or mechanical device intended to indicate the RADIATION BEAM AXIS and its point of exit from the PATIENT.	rm-35-13	IEC 60976/ A1:2000
BACK-SCATTERING	SCATTERING of particles or RADIATION by material through angles greater than 90° with respect to their initial direction.	rm-12-04	IEC 60806:1984
BACTERIAL FILTER	Device that removes bacteria and particulate matter from the gas stream. [ISO 4135:1995, definition 4.1.7 modified]		IEC 60601-2-12:2001
BASE DEPTH	Depth in a PHANTOM of the plane containing the distal point of 90 % of the maximum ABSORBED DOSE on the RADIATION BEAM AXIS.		IEC 60976/A1:2000
BASELINE VALUE	REFERENCE VALUE of functional parameter: – either the value obtained for this parameter in the initial CONSTANCY TEST immediately following a STATUS TEST, or – where described in a corresponding particular standard, the mean value of values obtained in a series of initial CONSTANCY TESTS, immediately following a STATUS TEST.	rm-73-11	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
BASIC INSULATION	Insulation applied to LIVE parts to provide basic protection against electric shock.	NG.03.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
BEAM ALIGNMENT AXIS	Straight line joining the points of maximum PULSE-INTENSITY INTEGRAL measured at several different distances in the far field. For the purposes of alignment, this line may be projected to the face of the ULTRASONIC TRANSDUCER.		IEC 60601-2-37:2001
BEAM APPLICATOR	In MEDICAL RADIOLOGY, device usually attached to the RADIATION SOURCE ASSEMBLY performing at least one of the following functions: – to indicate the RADIATION BEAM AXIS; to indicate the RADIATION FIELD; – to ensure a minimum distance from the RADIATION SOURCE to the ENTRANCE SURFACE; – to serve as COMPRESSION DEVICE. NOTE 1 A BEAM APPLICATOR may include PROTECTIVE SHIELDING and serve as a BEAM LIMITING DEVICE. NOTE 2 As BEAM APPLICATORS may be mentioned: pointing APPLICATOR, open-ended APPLICATOR, dental BEAM APPLICATOR, therapeutic BEAM APPLICATOR.	rm-37-30	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60976/A1:2000 IEC 61223-2-7:1999 IEC 61223-3-4:2000 IEC 62083:2000
BEAM AREA	Area in the specified plane perpendicular to the BEAM-ALIGNMENT AXIS consisting of all points at which the PULSE-INTENSITY INTEGRAL is greater than a specified fraction of the maximum PULSE-INTENSITY INTEGRAL in that plane. NOTE For measurement purposes the PULSE-INTENSITY INTEGRAL can be taken as being proportional to the PULSE PRESSURE-SQUARED INTEGRAL.		IEC 60601-2-37:2001
BEAM LIMITING DEVICE	Device to limit the RADIATION FIELD.	rm-37-28	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 62083:2000

Term	Definition	Reference	Used in IEC
BEAM LIMITING SYSTEM	Entirety of parts and their geometrical configuration contributing to the limitation of the RADIATION BEAM.	rm-37-27	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-1:1994
BEAM NON-UNIFORMITY RATIO	Ratio of the square of the maximum r.m.s. acoustic pressure to the spatial average of the square of the r.m.s. acoustic pressure where the spatial average is taken over the EFFECTIVE RADIATING AREA, determined in accordance with IEC 61689. [IEC 61689, definition 3.9, modified]		IEC 60601-2-5:2000
BEAM OFF	The condition in which the RADIATION SOURCE (S) is fully shielded, and is also in a position in which it can be secured.		IEC 60601-2-11:1997
BEAM ON	The condition in which the RADIATION SOURCE (S) is fully exposed for RADIOTHERAPY.		IEC 60601-2-11:1997
BEAM SCATTERING FILTER	FILTER used in order to scatter a beam of ELECTRONS.	rm-35-09	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000
BEAM TYPE	Descriptive classification for the ultrasonic beam in one of three types: collimated, convergent or divergent. [IEC 61689, definition 3.11]		IEC 60601-2-5:2000
BEST FOCUS	Setting of focusing potentials resulting in maximum integrated area under the MTF curve for the given slit orientation. NOTE This setting of focusing potentials is chosen to reduce ambiguity and may slightly deviate from settings in practical use of the XRII.		IEC 61262-7:1995
BIOPOTENTIAL INPUT PART	APPLIED PART(s) of EQUIPMENT or SYSTEM for the collection of biopotentials.		IEC 60601-2-40:1998
BIPOLAR ELECTRODE	Assembly of two ACTIVE ELECTRODES on the same support, so constructed that, when energised, the hf current flows mainly between these two ELECTRODES.		IEC 60601-2-2:1998
BLANKET	Flexible HEATING DEVICE, which may be folded, for use under or over a PATIENT.		IEC 60601-2-35:1996
BLOOD LEAK	A leakage of blood from the blood compartment to the DIALYSING FLUID compartment of the DIALYSER due to a rupture of the semi-permeable membrane.		IEC 60601-2-16:1998
BLOOMING VALUE	As a characteristic of the EFFECTIVE FOCAL SPOT of an X-RAY TUBE, ratio of two resolution limits obtained under specific LOADING conditions.	rm-20-15	IEC 60336:1993
BOLUS	Discrete quantity of liquid which is delivered in a short time.		IEC 60601-2-24:1998
BONE THERMAL INDEX	THERMAL INDEX for applications, such as foetal (second and third trimester) or neonatal cephalic (through the fontanelle), in which the ULTRASOUND beam passes through soft tissue and a focal region is in the immediate vicinity of bone. Symbol: *TIB*. Unit: None. NOTE See DD.4.2 and DD.5.2 for methods of determining the BONE THERMAL INDEX.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
BOUNDARY AND DIMENSIONS OF THE X-RAY FIELD	In this collateral standard IEC 60601-1-3:1994, the boundary of an X-ray field (see rm-37-07), is described by the locus of points at which the AIR KERMA RATE is 25 % of the mean of the AIR KERMA RATE at the approximate centres of the quarters of the area enclosed. The dimensions of an X-ray field are described in terms of the lengths of its intercepts on each of two orthogonal major axes in the plane of interest. Unless otherwise stated, it is to be assumed that the plane of interest is at right angles to the REFERENCE AXIS; also that the major axes intersect on the REFERENCE AXIS and are oriented so that one axis is collinear with the PROJECTION of the longitudinal axis of the X-RAY TUBE lying in the plane and passing through this point of intersection.		IEC 60601-1-3:1994
BOUNDED OUTPUT POWER	OUTPUT POWER emitted in SCANNING MODE from a region of the active area of the TRANSDUCER whose width in the scan plane is limited to 1 cm. Symbol: P_1. Unit: milliwatts, mW.		IEC 60601-2-37:2001
BRACHYRADIOTHERAPY	Intracavitary, interstitial or SUPERFICIAL RADIOTHERAPY using one or more SEALED RADIOACTIVE SOURCES.	rm-42-52	IEC 62083:2000
BRACHYTHERAPY SOURCE MODEL/BRACHYTHERAPY SOURCE MODELING	All physical, geometric and radiation parameters required to plan a course of RADIOTHERAPY for a particular BRACHYTHERAPY RADIOACTIVE SOURCE. The process of establishing the BRACHYTHERAPY SOURCE MODEL is referred to as "BRACHYTHERAPY SOURCE MODELING".		IEC 62083:2000
BREAK-POINT DEPTH	Value equal to 1,5 times the EQUIVALENT APERTURE DIAMETER, and given by $z_{bd} = 1{,}5\ D_{eq}$ where D_{eq} is the EQUIVALENT APERTURE DIAMETER. Symbol: z_{bp}. Unit: centimetres, cm.		IEC 60601-2-37:2001
BROAD BEAM	RADIATION BEAM of such a solid angle that a further increase of the solid angle does not appreciably increase a measured RADIATION QUANTITY, thus including the contribution of SCATTERED RADIATION.	rm-37-24	IEC 60627:2001 IEC 61331-1:1994
BROAD BEAM CONDITION	Arrangement for the measurement of a RADIATION QUANTITY in a BROAD BEAM of IONIZING RADIATION.	rm-37-25	IEC 60627:2001 IEC 61267:1994
BUFFER-FREE HAEMODIAFILTRATION	A specific form of HDF where the buffer is not given to the PATIENT with the DIALYSING FLUID, but with the SUBSTITUTION FLUID.		IEC 60601-2-16:1998
BUILD UP	Phenomenon of the increase with depth of the ABSORBED DOSE RATE due to the release of secondary charged particles and to SCATTERED RADIATION in matter beyond the ENTRANCE SURFACE.	rm-12-12	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60976/ A1:2000
BUILD UP FACTOR	Letter symbol: *B*. For a material irradiated, ratio of the value of a RADIATION QUANTITY in the centre of a BROAD BEAM of specified RADIATION QUALITY and the corresponding value of the RADIATION QUANTITY in the centre of a NARROW BEAM, both values measured in the material under consideration.	rm-13-49	IEC 61331-1:1994
CALIBRATION ("CAL")	Facility enabling the CALIBRATION VOLTAGE and zero voltage to be recorded in place of the ELECTROCARDIOGRAM.		IEC 60601-2-51:2003
CALIBRATION FACTOR	For a CHAMBER ASSEMBLY with an associated MEASURING ASSEMBLY it is the factor which converts the INDICATED VALUE, corrected to stated REFERENCE CONDITIONS, to the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the IONIZATION CHAMBER. For an IONIZATION CHAMBER calibrated on its own without a specified MEASURING ASSEMBLY, the CALIBRATION FACTOR converts the ionization charge or current, corrected to REFERENCE CONDITIONS, to the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the CHAMBER (this is the reciprocal of RESPONSE under REFERENCE CONDITIONS).		IEC 60731/A1:2002
CALIBRATION INTERVAL	Recommended time between calibrations as described in the ACCOMPANYING DOCUMENTS.		IEC 60601-3-1:1996
CALIBRATION VOLTAGE	Voltage step recorded for amplitude CALIBRATION PURPOSES.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
CAPACITIVELY COUPLED HF CURRENT	Unavoidable high frequency current flowing from an ENDOSCOPICALLY-USED ACCESSORY to the ENDOSCOPE.		IEC 60601-2-18 A1:2000
CAPACITOR DISCHARGE HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR in which the electrical energy is stored in a HIGH VOLTAGE capacitor to be supplied to an X-RAY TUBE by discharge in a single LOADING.	rm-21-08	IEC 60601-1-3:1994 IEC 60601-2-7:1998
CAPSULE	Of a SEALED RADIOACTIVE SOURCE, container in which the radioactive material is hermetically sealed for its intended use.	rm-20-16	IEC 60601-2-17/A1:1996
CARDIAC DEFIBRILLATOR	MEDICAL ELECTRICAL EQUIPMENT intended to defibrillate the heart by an electrical PULSE via ELECTRODES applied either to the PATIENT'S skin (external ELECTRODES), or to the exposed heart (internal ELECTRODES). May be referred to as DEFIBRILLATOR or EQUIPMENT. NOTE Such EQUIPMENT may also include other monitoring or therapeutic functions.		IEC 60601-2-4:2002
CASSETTE CHANGER	SERIAL CHANGER in which each RECORD is taken upon a RADIOGRAPHIC FILM in a separate RADIOGRAPHIC CASSETTE.	rm-31-06	IEC 61223-2-11:1999
CATEGORY AP EQUIPMENT	EQUIPMENT or EQUIPMENT part complying with specified requirements on construction, marking and documentation in order to avoid sources of ignition in a FLAMMABLE ANAESTHETIC MIXTURE WITH AIR.	NG.02.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
CATEGORY APG EQUIPMENT	EQUIPMENT or EQUIPMENT part complying with specified requirements on construction, marking and documentation in order to avoid sources of ignition in a FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE.	NG.02.03	IEC 60601-1:1988 IEC 60601-1/A2:1995
CATHETER TIP TRANSDUCER	TRANSDUCER mounted at or close to the tip of a catheter and intended for insertion into the cardiovascular system.		IEC 60601-2-34:2000
CATHODE	In an X-RAY TUBE, source of the ELECTRONS.	rm-22-05	IEC 60613:1989
CATHODE EMISSION CHARACTERISTIC	Dependence of the X-RAY TUBE CURRENT on variables, for example filament heating current, X-RAY TUBE VOLTAGE.	rm-36-20	IEC 60601-2-28:1993 IEC 60613:1989
CENTRAL AXIS	The line perpendicular to the ENTRANCE PLANE passing through the CENTRE OF THE ENTRANCE FIELD.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CENTRAL ILLUMINANCE	(E_c) Illuminance at 1 m distance from the light-emitting area of the EQUIPMENT in THE LIGHT FIELD CENTRE (LFC) without any obstruction of the light beam.		IEC 60601-2-41:2000
CENTRAL LINE INDICATION	Marking on the incident face of a LINEAR GRID, which is intended to indicate the position and direction of the TRUE CENTRAL LINE. NOTE In most cases, this marking coincides with the geometric centre line of the grid's incident face.		IEC 60627:2001
CENTRAL MAGNIFICATION	As a characteristic of XRIIs, the ratio of the length in the OUTPUT IMAGE of the actual length of a small object placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS.		IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
CENTRAL TERMINAL ACCORDING TO WILSON (CT)	Terminal at the average potential of the R, L and F potentials.		IEC 60601-2-51:2003
CENTRE OF ROTATION (COR)	Origin of that coordinate system, which describes the PROJECTIONS of a transverse slice with respect to their orientation in space. NOTE The CENTRE OF ROTATION of a transverse slice is given by the intersection of the SYSTEM AXIS with the mid-plane of the corresponding OBJECT SLICE.		IEC 61675-2:1998
CENTRE OF THE ENTRANCE FIELD	That point in the ENTRANCE PLANE which is imaged at the CENTRE OF THE OUTPUT IMAGE.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CENTRE OF THE OUTPUT IMAGE	The centre of the smallest circle circumscribing the OUTPUT IMAGE.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CERENKOV COUNTER	Counting system which detects the Cerenkov radiation emitted from the sample. NOTE CERENKOV COUNTERS are used for measuring samples with β-emitting RADIONUCLIDES that have a particle energy larger than the Cerenkov threshold. Under special conditions, a LIQUID SCINTILLATION COUNTER can be used as a CERENKOV COUNTER.		IEC 61948-1:2001
CERTIFIED RADIOACTIVE STANDARD SOURCE	RADIOACTIVE SOURCE hat has been calibrated by a laboratory recognized as a country's national standardizing laboratory for RADIOACTIVITY measurements and has been so certified by the aforementioned laboratory.		IEC 61303:1994

Term	Definition	Reference	Used in IEC
CHAMBER (ionization)	An IONIZING RADIATION DETECTOR consisting of a CHAMBER filled with air, in which an electric field insufficient to produce gas multiplication is provided for the collection at the ELECTRODES of charges associated with the ions and the ELECTRONS produced in the measuring volume of the detector by IONIZING RADIATION. NOTE For this standard IEC 60731/ A1:2002, the IONIZATION CHAMBER is considered to consist of the measuring volume, the collecting electrode, the guard electrode (if any) the outer electrode (which consists of the CHAMBER wall and possibly a conducting coating), those parts of the insulator adjacent to the measuring volume, the build-up cap and water-proof housing (if any). There are several categories of IONIZATION CHAMBER: Shell CHAMBER: an IONIZATION CHAMBER with a measuring volume of between 0,1 cm^3 and 1,0 cm^3 bounded by a rigid outer electrode mounted on a supporting stem. The measuring volume is usually symmetrical about the axis of the stem and the CHAMBER is intended to be used with the axis of symmetry perpendicular to the axis of the RADIATION BEAM. There are two types of shell CHAMBER: 1) thimble CHAMBER: the outer electrode takes the form of a rigid cylindrical wall closed at one end and mounted at the other on the supporting stem; 2) spherical CHAMBER: the outer electrode takes the form of a rigid spherical wall mounted on the supporting stem; Parallel-plate CHAMBER: an IONIZATION CHAMBER with a measuring volume of between 0,01 cm^3 and 0,5 cm^3 bounded by parallel ELECTRODES. The CHAMBER is intended to be used with the ELECTRODES perpendicular to the axis of the RADIATION BEAM; Vented CHAMBER: an IONIZATION CHAMBER constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere such that corrections to the RESPONSE for changes in air density need to be made; Sealed CHAMBER: an IONIZATION CHAMBER constructed in such a way as to restrict the pathway between the air inside the measuring volume and the atmosphere sufficiently to ensure that the RESPONSE of the CHAMBER is independent of changes in ambient conditions over a period of time stated by the MANUFACTURER; Unguarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the cable surrounding the centre (signal) conductor terminates in the cable and does not extend into the stem or body of the CHAMBER ASSEMBLY; Partially guarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the cable surrounding the centre (signal) conductor extends well into the stem or body of the CHAMBER ASSEMBLY but does not enter the air in the CHAMBER; Guarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the stem or body of the CHAMBER ASSEMBLY is continuous with a guard electrode that is in contact with the air inside the CHAMBER.		IEC 60731/A1:2002
CHAMBER ASSEMBLY	The IONIZATION CHAMBER and all other parts to which the CHAMBER is permanently attached, except the MEASURING ASSEMBLY. It includes the electrical fitting and any permanently attached cable.	rm-51-08	IEC 60601-2-9:1996 IEC 60731/A1:2002
CHANNEL	In EQUIPMENT for remotely controlled after-loading, tubing in which a particular SEALED RADIOACTIVE SOURCE or assembly of SEALED RADIOACTIVE SOURCES is moved.	rm-25-02	IEC 60601-2-17/A1:1996
CHANNEL	Complete system for the amplification and conditioning of potential differences between a pair or combination of ELECTRODES.		IEC 60601-2-26:2002
CHANNEL	Hardware and/or software selection of a particular ELECTROCARDIOGRAPHIC LEAD for purposes of display, recording, or TRANSMISSION.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
CHARGING CIRCUIT	Circuit within the DEFIBRILLATOR intended for charging the ENERGY STORAGE DEVICE. This circuit includes all parts conductively connected to the ENERGY STORAGE DEVICE during the charging period.		IEC 60601-2-4:2002
CINERADIOGRAPHY	INDIRECT RADIOGRAPHY of moving objects usually in rapid series on cine film.	rm-41-14	IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-3-1:1999
CLASS I EQUIPMENT	EQUIPMENT in which protection against electric shock does not rely on BASIC INSULATION only, but which includes an additional SAFETY precaution in that means are provided for the connection of the EQUIPMENT to the PROTECTIVE EARTH CONDUCTOR in the fixed wiring of the installation in such a way that ACCESSIBLE METAL PARTS cannot become LIVE in the event of a failure of the BASIC INSULATION.	NG.02.04	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
CLASS II EQUIPMENT	EQUIPMENT in which protection against electric shock does not rely on BASIC INSULATION only, but in which additional SAFETY precautions such as DOUBLE INSULATION or REINFORCED INSULATION are provided, there being no provision for protective earthing or reliance upon installation conditions.	NG.02.05	IEC 60601-1:1988 IEC 60601-1/A2:1995
CLEARLY LEGIBLE	Visual attribute of information displayed by the EQUIPMENT that allows the OPERATOR to discern (or identify) qualitative or quantitative values or functions under a specific set of environmental conditions.		IEC 60601-2-12:2001
COAGULATION	Sealing of small blood vessels or of body tissue caused by the passage of high frequency current at the ACTIVE ELECTRODE(S).		IEC 60601-2-2:1998
COEFFICIENT OF VARIATION	Standard deviation of a set of readings expressed as a percentage of the mean value of these readings.	rm-73-12	IEC 60580:2000 IEC 61674/ A1:2002
COINCIDENCE DETECTION	A method which checks whether two opposing detectors have detected one PHOTON each simultaneously. By this method the two PHOTONS are concatenated into one event. NOTE THE COINCIDENCE DETECTION between two detector elements serves as an electronic collimation to define the corresponding PROJECTION BEAM or LINE OF RESPONSE (LOR), respectively.		IEC 61675-1:1998
COINCIDENCE WINDOW	Time interval during which tow detected PHOTONS are considered being simultaneous.		IEC 61675-1:1998
COLD CONDITION	The condition obtained if EQUIPMENT is de-energized for a sufficiently long time to attain the ambient temperature.	NG.10.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
COLLIMATOR (for GAMMA CAMERAS)	In a RADIONUCLIDE imaging device, block of radiation attenuating material with one or more APERTURES defining the field of view and limiting the angular spread of the RADIATION that can reach the RADIATION DETECTOR ASSEMBLY.	rm-34-05	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998

Term	Definition	Reference	Used in IEC
COLLIMATOR AXIS	Straight line which passes through the geometrical centre of the exit and ENTRANCE FIELDS of the COLLIMATOR.	rm-34-32	IEC 60789:1992 IEC 61948-2:2001
COLLIMATOR BACK FACE	Surface of the COLLIMATOR which is closest to the radiation detection assembly.		IEC 60789:1992
COLLIMATOR FRONT FACE	Surface of the COLLIMATOR which is closest to the object being imaged.		IEC 60789:1992
COMBINED STANDARD UNCERTAINTY	Defined in ISO: Guide to the expression of uncertainty in measurement (1993)		IEC 60580:2000
COMBINED-OPERATING MODE	Mode of operation of an EQUIPMENT which combines more than one DISCRETE-OPERATING MODE.		IEC 60601-2-37:2001
COMMON MODE DC OFFSET VOLTAGE	DC voltage appearing on LEAD ELECTRODES with respect to the NEUTRAL ELECTRODE resulting from ELECTRODE-skin voltages.		IEC 60601-2-51:2003
COMMON MODE REJECTION	Ability of the ELECTROCARDIOGRAPH including the PATIENT CABLE and LEAD ELECTRODES, high frequency filters, protection networks, LEAD networks, amplifier input, etc., to discriminate between signals with differences between amplifier inputs (differential signal) and signals common to both amplifier inputs (common signal), in the presence of LEAD ELECTRODE impedance imbalance.		IEC 60601-2-51:2003
(IMMUNITY) COMPLIANCE LEVEL	Level less than or equal to the IMMUNITY LEVEL for which the EQUIPMENT or SYSTEM meets the requirements of the applicable subclause of 36.202. NOTE Additional requirements for COMPLIANCE LEVELS are specified in 6.8.201.1.		IEC 60601-1-2:2001
COMPLIANCE VOLUME	Area of PATIENT accessible space in which compliance of GRADIENT OUTPUT is inspected In MR EQUIPMENT with a cylindrical WHOLE BODY MAGNET, the COMPLIANCE VOLUME is a cylinder with its axis coinciding with the magnet axis and with a radius of 0,20 m. In MR EQUIPMENT with a TRANSVERSE FIELD MAGNET and a WHOLE BODY GRADIENT SYSTEM, the COMPLIANCE VOLUME is a volume bound by planes parallel to the magnet poles and separated by a distance that is either the largest dimension of the accessible space between the poles of the magnet, or 0,40 m, whichever is less. In all other MR EQUIPMENT the COMPLIANCE VOLUME is the volume where any part of a PATIENT body can be properly located according to the intended use of the MR EQUIPMENT.		IEC 60601-2-33:2002
COMPOSITION OF REFERENCE MATERIALS	Values of ATTENUATION EQUIVALENT, HALF-VALUE LAYER and QUALITY EQUIVALENT FILTRATION expressed in this collateral standard IEC 60601-1-3:1994 as thickness of aluminum or lead, apply to reference materials of the following composition: – aluminum of purity 99,99 % or higher and density 2,70 g cm^{-3}; – lead of purity 99,99 % or higher and density 11,35 g cm^{-3}.		IEC 60601-1-3:1994

Term	Definition	Reference	Used in IEC
COMPRESSION DEVICE	In MEDICAL RADIOLOGY, device used to exert pressure upon a part of a PATIENT during either examination or TREATMENT.	rm-35-15	IEC 60601-1-3:1994 IEC 60601-2-45:2001 IEC 61223-2-10:1999
COMPUTED TOMOGRAPHY	RECONSTRUCTIVE TOMOGRAPHY in which recording and processing is effected by a computing system.	rm-41-20	IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-3-1:1999 IEC 62083:2000
COMPUTED TOMOGRAPHY DOSE INDEX (CTDI)	Integral of the DOSE PROFILE along a line perpendicular to the TOMOGRAPHIC PLANE from –7 times *T* to +7 times *T* (where *T* is the NOMINAL TOMOGRAPHIC SLICE THICKNESS), divided by the product of the NOMINAL TOMOGRAPHIC SLICE THICKNESS and the number of tomograms *N* produced in a single scan. $CTDI = {}_{-7xT}\int^{+7xT} \frac{D(z)}{NxT} dz$ where *T* is the NOMINAL TOMOGRAPHIC SLICE THICKNESS; *N* is the number of tomograms produced in a single scan; *D*(z) is the DOSE PROFILE along a line z perpendicular to the TOMOGRAPHIC PLANE. NOTE A scan can consist of a number of tomograms (slices).		IEC 61223-2-6:1994

Term	Definition	Reference	Used in IEC
COMPUTED TOMOGRAPHY DOSE INDEX 100 (CTDI100)	The integral of the DOSE PROFILE produced in a single axial scan along a line perpendicular to the TOMOGRAPHIC PLANE from –50 mm to –50 mm, divided by the product of the number of TOMOGRAPHIC SECTIONS *N* and the NOMINAL TOMOGRAPHIC SECTION THICKNESS *T* $CTDI_{100} = \int_{-50mm}^{+50mm} \frac{D(z)}{NxT} dz$ where *D(z)* is the DOSE PROFILE along a line *z* perpendicular to the TOMOGRAHIC PLANE, where dose is reported as ABSORBED DOSE to air; *N* is the number of TOMOGRAPHIC SECTIONS produced in a single axial scan of the X-RAY SOURCE; *T* is the NOMINAL TOMOGRAPHIC SECTION THICKNESS. NOTE 1 The term $CTDI_{vol}$ has been introduced as a more representative value for dose than the traditional *CTDI* integrated from –7T to –7T as defined by the FDA in 21 CFR 1020.331. NOTE 2 The dose is reported as ABSORBED DOSE to air. This is required in order to avoid present confusion, as some MANUFACTURERS of CT SCANNERS express dose values calculated as ABSORBED DOSE to air and others as ABSORBED DOSE to polymethyl-methacrylate (PMMA). Although $CTDI_{100}$ refers to ABSORBED DOSE to air, for practical purposes the evaluation of ABSORBED DOSE to air within a PMMA dosimetry PHANTOM is well approximated by measurement of the AIR KERMA with an IONIZATION CHAMBER in the PHANTOM. NOTE 3 This definition assumes that the DOSE PROFILE is centred on z = 0. NOTE 4 A single axial scan is typically a 360° rotation of the X-RAY SOURCE.		IEC 60601-2-44:2002
COMPUTED TOMOGRAPHY NUMBER (CT NUMBER)	Number used to represent the mean X-RAY ATTENUATION associated with each elemental area of the COMPUTED TOMOGRAPHY image. NOTE The COMPUTED TOMOGRAPHY NUMBER is normally expressed in Hounsfield units. MEASURED VALUES of ATTENUATION are transformed INTO COMPUTED TOMOGRAPHY NUMBERS using the international Hounsfield scale, using the expression: CT number of material = $\frac{\mu material - \mu water}{\mu water}$ x 1 000 where μ is the linear ATTENUATION COEFFICIENT. The CT number scale is defined so that water has a value of 0 and air a value of 1 000.		IEC 61223-2-6:1994
CONDITIONS OF ADEQUATE HEAT DISCHARGE	The conditions achieved when a HEATING DEVICE is supported and covered as specified in Annex EE.		IEC 60601-2-35:1996

Term	Definition	Reference	Used in IEC
CONDUCTIVE CONNECTION	Connection through which a current can flow exceeding the allowable LEAKAGE CURRENT.	NG.07.05	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-17/A1:1996 IEC 60601-2-51:2003
CONSTANCY TEST	Each of a series of tests, carried out: – to ensure that the functional performance of EQUIPMENT meets ESTABLISHED CRITERIA; or – to enable the early recognition of changes in the properties of components of the EQUIPMENT.	rm-70-03	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR with a PERCENTAGE RIPPLE of the output voltage not exceeding a specific value.	rm-21-06	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001
CONTACT SURFACE TEMPERATURE	The temperature T_R at the reference point of the heated APPLIED PART (see Figures 101a and 101b).		IEC 60601-2-35:1996
CONTINUATION	In RADIOTHERAPY, re-starting IRRADIATION after INTERRUPTION of IRRADIATION without re-selection of operating conditions.		IEC 60601-2-17 /A1:1996
CONTINUOUS MODE	For an X-RAY GENERATOR, mode of LOADING an X-RAY TUBE continuously as in RADIOTHERAPY or in RADIOSCOPY.	rm-36-42	IEC 60601-1-3:1994 IEC 60601-2-7:1998
CONTINUOUS OPERATION	Operation under normal load for an unlimited period, without the specified limits of temperature being exceeded.	NG.10.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-17/A1:1996 IEC 60601-2-51:2003
CONTINUOUS OPERATION WITH INTERMITTENT LOADING	Operation in which EQUIPMENT is connected continuously to the SUPPLY MAINS. The stated permissible LOADING TIME is so short that the long term on-load operating temperature is not attained. The ensuing interval in LOADING is, however, not sufficiently long for cooling down to the long term no-load operating temperature.	NG.10.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
CONTINUOUS OPERATION WITH SHORT-TIME LOADING	Operation in which EQUIPMENT is connected continuously to the SUPPLY MAINS. The stated permissible LOADING TIME is so short that the long term on-load operating temperature is not attained. The ensuing interval is, however, sufficiently long for cooling down to the long term no-load operating temperature.	NG.10.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
CONTINUOUS RECORDER	EQUIPMENT which performs continuous analysis and/or recording of the ECG.		IEC 60601-2-47:2001
CONTRAST IMPROVEMENT RATIO	Letter symbol: *K*. Characteristic of an ANTI-SCATTER GRID, evaluated as the ratio of the TRANSMISSION OF PRIMARY RADIATION to the TRANSMISSION OF TOTAL RADIATION, under specific measuring conditions.		IEC 60627:2001
CONTRAST INDEX	For CONSTANCY TESTS in X-RAY EQUIPMENT, difference between the SPEED INDEX and the value of optical density produced by a constant EXPOSURE from a light source, greater than that used for producing the SPEED INDEX. NOTE 1 This EXPOSURE is normally aimed at an optical density in the range from 1,6 to 2,0 above that of film base plugs fog density. NOTE 2 SPEED INDEX and CONTRAST INDEX are used as constancy parameters and are intended to facilitate the routine checks described in Technical report IEC 61223-2-1:1993. They must not be confused with the sensitometric definitions of SENSITIVITY in terms of speed and average gradient.		IEC 61223-2-1:1993 IEC 61223-2-10:1999
CONTRAST RATIO (abbreviation CR)	The ratio of the luminance at the CENTRE OF THE OUTPUT IMAGE with an unblocked X-ray beam to the luminance at the CENTRE OF THE OUTPUT IMAGE when the X-ray beam is blocked at the CENTRE OF THE ENTRANCE FIELD, under specific conditions.		IEC 61262-6:1994
CONTROL PANEL	Part of EQUIPMENT in which one or more manually operated devices are mounted for the purpose of controlling all, or some, of the functions of the EQUIPMENT. The CONTROL PANEL may contain devices for indicating and displaying operating factors.	rm-83-02	IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-3-1:1999
CONTROL SIDE RAIL	SIDE RAIL which incorporates BED function controls for PATIENT activation.		IEC 60601-2-38 /A1:1999
CONTROL TEMPERATURE	Temperature selected at the temperature control.		IEC 60601-2-19/A1:1996 IEC 60601-2-20/A1:1996
CONTROL TEMPERATURE	The temperature set at the temperature control.		IEC 60601-2-21/A1:1996
CONTROLLED ACCESS AREA	Area to which access is controlled for SAFETY reasons.		IEC 60601-2-33:2002
CONTROLLED AREA	Defined area which is part of an area under surveillance and for which access, occupancy and working conditions are regulated and controlled in order to protect persons against IONIZING RADIATION.	rm-63-05	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-45:2001
CONTROLLING TIMER	TIMING DEVICE changing a state of operation at the end of a predetermined time interval or of a predetermined total time that may consist of separate time intervals.	rm-83-04	IEC 60601-2-17 /A1:1996
CONTROLLING TIMER (abbreviation: timer)	Device to measure the time during which IRRADIATION occurs and, when a predetermined time is reached, to terminate IRRADIATION.		IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
CONVENTIONAL TRUE VALUE	Value used instead of the TRUE VALUE when calibrating or determining the performance of an instrument, since in practice the TRUE VALUE is unknown and unknowable. NOTE The CONVENTIONAL TRUE VALUE will usually be the value determined by the STANDARD with which the instrument under test is compared.	rm-73-13	IEC 60580:2000 IEC 61674/A1:2002 IEC 60731/A1:2002
CONVERGING COLLIMATOR	Focused COLLIMATOR the geometrical focal plane of which lies before its entrance face.	rm-34-07	IEC 60789:1992
CONVERSION FACTOR	The ratio of the luminance in the CENTRE OF THE OUTPUT IMAGE of a specific zone in the OUTPUT IMAGE to the AIR KERMA RATE in the CENTRE OF THE ENTRANCE FIELD.		IEC 61262-2:1994
COORDINATE SYSTEM OF PROJECTION	Cartesian system of the IMAGE MATRIX of each two-dimensional PROJECTION with axes X_p and Y_p (defined by the axis of the IMAGE MATRIX). The Y_p axis and the PROJECTION of the SYSTEM AXIS onto the detector front face have to be in parallel. The origin of the COORDINATE SYSTEM OF PROJECTION is the centre of the IMAGE MATRIX.		IEC 61675-2:1998
COORDINATE SYSTEM OF PROJECTION	Recommended replacement: IEC 61675-2:1998		IEC 61675-2:1998
CORE BIOPSY GUN	Automatic needle device for performing core biopsy.		IEC 60601-2-45:2001
CORRECTION FACTOR	Dimensionless multiplier which corrects the INDICATED VALUE of an instrument from its value when operated under particular conditions to its value when operated under stated REFERENCE CONDITIONS.	rm-73-14	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002 IEC 61676:2002
COUNT LOSS	Difference between measured COUNT RATE and TRUE COUNT RATE, which is caused by the finite RESOLVING TIME of the instrument.		IEC 61675-1:1998
COUNT RATE	Number of counts per unit of time.	rm-34-33	IEC 61675-1:1998 IEC 61675-3:1998
COUNT RATE	Recommended replacement: IEC 61675-1:1998, IEC 61675-3:1998		IEC 61675-2:1998
COUNT RATE CHARACTERISTIC	Function giving the relationship between observed COUNT RATE and TRUE COUNT RATE.	rm-34-21	IEC 60789:1992 IEC 61675-1:1998
CRANIAL-BONE THERMAL INDEX	THERMAL INDEX for applications, such as paediatric and adult cranial applications, in which the ULTRASOUND beam passes through bone near the beam entrance into the body. Symbol: *TIC*. Unit: None. NOTE See DD.4.3 for methods of determining the CRANIAL BONE THERMAL INDEX.		IEC 60601-2-37:2001
CREEPAGE DISTANCE	Shortest path along the surface of insulating material between two conductive parts.	NG.03.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
CROSS-GRID	ANTI-SCATTER GRID composed of two LINEAR GRIDS built together in such a way that the directions of their absorbing strips form an angle.		IEC 60627:2001

Term	Definition	Reference	Used in IEC
CUTTING	Resection or DISSECTION of body tissue caused by the passage of high frequency current of high current density at the ACTIVE ELECTRODE(S).		IEC 60601-2-2:1998
CT CONDITIONS OF OPERATION	All selectable parameters governing the operation of a CT SCANNER, for example NOMINAL TOMOGRAPHIC SECTION THICKNESS, PITCH FACTOR, FILTRATION, PEAK X-RAY TUBE VOLTAGE and either X-RAY TUBE CURRENT and LOADING TIME or CURRENT TIME PRODUCT.		IEC 60601-2-44:2002
CT DETECTOR	RADIATION DETECTOR which is used for CT DOSIMETRY.		IEC 61674/A1:2002
CT DOSIMETER	Diagnostic DOSIMETER which uses long narrow IONIZATION CHAMBERS and/or semi-conductor detectors for the measurement of AIR KERMA integrated along the length of the detector when the detector is exposed to a cross-sectional X-ray scan of a computed tomographic machine. A CT DOSIMETER contains the following components: – one or more detector assemblies; – a MEASURING ASSEMBLY.		IEC 61674/ A1:2002
CT PITCH FACTOR	The ratio of the PATIENT SUPPORT travel Δd along the z direction per rotation of the X-RAY SOURCE divided by the product of the NOMINAL TOMOGRAPHIC SECTION THICKNESS T and the number of TOMOGRAPHIC SECTIONS N. CT *pitch factor* $= \frac{\Delta d}{NxT}$ where Δd is the PATIENT SUPPORT travel along the z direction per rotation of the X-RAY SOURCE; T is the NOMINAL TOMOGRAPHIC SECTION THICKNESS; N is the number of TOMOGRAPHIC SECTIONS produced by a single axial scan of the X-RAY SOURCE.		IEC 60601-2-44:2002
CT SCANNER	X-RAY EQUIPMENT for COMPUTED TOMOGRAPHY (CT). A computed TOMOGRAPHY X-ray system is a diagnostic X-ray system intended to generate cross-sectional images of the body by computer reconstruction of X-ray transmission data from the same axial plane at different angles. This generic type of device may include signal analysis and display EQUIPMENT, PATIENT and EQUIPMENT supports, support parts and accessories. NOTE Secondary imaging processing is not included in the scope of this standard.		IEC 60601-2-44:2002
CT SCANNER	X-RAY EQUIPMENT for COMPUTED TOMOGRAPHY (CT). A computed TOMOGRAPHY X-ray system is a diagnostic X-ray system intended to generate cross-sectional images of the body by computer reconstruction of X-ray transmission data obtained at different angles. This generic type of device may include signal analysis and display EQUIPMENT, PATIENT SUPPORT, support parts and ACCESSORIES. NOTE Secondary imaging processing is not included in the scope of this standard		IEC 60601-2-44:2002

Term	Definition	Reference	Used in IEC
CURRENT TIME PRODUCT	In MEDICAL RADIOLOGY, quantity of electricity resulting from the LOADING of an X-RAY TUBE, expressed in milliampere seconds, as the product of the mean X-RAY TUBE CURRENT in milliamperes and the duration of the LOADING in seconds.	rm-36-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
DAS CONTRAST SENSITIVITY	Ability of the DAS system to display low contrast vessels against background.		IEC 61223-3-3:1996
DAS VISUAL SPATIAL RESOLUTION	Ability of the DAS system to display small structures of high contrast. NOTE DAS VISUAL SPATIAL RESOLUTION depends both on technical and observer performance.		IEC 61223-3-3:1996
DECENTRING OF A FOCUSED GRID	Distance from the FOCAL SPOT of an X-RAY TUBE to the plane through the TRUE CENTRAL LINE of a FOCUSED GRID and perpendicular to the incident face of the grid.		IEC 60627:2001
DECREASING INPUT POWER RATING	Highest permitted X-RAY TUBE LOAD given as a function of LOADING TIME for single LOADINGS during which the ANODE INPUT POWER is decreased in steps or continuously.	rm-36-39	IEC 60613:1989
DEFAULT SETTING	Specific state of control, THE ULTRASONIC DIAGNOSTIC EQUIPMENT will enter upon power-up, new PATIENT select or change from non-foetal to foetal applications.		IEC 60601-2-37:2001
DEFIBRILLATOR ELECTRODES	ELECTRODES intended to deliver an electrical PULSE to the PATIENT for the purpose of cardiac defibrillation. NOTE DEFIBRILLATOR ELECTRODES may also provide other monitoring (e.g. ECG acquisition) or therapeutic (e.g. transcutaneous pacing) functions and may be disposable or reusable.		IEC 60601-2-4:2002
DEFIBRILLATION-PROOF APPLIED PART	APPLIED PART having protection against the effects of a discharge of a cardiac DEFIBRILLATOR to the PATIENT.	NG.01.27	IEC 60601-1/A2:1995 IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-51:2003
DEFOCUSING OF A FOCUSED GRID	Difference between the distance from the FOCAL SPOT of an X-RAY TUBE to the incident face of a FOCUSED GRID and the FOCUSING DISTANCE of that grid.		IEC 60627:2001
DEGRADATION (OF PERFORMANCE)	Undesired departure in the operational performance of an EQUIPMENT or SYSTEM from its intended performance. NOTE The term "DEGRADATION" can apply to temporary or permanent failure. [IEV 161-01-19, modified]		IEC 60601-1-2:2001
DELINEATED LIGHT FIELD	For RADIOTHERAPY SIMULATORS, the area of the LIGHT FIELD bounded by the DELINEATOR shadow and in a plane perpendicular to the X-ray beam axis.		IEC 61168:1993
DELINEATED RADIATION BEAM	That part of the RADIATION BEAM bordered by the shadow cast by the DELINEATORS.		IEC 60601-2-29:1999
DELINEATED RADIATION FIELD	Interception of the DELINEATED RADIATION BEAM by a perpendicular plane to the RADIATION BEAM AXIS.		IEC 61217:2002

Term	Definition	Reference	Used in IEC
DELINEATED RADIATION FIELD	Area of the DELINEATED RADIATION BEAM intercepted on a plane perpendicular to the REFERENCE AXIS.		IEC 60601-2-29:1999
DELINEATOR	A means for defining the border which outlines the simulated RADIATION FIELD.		IEC 61217:2002
DELINEATOR(S)	Means for defining the border(s) of the simulated RADIATION FIELD.		IEC 60601-2-29:1999 IEC 61217:2002
DELIVERED ENERGY	Energy which is delivered through the DEFIBRILLATOR ELECTRODES and dissipated in the PATIENT or in a resistance of specified value.		IEC 60601-2-4:2002
DENTAL PANORAMIC RADIOGRAPHY	DIRECT RADIOGRAPHY of a part of or the complete dentition by the use of an intraoral X-RAY TUBE.	rm-41-11	IEC 61223-1:1993
DENTAL PANORAMIC TOMOGRAPHY	DIRECT RADIOGRAPHY of a part or of the complete dentition by the application of a slit-DIAPHRAGM in combination with the relative motion of the X-RAY TUBE and the X-RAY IMAGE RECEPTOR.	rm-41-12	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-3-4:2000
DEPTH DOSE	ABSORBED DOSE at a specified depth beneath the ENTRANCE SURFACE or the irradiated object, usually on the RADIATION BEAM AXIS.	rm-13-51	IEC 62083:2000
DEPTH FOR BONE THERMAL INDEX	Distance from the plane where the –12 dB OUTPUT BEAM DIMENSIONS are determined along the BEAM ALIGNMENT AXIS to the plane where the product of ATTENUATED OUTPUT POWER and attenuated PULSE-INTENSITY INTEGRAL is maximum. Symbol: z_b. Unit: centimetres, cm.		IEC 60601-2-37:2001
DEPTH FOR SOFT-TISSUE THERMAL INDEX	Distance from the plane where the –12 dB OUTPUT BEAM DIMENSIONS are determined along the BEAM ALIGNMENT AXIS to the plane at which the lower value of the ATTENUATED OUTPUT POWER and the product of the ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY and 1 cm^2 is maximized over the distance range equal to, or more than, 1,5 times the EQUIVALENT APERTURE DIAMETER. Symbol: z_s. Unit: centimetres, cm. NOTE In this particular standard, the restricted definition of SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY from 3.49 of IEC 61102 relating to a specified plane is used where SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY is replaced by ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY.		IEC 60601-2-37:2001
DEPTH OF ILLUMINATION	Working distance around 1 m below the emitting surface of the EQUIPMENT, in which the illuminance reaches at least 20 % of CENTRAL ILLUMINANCE (E_c). (See Figure 115.)		IEC 60601-2-41:2000
DEPTH OF DOSE MAXIMUM	Depth in a PHANTOM of the maximum ABSORBED DOSE on the RADIATION BEAM AXIS with the surface of the PHANTOM at a specified distance.		IEC 60976/ A1:2000
DESIGNED FOR	When used in standards to characterize EQUIPMENT, devices, components or arrangements: designates an intended and usually apparent purpose or use for the product.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
DETACHABLE POWER SUPPLY CORD	Flexible cord intended to be connected to EQUIPMENT by means of a suitable APPLIANCE COUPLER.	NG.07.06	IEC 60601-1:1988 IEC 60601-1/A2:1995
DETECTIVE QUANTUM EFFICIENCY (DQE)	The ratio of the squared signal-to-noise ratio present at the output of a RADIATION DETECTOR to the squared signal-to-noise ratio present at the input of that RADIATION DETECTOR.		IEC 61262-5:1994

Term	Definition	Reference	Used in IEC
DETECTOR ASSEMBLY	The RADIATION DETECTOR and all other parts to which the RADIATION DETECTOR is permanently attached, except the MEASURING ASSEMBLY.		IEC 60601-2-9:1996
DETECTOR ASSEMBLY	RADIATION DETECTOR and all other parts to which the RADIATION DETECTOR is permanently attached, except the MEASURING ASSEMBLY. NOTE The DETECTOR ASSEMBLY normally includes: – the RADIATION DETECTOR and the stem (or body) on which the RADIATION DETECTOR is permanently mounted (or embedded); – the electrical fitting and any permanently attached cable or pre-amplifier.		IEC 61674/A1:2002
DETECTOR FIELD OF VIEW (FOV)	Region of the detector within which events are included in the display image. This region shall be specified by the MANUFACTURER.		IEC 60789:1992 IEC 61675-3:1998
DETECTOR FIELD OF VIEW	Region of the detector within which events are included in the displayed image. This region has to be specified by the MANUFACTURER.		IEC 61948-2:2001
DETECTOR HEAD	Assembly of the RADIATION DETECTOR ASSEMBLY, the COLLIMATOR and the DETECTOR SHIELD.	rm-34-09	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998
DETECTOR HEAD	Consists of the RADIATION DETECTOR, the COLLIMATOR and the radiation shield.		IEC 61948-2:2001
DETECTOR HEAD TILT	Deviation of the COLLIMATOR AXIS from orthogonality with the SYSTEM AXIS.	rm-34-34	IEC 61675-2:1998 IEC 61948-2:2001
DETECTOR LINE SPREAD FUNCTION	The LSF measured with an uncollimated LINE SOURCE at a specified distance Z from the COLLIMATOR FRONT FACE.		IEC 60789:1992
DETECTOR POSITIONING TIME	Fraction of the total time spent on an acquisition which is not used in collecting data.		IEC 61675-2:1998
DETECTOR SHIELD	Component for attenuating IONIZING RADIATION outside the ENTRANCE FIELD of the COLLIMATOR.	rm-34-10	IEC 60789:1992
DEVELOPMENT LIFE-CYCLE	Necessary activities occurring during a period of time that starts at the concept phase of a project and finishes when the VALIDATION of the PEMS is complete.	rm-80-01	IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
DIALYSER	For the purpose of this Particular Standard, the term DIALYSER is used to describe any device containing a semi-permeable membrane that is used to perform HD/HDF/HF.		IEC 60601-2-16:1998
DIALYSING FLUID	A solution which is intended to exchange solutes and/or water with blood during HD/HDF. NOTE The words dialysate and dialysis fluid are commonly used as supplicated synonyms of DIALYSING FLUID.		IEC 60601-2-16:1998
DIALYSING FLUID CONCENTRATE	A solution of chemicals which, when appropriately diluted, produces DIALYSING FLUID.		IEC 60601-2-16:1998
DIALYSING SOLUTION	Pharmaceutical preparation (solution), according to the relevant Pharmacopoeia monograph for use with PERITONEAL DIALYSIS EQUIPMENT.		IEC 60601-2-39:1999

Term	Definition	Reference	Used in IEC
DIAPHRAGM	BEAM LIMITING DEVICE with either a fixed or an adjustable aperture in practically one plane.	rm-37-29	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 60976/A1:2000 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994
DIFFERENTIAL RADIAL IMAGE DISTORTION	IMAGE DISTORTION for a small, radially oriented TEST DEVICE of constant length placed in any position in the ENTRANCE PLANE. DIFFERENTIAL RADIAL IMAGE DISTORTION is a function of position of this TEST DEVICE in the ENTRANCE PLANE.		IEC 61262-4:1994
DIRECT CARDIAC APPLICATION	Use of APPLIED PART which may come in direct CONDUCTIVE CONNECTION to the PATIENT'S heart.	NG.02.07	IEC 60601-1:1988 IEC 60601-1/A2:1995
DIRECT FOCAL DISTANCE	Shortest distance from the X-RAY IMAGE RECEPTOR to the position of the FOCAL SPOT.		IEC 60601-2-45:2001
DIRECT RADIOGRAM	RADIOGRAM obtained directly at the IMAGE RECEPTION AREA.	rm-32-03	IEC 60601-2-1/A1:2002 IEC 60806:1984
DIRECT RADIOGRAPHY	RADIOGRAPHY in which the recording is effected at an IMAGE RECEPTION AREA.	rm-41-07	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000
DIRECT RADIOSCOPY	RADIOSCOPY in which the visible images are presented at the IMAGE RECEPTION AREA, or close to it, in the RADIATION BEAM.	rm-41-02	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61331-2:1994
DISABLE	State of indefinite duration in which the ALARM SYSTEM or part of the ALARM SYSTEM does not annunciate an auditory ALARM SIGNAL.		IEC 60601-2-13:2003
DISCHARGE CIRCUIT	Circuit within the DEFIBRILLATOR which connects the ENERGY STORAGE DEVICE to the DEFIBRILLATOR ELECTRODES. This circuit includes all switching connections between that device and the DEFIBRILLATOR ELECTRODES.		IEC 60601-2-4:2002
DISCHARGE CONTROL CIRCUIT	Circuit including the manually operated discharge controls and all parts conductively connected to them.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
DISCRETE-OPERATING MODE	Mode of operation of ULTRASONIC DIAGNOSTIC EQUIPMENT in which the purpose of the excitation of the ULTRASONIC TRANSDUCER or ULTRASONIC TRANSDUCER element group is to utilize only one diagnostic methodology.		IEC 60601-2-37:2001
DISINFECTABLE EQUIPMENT	EQUIPMENT parts which come into contact with the PATIENT during NORMAL USE and which may be disinfected in accordance with the MANUFACTURER'S instructions.		IEC 60601-2-9:1996
DISPLAY	Visual presentation of information.	rm-84-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 62083:2000
DIVERGING COLLIMATOR	Focused COLLIMATOR, the geometrical focal plane of which lies behind its entrance face.	rm-34-08	IEC 60789:1992
DOME	The means for hydraulically coupling the PATIENT'S blood pressure to the TRANSDUCER, where a TRANSDUCER external to the PATIENT is used.		IEC 60601-2-34:2000
DOSE AREA PRODUCT	Product of the area of the cross-section of an X-ray beam and the averaged AIR KERMA over that cross-section. The unit is the Gray square metre ($Gy \cdot m^2$). Dose area product rate, with the unit $Gy \cdot m^2 \cdot s^{-1}$; Dose area product (rate), used for brevity where either dose area product or dose area product rate apply, according to the context. NOTE The SI unit $Gy \cdot m^2$ may be expressed with a prefix, e.g. as $\mu Gy \cdot m^2$, to retain earlier used numeric dimensions of values displayed to the OPERATOR. **Recommended replacement: rm-13-54**		IEC 60601-2-43:2000
DOSE AREA PRODUCT	Letter symbol: $K \cdot A$. Product of the area of the USEFUL BEAM and the AIR KERMA over the cross-section of the USEFUL BEAM, both quantities being measured at the same distance from the FOCAL SPOT. The unit of DOSE AREA PRODUCT is Gym^2.	rm-13-54	IEC 60580:2000
DOSE AREA PRODUCT METER	EQUIPMENT which uses IONIZATION CHAMBERS for the measurement of DOSE AREA PRODUCT or DOSE AREA PRODUCT RATE in the beam of an X-ray machine used for diagnostic MEDICAL RADIOLOGICAL EXAMINATIONS. A DOSE AREA PRODUCT METER contains the following components: – IONIZATION CHAMBER; – MEASURING ASSEMBLY; – STABILITY CHECK DEVICE.	rm-51-09	IEC 60580:2000

Term	Definition	Reference	Used in IEC
DOSE AREA PRODUCT RATE	Letter symbol: $\dot{K} \cdot A$. Quotient of an increment of DOSE AREA PRODUCT by the corresponding increment of time. The unit of DOSE AREA PRODUCT RATE is Gym^2/s.	rm-13-55	IEC 60580:2000
DOSE EQUIVALENT	Letter symbol: *H*. Quantity used to express the RISK of the deleterious effects of IONIZING RADIATION upon living organisms, given by the product of *D*, *Q* and *N*, at the point of interest in tissue: *H* = *Q N D* where: *D* is the ABSORBED DOSE, *Q* is the quality factor and *N* is the product of any other modifying factors. The unit of DOSE EQUIVALENT is the joule per kilogram ($J.kg^{-1}$). The special name of the unit of DOSE EQUIVALENT is the sievert (Sv). The earlier unit of DOSE EQUIVALENT was the rem, 1 rem being equal to 10^{-2} $J.kg^{-1}$.	rm-13-24	IEC 60601-1-3:1994 IEC 60601-2-11:1997
DOSE EQUIVALENT LIMIT	Value, accumulated within a stated time, of effective dose equivalent to the body or of DOSE EQUIVALENT to parts of it, other than from natural IONIZING RADIATION and from IONIZING RADIATION due to medical procedures, which has been fixed as a limit for enforcement of RADIOLOGICAL PROTECTION.	rm-61-01	IEC 61331-3:1998
DOSE MONITOR UNIT	In a DOSE MONITORING SYSTEM, arbitrary unit in which a quantity is displayed and from which ABSORBED DOSE can be calculated.	rm-13-26	IEC 60601-2-1/A1:2002 IEC 60976/ A1:2000 IEC 62083:2000
DOSE MONITORING SYSTEM	System of devices for the measurement and display of a RADIATION QUANTITY directly related to the ABSORBED DOSE. It may include means for terminating IRRADIATION when a pre-selected value is reached.	rm-33-01	IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60976/ A1:2000
DOSE PROFILE	The representation of the dose as a function of position along a line.		IEC 60601-2-44:2002
DOSE PROFILE	Representation of the dose as a function of position along a line perpendicular to the TOMOGRAPHIC PLANE.		IEC 61223-2-6:1994
DOSE RATE MONITORING SYSTEM	System of devices for the measurement and display of a RADIATION QUANTITY directly related to the ABSORBED DOSE RATE.	rm-33-02	IEC 60601-2-1/A1:2002
DOSEMETER	RADIATION METER intended to measure the ABSORBED DOSE.	rm-50-02	IEC 60601-2-9:1996 IEC 60601-2-43:2000 IEC 61223-2-10:1999
DOSEMETER (PATIENT contact)	RADIATION METER used for the measurement on or in the PATIENT of ABSORBED DOSE, ABSORBED DOSE RATE, or any dose-related quantities in IONIZING RADIATION, such as EXPOSURE or KERMA. This EQUIPMENT usually consists of one or more RADIATION DETECTOR assemblies (for example CHAMBER assemblies) and a MEASURING ASSEMBLY.		IEC 60601-2-9:1996
DOSIMETER (diagnostic)	EQUIPMENT which uses IONIZATION CHAMBERS and/or semi-conductor detectors for the measurement of AIR KERMA, AIR KERMA LENGTH and/or KERMA, AIR KERMA RATE in the beam of an X-ray machine used for diagnostic MEDICAL RADIOLOGICAL EXAMINATIONS. A diagnostic DOSIMETER contains the following components: – one or more detector assemblies which may or may not be an integral part of the MEASURING ASSEMBLY; – a MEASURING ASSEMBLY; – one or more STABILITY CHECK DEVICES (optional).		IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
DOSIMETER (RADIOTHERAPY)	EQUIPMENT which uses IONIZATION CHAMBERS for the measurement of AIR KERMA, ABSORBED DOSE, or the corresponding rates, in PHOTON and ELECTRON radiation as used in radiation therapy. A RADIOTHERAPY DOSIMETER contains the following components: – one or more CHAMBER assemblies; – a MEASURING ASSEMBLY (including possibly a separate display device); – one or more STABILITY CHECK DEVICES (optional); – one or more PHANTOMS or build-up caps (optional).	rm-33-07	IEC 60601-2-9:1996 IEC 60731/A1:2002
DOUBLE EMULSION FILM	For use in DIRECT RADIOGRAPHY, RADIOGRAPHIC FILM covered with radiation-sensitive emulsion on both sides of its carrier.	rm-32-34	IEC 61223-2-1:1993
DOUBLE INSULATION	Insulation comprising both BASIC INSULATION and SUPPLEMENTARY INSULATION.	NG.03.04	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-51:2003
DRIFT	Change of the GAS READING of a RGM, for a given GAS LEVEL over a stated period of time, under REFERENCE CONDITIONS that remain constant.		IEC 60601-2-55:To be published
DRIP-RATE INFUSION CONTROLLER	INFUSION CONTROLLER in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT as a number of drops per unit of time.		IEC 60601-2-24:1998
DRIP-RATE INFUSION PUMP	INFUSION PUMP in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT as a number of drops per unit of time.		IEC 60601-2-24:1998
DUMMY COMPONENT	Test replacement for moulded components like transformers, semiconductors etc. The DUMMY COMPONENT has a geometry equal to that of the component it will replace during the TEST. The moulded volume does not incorporate parts of the original components (ex-semiconductor dye, transformer cores and windings). The DUMMY COMPONENT makes it possible to test creepage, clearance and dielectric strength with the correct geometry without exceeding the internal maximum voltage of the part being replaced.		IEC 60601-2-4:2002
DUTY CYCLE	Ratio of the operating time to the sum of the operating time and the ensuing interval. In the case of operating times and intervals of varying duration, it is calculated as a mean value over a sufficiently long time.	NG.10.05	IEC 60601-1:1988 IEC 60601-1/A2:1995
DUTY FACTOR	Ratio of the PULSE DURATION to the PULSE REPETITION PERIOD (see 5.3.2.4 of IEC 60469-1). [IEC 61689, definition 3.17]		IEC 60601-2-5:2000
DYNAMIC RANGE	Range of ATTENUATION that can be used for subtraction.		IEC 61223-3-3:1996

Term	Definition	Reference	Used in IEC
EARTH LEAKAGE CURRENT	Current flowing from the MAINS PART through or across the insulation into the PROTECTIVE EARTH CONDUCTOR.	NG.05.01	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
ECG RECORD	A registration (e.g. a hard copy write-out or a display) of an ECG signal including the associated data such as date and time of the registration, name and identification of the PATIENT, etc.		IEC 60601-2-51:2003
EDGE FILTER	FILTER whose ABSORPTION characteristic as a function of RADIATION ENERGY shows a discontinuity.	rm-35-05	IEC 60601-1-3:1994
EFFECTIVE APERTURE	The area of the INPUT SCREEN of the XRII which is irradiated by the RADIATION SOURCE through the INPUT APERTURE. NOTE Due to geometrical enlargement and the source size, the diameter of this area is always larger than the diameter of the INPUT APERTURE itself.		IEC 61262-5:1994
EFFECTIVE FOCAL SPOT	Perpendicular PROJECTION of the ACTUAL FOCAL SPOT on the REFERENCE PLANE. NOTE The shortened term FOCAL SPOT refers to the EFFECTIVE FOCAL SPOT (IEC 60806:1984).	rm-20-13	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60806:1984 IEC 61262-1:1994 IEC 61267:1994
EFFECTIVE IMAGE RECEPTION AREA	The term IMAGE RECEPTION AREA defined in IEC 60788 (rm-37-16) is taken in this collateral standard IEC 60601-1-3:1994 to include only those parts of the surface that are configured at the relevant time to be able to receive an X-RAY PATTERN and have at the same time appropriate means of processing for display or storage of the information contained. NOTE In accordance with this convention, the IMAGE RECEPTION AREA of a multi-field X-RAY IMAGE INTENSIFIER TUBE is considered to be restricted by the selection of magnification modes, to exclude any portion of the INPUT SCREEN from which the X-RAY PATTERN cannot be electronically processed.	rm-37-16	IEC 60601-1-3:1994
EFFECTIVE INTENSITY	Ratio of the OUTPUT POWER to the EFFECTIVE RADIATING AREA. It is expressed in watts per square centimetre. [IEC 61689, definition 3.18, modified]		IEC 60601-2-5:2000
EFFECTIVE LENGTH	Length along the axis of the CT DETECTOR between the two points at which the RESPONSE has fallen to 50 % of its maximum value (at the centre).		IEC 61674/A1:2002

Term	Definition	Reference	Used in IEC
EFFECTIVE RADIATED POWER (ERP)	Power required at the input of a lossless reference antenna to produce, in a given direction at any specified distance, the same power flux density as that radiated by a given device. NOTE As used by the ITU and as used in IEC 60050 (712), the term "effective radiated power" appears without qualification only when the reference antenna is a half-wave dipole. [IEV 161-04-16, modified]		IEC 60601-1-2:2001
EFFECTIVE RADIATING AREA	Beam cross-sectional area extrapolated to the front face of the TREATMENT HEAD and multiplied by a dimensionless factor according to IEC 61689. [IEC 61689, definition 3.20, modified] NOTE This may be thought of as the area of the face of the TREATMENT HEAD which contains 100 % of the total mean square acoustic power.		IEC 60601-2-5:2000
EFFECTIVE RANGE	Range of INDICATED VALUES for which an instrument complies with a stated performance. The maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range.		IEC 61676:2002
EFFECTIVE RANGE (of INDICATED VALUES)	Range of INDICATED VALUES for which an instrument complies with a stated performance, the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may also be applied to SCALE READINGS and to related quantities that are not directly indicated by the instrument, for example the input signal. NOTE 1 The EFFECTIVE RANGE of INDICATED VALUES is referred to as EFFECTIVE RANGE in this standard IEC 61674. NOTE 2 For CT DOSIMETERS the EFFECTIVE RANGE of AIR KERMA LENGTH need not be stated as the largest range of which is of practical interest to the USER, e.g. 1μGy·m to 2mGy·m.		IEC 61674/ A1:2002
EFFECTIVE RANGE (of INDICATED VALUES)	The range of INDICATED VALUES for which an instrument complies with a stated performance; the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may, for example, also be applied to SCALE READINGS and to related quantities not directly indicated by the instrument e.g. input current. NOTE Referred to as EFFECTIVE RANGE in this standard IEC 60731/A1:2002. **Recommended replacement: IEC 61674**		IEC 60731/A1:2002
EFFECTIVE RANGE (of INDICATED VALUES)	Range of INDICATED VALUES for which an instrument complies with a stated performance; the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may, for example, also be applied to SCALE READINGS and to related quantities that are not directly indicated by the instrument, e.g. input current. NOTE The EFFECTIVE RANGE of INDICATED VALUES is referred to as EFFECTIVE RANGE in this standard IEC 60580. **Recommended replacement: IEC 61674**		IEC 60580:2000
EFFECTIVE RECORDING WIDTH	Width of the recording paper within which the signal of a CHANNEL can be recorded according to this performance standard.		IEC 60601-2-51:2003
EFFECTIVE STIMULATION DURATION ($t_{s,eff}$)	Duration of any period of the monotonic increasing or decreasing gradient, used to describe its limits for cardiac or peripheral nerve stimulation. It is defined as the ratio of the peak-to-peak field variation and the maximum value of the time derivative of the gradient in that period.		IEC 60601-2-33:2002

Term	Definition	Reference	Used in IEC
EFFECTIVE SURFACE AREA	Surface on which the PATIENT rests according to the intended position and which is radiated by the PHOTOTHERAPY EQUIPMENT. NOTE The EFFECTIVE SURFACE AREA is the intended TREATMENT surface which is illuminated by the phototherapy light. The area of 60 cm x 30 cm is used as a standard sized surface unless specified differently in the ACCOMPANYING DOCUMENTS.		IEC 60601-2-50:2000
ELECTRICAL STIMULATOR	Parts of EQUIPMENT for the application of electric currents via ELECTRODES in direct contact with the PATIENT, for the evoking of biopotentials or other action.		IEC 60601-2-40:1998
ELECTRICALLY OPERATED HOSPITAL BED	BED and its accessories intended for use in the diagnosis, TREATMENT or monitoring of an adult PATIENT while under medical supervision.		IEC 60601-2-38 /A1:1999
ELECTROCARDIOGRAM (ECG)	Visible RECORD of heart action potentials.		IEC 60601-2-25/A1:1999 IEC 60601-2-26:2002
ELECTROCARDIOGRAM (ECG)	Visual RECORD of heart action potentials. [IEC 60601-2-25:1999, definition 2.101] **Recommendation: unify with IEC 60601-2-25**		IEC 60601-2-47:2001
ELECTROCARDIOGRAM (ECG)	Visible recording of heart action potentials as measured at the body surface (see also the definition of 'ECG RECORD'). **Recommendation: unify with IEC 60601-2-25**		IEC 60601-2-51:2003
ELECTROCARDIOGRAPH (ECG)	MEDICAL ELECTRICAL EQUIPMENT and associated ELECTRODES intended for the production of detachable ELECTROCARDIOGRAMS for diagnostic purposes. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999**		IEC 60601-2-25/A1:1999
ELECTROCARDIOGRAPH (ECG)	MEDICAL ELECTRICAL EQUIPMENT and associated ELECTRODES intended for the production of ELECTROCARDIOGRAMS for diagnostic purposes. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999**		IEC 60601-2-51:2003
ELECTROCARDIOGRAPHIC (ECG) MONITORING EQUIPMENT	EQUIPMENT and associated ELECTRODES for the monitoring and/or recording of heart action potentials and displaying the resultant data locally and/or transmitting to a central station. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999.**		IEC 60601-2-27:1994
ELECTRODE	ELECTRODE attached to a specified part of the body to detect heart action voltages in combination with another ELECTRODE or ELECTRODES. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999**		IEC 60601-2-25/A1:1999
ELECTRODE	Conductor attached to a specified part of the body to detect heart action voltages in combination with another ELECTRODE or ELECTRODES. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999**		IEC 60601-2-27:1994
ELECTRODE(S)	Means (typically, an electrical sensor) in contact with a specified part of the body to detect heart action voltage in combination with another means (see also Table 109). Both means (electrical sensors) are connected to the ELECTROCARDIOGRAPH via a PATIENT CABLE. **Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999**		IEC 60601-2-51:2003
ELECTROENCEPHALOGRAM (EEG)	Display or RECORD of the variation with time of voltages taken from ELECTRODES on the scalp, whose positions are specified. [IEV 891-04-23, modified]		IEC 60601-2-26:2002

Term	Definition	Reference	Used in IEC
ELECTROENCEPHALOGRAPH (EQUIPMENT)	Device to produce an ELECTROENCEPHALOGRAM. [IEV 891-04-24]	IEV 891-04-24	IEC 60601-2-26:2002
ELECTROMAGNETIC COMPATIBILITY (abbreviation EMC)	The ability of an EQUIPMENT or system to function satisfactorily in its ELECTROMAGNETIC ENVIRONMENT without introducing intolerable ELECTROMAGNETIC DISTURBANCES to anything in that environment (IEV 161-01-07).	IEV 161-01-07	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 62083:2000
ELECTROMAGNETIC COMPATIBILITY (EMC)	Ability of an EQUIPMENT or SYSTEM to function satisfactorily in its ELECTROMAGNETIC ENVIRONMENT without introducing intolerable ELECTROMAGNETIC DISTURBANCES to anything in that environment. [IEV 161-01-07]		IEC 60601-1-2:2001
ELECTROMAGNETIC DISTURBANCE	Any electromagnetic phenomenon which may degrade the performance of an EQUIPMENT and/or system (IEV 161-01-05, modified). NOTE An ELECTROMAGNETIC DISTURBANCE may be an electromagnetic NOISE, an unwanted signal or a change in the propagation medium itself.		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
ELECTROMAGNETIC DISTURBANCE	Any electromagnetic phenomenon that may degrade the performance of a device, EQUIPMENT or system. NOTE An ELECTROMAGNETIC DISTURBANCE may be an ELECTROMAGNETIC NOISE, an unwanted signal or a change in the propagation medium itself. [IEV 161-01-05, modified].		IEC 60601-1-2:2001
(ELECTROMAGNETIC) EMISSION	Phenomenon by which electromagnetic energy emanates from a source. [IEV 161-01-08]	IEV 161-01-08	IEC 60601-1-2:2001
ELECTROMAGNETIC ENVIRONMENT	Totality of electromagnetic phenomena existing at a given location. NOTE In general, the ELECTROMAGNETIC ENVIRONMENT is time dependent and its description may need a statistical approach. [IEV 161-01-01, modified]		IEC 60601-1-2:2001
ELECTROMAGNETIC NOISE	Time-varying electromagnetic phenomenon apparently not conveying information and which may be superimposed on or combined with a wanted signal. [IEV 161-01-02]	IEV 161-01-02	IEC 60601-1-2:2001
ELECTROMYOGRAPH	MEDICAL ELECTRICAL EQUIPMENT for the detection and analysis of biopotentials accompanying nerve and muscle action, originating either spontaneously, intentionally or by electrical or other stimulation.		IEC 60601-2-40:1998
ELECTRON	Stable elementary particle having an electric charge of ± 1,60219 x 10^{-19} C and a rest mass of 9,10956 x 10^{-31} kg.	rm-11-18	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997
ELECTRON BEAM APPLICATOR	BEAM LIMITING DEVICE for ELECTRON RADIATION BEAMS.		IEC 60601-2-1/A1:2002

Term	Definition	Reference	Used in IEC
ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER	X-RAY IMAGE INTENSIFIER incorporating an electro-optical vacuum device.	rm-32-40	IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ELECTROSTATIC DISCHARGE (ESD)	A transfer of electric charge between bodies of different electrostatic potential in proximity or through direct contact. (IEV 161-01-22).		IEC 60601-1-2:2001
EMERGENCY AIR INTAKE PORT	Dedicated intake port through which ambient air may be drawn when the supply of FRESH GAS is insufficient or absent. [ISO 4135:1995, definition 4.2.2 modified]		IEC 60601-2-12:2001
EMERGENCY FIELD SHUT DOWN UNIT	Device for de-energizing a superconducting or resistive magnet in case of an emergency situation.		IEC 60601-2-33:2002
EMERGENCY TROLLEY	Wheeled trolley intended to support and convey life-supporting and resuscitation EQUIPMENT for cardio-respiratory emergencies.	NG.12.14	IEC 60601-1:1988 IEC 60601-1/A2:1995
EMISSION (electromagnetic)	The phenomenon by which electromagnetic energy emanates from a source (IEV 161-01-08).		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
EMISSION COMPUTED TOMOGRAPHY (ECT)	Imaging method for the representation of the spatial distribution of incorporated RADIONUCLIDES in selected two-dimensional slice through the object.	rm-34-35	IEC 61675-1:1998 IEC 61675-2:1998
ENCLOSURE	Exterior surface of EQUIPMENT including: – all ACCESSIBLE METAL PARTS, knobs, grips and the like; – accessible shafts; – for the purpose of tests, metal foil, with specified dimensions, applied in contact with parts of the exterior surface made of material with low conductivity or made of insulating material.	NG.01.06	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
ENCLOSURE LEAKAGE CURRENT	Current flowing from the ENCLOSURE or from parts thereof, excluding APPLIED PARTS, accessible to the OPERATOR or PATIENT in NORMAL USE, through an external CONDUCTIVE CONNECTION other than the PROTECTIVE EARTH CONDUCTOR to earth or to another part of the ENCLOSURE.	NG.05.02	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002
ENDOSCOPE	An APPLIED PART of MEDICAL EQUIPMENT introduced into a PATIENT to provide an internal view or image for examination, diagnosis and/or therapy.		IEC 60601-2-18/ A1:2000
ENDOSCOPIC EQUIPMENT	An ENDOSCOPE together with its SUPPLY UNIT(S), as required for its intended use.		IEC 60601-2-18 /A1:2000
ENDOSCOPICALLY-USED ACCESSORY	An ACCESSORY, which may be the APPLIED PART of MEDICAL ELECTRICAL EQUIPMENT that is not ENDOSCOPIC EQUIPMENT, introduced into a PATIENT through the same orifice in the PATIENT as the ENDOSCOPE.		IEC 60601-2-18 /A1:2000
ENDOSCOPICALLY USED ACCESSORY	See definition in IEC 60601-2-18:1996. NOTE The reader is referred to IEC 60601-2-18 to ensure that a consistent definition is used.		IEC 60601-2-2:1998
ENERGY CALIBRATION	Process of establishing a relation between the window setting of the PULSE height analyzer and the energy of the PHOTONS.		IEC 61948-1:2001
ENERGY FLUENCE RATE	Letter symbol: ψ. Increment of energy fluence during a suitably small interval of time dt divided by that interval of time. $\psi = \frac{d\Psi}{dt}$	rm-13-05	IEC 60627:2001
ENERGY METER/DEFIBRILLATOR TESTER	An INSTRUMENT capable of measuring the energy output from a CARDIAC DEFIBRILLATOR while generating a simulated ECG output to the CARDIAC DEFIBRILLATOR.		IEC 60601-2-4:2002
ENERGY RESOLUTION	A term used to characterize the ability of a RADIATION DETECTOR to distinguish between PHOTONS of different energies. NOTE The ENERGY RESOLUTION can be expressed as the ratio of the photopeak FULLWIDTH AT HALF MAXIMUM (FWHM) to photopeak energy expressed as a percentage.		IEC 61948-1:2001
ENERGY STORAGE DEVICE	The component (for example a capacitor) that is charged with the energy necessary to deliver an electrical defibrillation PULSE to the PATIENT.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
ENTRANCE FIELD	For an XRII, the area in the ENTRANCE PLANE that can be used for the TRANSMISSION of an X-RAY PATTERN under specific conditions.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE FIELD	For a COLLIMATOR, area on the entrance face bounded by the shortest perimeter tangential to the outside edges of the peripheral apertures on its entrance face.	rm-34-12	IEC 61223-3-3:1996
ENTRANCE FIELD OF A COLLIMATOR	Area bounded by the shortest line which is tangential to the outside edges of the peripheral COLLIMATOR apertures on the COLLIMATOR FRONT FACE.		IEC 60789:1992
ENTRANCE FIELD SIZE	For an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, diameter of the field in the ENTRANCE PLANE that can be used for the TRANSMISSION of an X-RAY PATTERN under specific conditions.	rm-32-43	IEC 60601-2-43:2000 IEC 61223-3-3:1996
ENTRANCE FIELD SIZE	For an XRII, the diameter of the field in the ENTRANCE PLANE that can be used at a specified SED for the TRANSMISSION of an X-RAY PATTERN. For an XRII with more than one magnification mode, the ENTRANCE FIELD SIZE for each of the magnification modes shall correspond to the same diameter of the XRII OUTPUT IMAGE occurring with the largest ENTRANCE FIELD SIZE. **Recommended replacement: rm-32-43**		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE PLANE	For AN ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, plane perpendicular to its axis of symmetry and grazing the part which protrudes most in the direction of the RADIATION SOURCE.	rm-32-42	IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996
ENTRANCE PLANE	The plane perpendicular to the axis of symmetry of the XRII and grazing the part of the XRII, including its housing, that protrudes most in the direction of the RADIATION SOURCE. **Recommended replacement: rm-32-42**		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE SURFACE	In RADIOLOGY, plane or curved surface through which the radiation enters an irradiated object including any bolus which is present.	rm-37-17	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-2-7:1999 IEC 61223-2-11:1999 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
EQUILIBRATION TIME	The time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value after a sudden change in an INFLUENCE QUANTITY has been applied to the instrument.		IEC 60731/A1:2002
EQUILIBRATION TIME	Time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value, after a sudden change in an INFLUENCE QUANTITY has been applied to the instrument. **Recommended replacement: IEC 60731/A1:2002**		IEC 61674/ A1:2002
EQUIPMENT	(see NG.02.15)	NG.02.11	IEC 60522:1999 IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 62083:2000
EQUIPMENT ELECTRODE	Conductor applied over, or inserted into, a region of the scalp or brain to detect electrical ACTIVITY of the brain in combination with another ELECTRODE or ELECTRODES.		IEC 60601-2-26:2002
EQUIPMENT FOR EXTRACORPOREALLY INDUCED LITHOTRIPSY	Device for TREATMENT with extracorporeally generated PRESSURE PULSES.		IEC 60601-2-36:1997
EQUIPMENT MODEL/EQUIPMENT MODELLING	All physical, geometric and radiation parameters required to plan a course of RADIOTHERAPY for particular EQUIPMENT. The process of establishing the EQUIPMENT model is referred to as "EQUIPMENT MODELLING".		IEC 62083:2000
EQUIVALENT ANODE INPUT POWER	Value of ANODE INPUT POWER which, if applied continuously under specified ambient conditions, would maintain a specific level of ANODE HEAT CONTENT.	rm-36-24	IEC 60613:1989

Term	Definition	Reference	Used in IEC
EQUIVALENT APERTURE DIAMETER	Diameter of a circle whose area is the –12 dB OUTPUT BEAM AREA and given by $D_{eq} \equiv \sqrt{\frac{4}{\pi}} A_{aprt}$ where A_{aprt} is the –12 dB OUTPUT BEAM AREA. Symbol: D_{eq}. Unit: centimetres, cm. NOTE This formula gives the diameter of a circle whose area is the –12 dB OUTPUT BEAM AREA. It is used in the calculation of the CRANIAL-BONE THERMAL INDEX and the SOFT TISSUE THERMAL INDEX.		IEC 60601-2-37:2001
EQUIVALENT BEAM AREA	Value of the area of the acoustic beam at the distance z in terms of power and intensity, and given by $A_{eq}(z) \equiv \frac{P_{\alpha}(z)}{I_{zpta,\alpha}(z)} = \frac{P}{I_{zpta}(z)}$ where $P_{\alpha}(z)$ is the ATTENUATED OUTPUT POWER, at the distance z, in milliwatts, $I_{zpta,\alpha}(z)$ is he ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at the distance z, in milliwatts per square centimetre, P is the OUTPUT POWER in milliwatts, $I_{zpta}(z)$ is the SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at the distance z, in milliwatts per square centimetre, and z is the distance from the source to the specified point in centimetres. Symbol: $A_{eq}(z)$. Unit: centimetres squared, cm^2.		IEC 60601-2-37:2001
EQUIVALENT BEAM DIAMETER	Value of the diameter of the acoustic beam at the distance z in terms of the EQUIVALENT BEAM AREA, and given by $d_{eq}(z) \equiv \sqrt{\frac{4}{\pi} A_{eq}(z)}$ where $A_{eq}(z)$ is the EQUIVALENT BEAM AREA; z is the distance from the source to the specified point. Symbol: $d_{eq}(z)$. Unit: centimetres, cm.		IEC 60601-2-37:2001
EQUIVALENT WIDTH (EW)	Width of that rectangle having the same area and the same height as the RESPONSE function, e.g. the POINT SPREAD FUNCTION.	rm-34-45	IEC 61675-1:1998 IEC 61675-2:1998
EQUIVALENT WIDTH (EW)	The width of a rectangle having the same area as the LSF and a height equal to the maximum value of the LSF. **Recommended replacement: IEC 61675-1:1998, IEC 61675-2:1998**		IEC 60789:1992
ERROR OF MEASUREMENT	Difference between the MEASURED VALUE of a quantity and the TRUE VALUE of that quantity.		IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
ERROR OF MEASUREMENT	The difference remaining between the MEASURED VALUE of a quantity and the TRUE VALUE of that quantity.		IEC 60731/A1:2002
ESSENTIAL PERFORMANCE (of an EQUIPMENT or SYSTEM)	PERFORMANCE CHARACTERISTICS necessary to maintain the RESIDUAL RISK within acceptable limits. NOTE See also 3.201.2. This definition will be inserted in the 3rd edition of IEC 60601-1 (in preparation).		IEC 60601-1-2:2001
ESTABLISHED CRITERIA	In a QUALITY ASSURANCE PROGRAMME, acceptable VARIATIONS in results of a CONSTANCY TEST which signal satisfactory functional performance of the EQUIPMENT tested.	rm-70-04	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
EVOKED RESPONSE EQUIPMENT	MEDICAL ELECTRICAL EQUIPMENT for the detection and analysis of biopotentials resulting from an evoking stimulus. The stimulus may be electrical, tactile, auditory, visual, olfactory etc.		IEC 60601-2-40:1998
EXAMINATION ROOM	In MEDICAL DIAGNOSTIC RADIOLOGY, room in which IONIZING RADIATION is applied to the PATIENT or measured on the PATIENT, and which has the required structural means for RADIATION PROTECTION and for mechanical support.	rm-20-22	IEC 60601-2-7:1998 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61331-3:1998
EXCLUSION BAND	Frequency band for intentional receivers of RF electromagnetic energy that extends from – 5 % to + 5 % of the frequency, or frequency band, of reception for frequencies of reception greater than or equal to 80 MHz and from –10 % to + 10 % of the frequency, or frequency band, of reception for frequencies of reception less than 80 MHz. NOTE Other definitions of this term are sometimes used for other purposes in national radio regulations.		IEC 60601-1-2:2001
EXIT FIELD OF A COLLIMATOR	Area bounded by the shortest line which is tangential to the outside edges of the peripheral COLLIMATOR apertures on the COLLIMATOR BACK FACE.		IEC 60789:1992
EXIT SURFACE	In RADIOLOGY, plane or curved surface through which the RADIATION BEAM emerges from an irradiated object.		IEC 61267:1994
EXPANDED UNCERTAINTY	Quantity defining the interval about the result of a measurement within which the values that could reasonably be attributed to the measure and may be expected to lie with a higher degree of confidence.	rm-73-15	IEC 60580:2000 IEC 61674/A1:2002

Term	Definition	Reference	Used in IEC
EXPOSURE	Letter symbol: *X*. Electric charge produced by IONIZING RADIATION in air. EXPOSURE is determined as the quotient of d*Q* by d*m*, where the value of d*Q* is the absolute value of the total charge of the ions of one sign produced in air when all the ELECTRONS (negatrons and positrons) liberated by PHOTONS in air of mass d*m* are completely stopped in air: $X = \frac{dQ}{dm}$ The unit of EXPOSURE is the coulomb per kilogram ($C \cdot kg^{-1}$). The earlier unit of EXPOSURE was the roentgen (R), being equal to $2{,}58 \times 10^{-4}$ $C \cdot kg^{-1}$.	rm-13-14	IEC 60601-1-3:1994 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1993 IEC 61223-3-1:1999
EXPOSURE	Letter symbol: *X*. Following the definition in C.8 of ICRU 33 EXPOSURE is the quotient of d*Q* by d*m* where d*Q* is the absolute value of the total charge of the ions of one sign produced in air when all the ELECTRONS (negatrons and positrons) liberated by PHOTONS in air of mass d*m* are completely stopped in air. The unit of EXPOSURE is $C \cdot kg^{-1}$. **Recommended replacement: rm-13-14**		IEC 60731/A1:2002
EXPOSURE RATE	Letter symbol: $\dot{X}$. EXPOSURE per unit time. EXPOSURE RATE is determined as the quotient of d*X* by d*t*, where d*X* is the increment of EXPOSURE in the time interval d*t*: $\dot{X} = \frac{dX}{dt}$ A unit of EXPOSURE RATE is any quotient of the unit of EXPOSURE or its multiples or submultiples by a suitable unit of time ($C \cdot kg^{-1} \cdot s^{-1}$, $mC \cdot kg^{-1} \cdot h^{-1}$, etc.).	rm-13-15	IEC 60601-1-3:1994 IEC 61223-2-9:1999 IEC 61262-2:1994
EXPOSURE RATE	Letter symbol: $\dot{X}$. Following the definition in C.9 of ICRU 33 EXPOSURE RATE is the quotient of d*X* by d*t*, where d*X* is the increment of EXPOSURE in the time interval d*t*. The unit of EXPOSURE RATE is $C \cdot kg^{-1} \cdot s^{-1}$ ($C \cdot kg^{-1} \cdot min^{-1}$; $C \cdot kg^{-1} \cdot h^{-1}$). **Recommended replacement: rm-13-15**		IEC 60731/A1:2002
EXTERNAL PACEMAKER	Pacemaker with a NON-IMPLANTABLE PULSE GENERATOR and PATIENT CABLE(S) (if used).		IEC 60601-2-31/A1:1998
EXTERNAL TERMINAL DEVICE	TERMINAL DEVICE by which electrical connection to other EQUIPMENT is made.	NG.07.07	IEC 60601-1:1988 IEC 60601-1/A2:1995
EXTRA-FOCAL RADIATION	In an X-ray source assembly, X-radiation emitted from the RADIATION SOURCE other than that emitted from the ACTUAL FOCAL SPOT.	rm-11-11	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60627:2001 IEC 61223-3-2:1996
EXTRACORPOREAL CIRCUIT	Blood lines and any integral ACCESSORY thereof.		IEC 60601-2-16:1998
EXTRACORPOREALLY INDUCED LITHOTRIPSY	LITHOTRIPSY inside the PATIENT by PRESSURE PULSES generated outside the PATIENT.		IEC 60601-2-36:1997
FAIL SAFE	Capability of an EQUIPMENT to provide a minimum illuminance and to be directed on the operation area even in SINGLE FAULT CONDITION.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
FIELD FLATTENING FILTER	FILTER used to homogenize the ABSORBED DOSE RATE over the RADIATION FIELD.	rm-35-07	IEC 60601-2-11:1997 IEC 60601-2-1/A1:2002 IEC 60976/ A1:2000
FIELD SIZE	Abbreviation for IRRADIATION FIELD SIZE.		IEC 60601-2-11:1997
FIELD-CLASS DOSIMETER	Dosimeter whose performance and stability are sufficient for it to be used to make ordinary routine measurements.	rm-71-05	IEC 60601-2-9:1996 IEC 60731/A1:2002
FILAMENT CURRENT	For an X-RAY TUBE, electric current applied to the filament for control of the thermionic emission from the CATHODE.	rm-36-08	IEC 60613:1989
FILM BASE PLUS FOG DENSITY	For CONSTANCY TESTS in X-RAY EQUIPMENT, the optical density in an area of the RADIOGRAM, on the processed control film, that has not been exposed to light from a sensitometer.	rm-72-04	IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
FILM CHANGER	SERIAL CHANGER in which each RECORD is taken upon a separate RADIOGRAPHIC FILM not contained in an individual RADIOGRAPHIC CASSETTE.	rm-31-07	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-3-1:1999
FILM ILLUMINATOR	Luminous surface in combination with additional provisions for the observation of transparent objects such as RADIOGRAMS on RADIOGRAPHIC FILM.	rm-70-10	IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999
FILM PROCESSOR	For use in MEDICAL DIAGNOSTIC RADIOLOGY, a combination of EQUIPMENT and device to process the latent RADIOLOGICAL information, recorded on, or transferred to, radiographic material, into a permanent, visible image.	rm-70-11	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999

Term	Definition	Reference	Used in IEC
FILTER	In RADIOLOGICAL EQUIPMENT, material or device provided to effect FILTRATION of the RADIATION BEAM.	rm-35-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976/ A1:2000 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-5:1994
FILTER(S)	Means, realised in hardware, firmware or software, to attenuate unwanted components in the signal being recorded, e.g. muscle action voltages in ECG signal.		IEC 60601-2-51:2003
FILTRATION	Modification of characteristics of IONIZING RADIATION on passing through matter. NOTE FILTRATION may be: – preferential ABSORPTION of certain components of polyenergetic X or gamma radiation accompanying its ATTENUATION; – a modification of the distribution of radiation intensity over the cross-section of a RADIATION BEAM.	rm-12-11	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61331-3:1998
FILTRATION	Modification of characteristics of IONIZING RADIATION on passing through matter. NOTE FILTRATION includes: – modification of the energy spectrum of IONIZING RADIATION by preferential ABSORPTION of components; – modification of the spatial distribution of radiation intensity over the cross section of a RADIATION BEAM, by differential ATTENUATION. **Recommended replacement: rm-12-11**		IEC 60580:2000
FIRST LEVEL CONTROLLED OPERATING MODE	Mode of operation of the MR EQUIPMENT in which one or more outputs reach a value that may cause physiological stress to PATIENTS which needs to be controlled by MEDICAL SUPERVISION.		IEC 60601-2-33:2002
FIXED COORDINATE SYSTEM	Cartesian system with axes *X*, *Y*, and *Z*, *Z* being the SYSTEM AXIS. The origin of the FIXED COORDINATE SYSTEM is defined by the centre of the TOMOGRAPHIC VOLUME. The SYSTEM AXIS is orthogonal to all transverse slices.		IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
FIXED EQUIPMENT	EQUIPMENT which is fastened or otherwise secured at a specified location in a building or a vehicle and can only be detached by means of a TOOL.	NG.02.12	IEC 60601-1:1988 IEC 60601-1/A2:1995
FIXED MAINS SOCKET OUTLET	Mains socket-outlet installed in a fixed wiring system in a building or a vehicle. According to IEC 60601-1/A1:1991 modify title in IEC 60601-1:1988 to read: Fixed mains socket-outlet	NG.07.08	IEC 60601-1:1988 IEC 60601-1/A1:1991 IEC 60601-1/A2:1995
FIXED SETTING (of a control or limiting device)	Setting not intended to be altered by the OPERATOR and which can only be altered by means of a TOOL.	NG.09.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
FLAMMABLE ANAESTHETIC MIXTURE WITH AIR	Mixture of a flammable anaesthetic vapour with air in such a concentration that ignition may occur under specified conditions. A mixture of the vapour of a flammable disinfection or cleaning agent with air may be treated as a FLAMMABLE ANAESTHETIC MIXTURE with air subject to national or local regulations.	NG.12.15	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999
FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE	Mixture of a flammable anaesthetic vapour with oxygen or with nitrous oxide in such a concentration that ignition may occur under specified conditions.	NG.12.16	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999
FLOW-DIRECTION-SENSITIVE COMPONENT	VENTILATOR component through which the gas flow has to be in one direction only for its proper functioning and/or PATIENT SAFETY. [ISO 4135:1995, definition 4.1.13]		IEC 60601-2-12:2001
FLUORESCENT SCREEN	Layer of a fluorescent substance on a carrier, emitting light when irradiated with IONIZING RADIATION.	rm-32-30	IEC 60601-1-3:1994 IEC 60627:2001 IEC 61331-2:1994
FOCAL RADIATION	In an X-ray source assembly, X-radiation emitted from the ACTUAL FOCAL SPOT.	rm-11-10	IEC 60627:2001

Term	Definition	Reference	Used in IEC
FOCAL SPOT	Shortened term (see EFFECTIVE FOCAL SPOT).	rm-20-13s	IEC 60336:1993 IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
FOCAL SPOT PINHOLE RADIOGRAM	RADIOGRAM obtained by means of a PINHOLE CAMERA, showing the shape and orientation of an EFFECTIVE FOCAL SPOT, and the spatial distribution of intensity of radiation across it.	rm-72-02	IEC 60336:1993
FOCAL SPOT SLIT RADIOGRAM	RADIOGRAM obtained by means of a SLIT CAMERA, showing the distribution, across an EFFECTIVE FOCAL SPOT, in the direction normal to the length of the slit, of the intensity of the radiation emitted.	rm-72-01	IEC 60336:1993
FOCAL SPOT STAR RADIOGRAM	Radiogram obtained by means of a STAR PATTERN CAMERA for the determination of the STAR PATTERN RESOLUTION LIMIT in one or more directions across an EFFECTIVE FOCAL SPOT.	rm-72-03	IEC 60336:1993

Term	Definition	Reference	Used in IEC
FOCAL SPOT TO IMAGE RECEPTOR DISTANCE	Distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to the point at which the REFERENCE AXIS intersects with the image receptor plane.	rm-37-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996
FOCAL SPOT TO SKIN DISTANCE	In MEDICAL DIAGNOSTIC RADIOLOGY, distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to a plane normal to the REFERENCE DIRECTION and containing the point on the PATIENT SURFACE nearest to the RADIATION SOURCE. In RADIOTHERAPY, distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to the point at which the REFERENCE AXIS intersects with the ENTRANCE SURFACE.	rm-37-12	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-3-4:2000
FOCAL TRACK	In a rotating ANODE X-RAY TUBE, part of the ANODE which is struck by the beam of ELECTRONS during rotation of the ANODE.	rm-22-08	IEC 60336:1993 IEC 60806:1984
FOCAL VOLUME	Volume in space contained within the surface defined by the –6 dB isobar of the maximum peak compressional acoustic pressure.		IEC 60601-2-36:1997
FOCUSED GRID	LINEAR GRID where the planes of the absorbing strips converge at the FOCUSING DISTANCE to a straight line.	rm-32-09	IEC 60601-2-7:1998 IEC 61223-3-1:1999
FOCUSED GRID	LINEAR GRID in which the planes of the absorbing strips converge to a straight line at the FOCUSING DISTANCE. **Recommended replacement: rm-32-09**		IEC 60627:2001
FOCUSING DISTANCE	Letter symbol: f_0, unit: cm. Distance between the incident face of a FOCUSED GRID and the line into which the planes of the absorbing strips of the grid converge. NOTE Attention is drawn to the differences between FOCUSING DISTANCE, FOCAL SPOT to grid distance and "FOCAL SPOT to film distance".		IEC 60627:2001
FREE FLOW	Flow in an ADMINISTRATION SET which is not controlled by the EQUIPMENT, for example, due to the unintended effects of gravity by the removal of the ADMINISTRATION SET from the EQUIPMENT.		IEC 60601-2-24:1998
FREQUENT USE DEFIBRILLATOR	Term used to describe a DEFIBRILLATOR designed to endure more than 2 500 discharges.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
FRESH GAS	Gas supplied to the VENTILATOR BREATHING SYSTEM. It excludes the following: – air drawn through the EMERGENCY AIR INTAKE PORT; – air drawn through leaks in the VENTILATOR BREATHING SYSTEM; – expired gas from the PATIENT.		IEC 60601-2-12:2001
FRESH GAS INTAKE PORT	Intake port, other than the EMERGENCY AIR INTAKE PORT, through which FRESH GAS may be drawn into the VENTILATOR BREATHING SYSTEM. [ISO 4135:1995, definition 4.2.6 modified]		IEC 60601-2-12:2001
FRONT POINTER	Luminous or mechanical device intended to indicate the RADIATION BEAM AXIS and its point of entry into the PATIENT.	rm-35-12	IEC 60976 /A1:2000
F-TYPE ISOLATED (floating) APPLIED PART (hereinafter referred to as F-type APPLIED PART)	APPLIED PART isolated from other parts of the EQUIPMENT to such a degree that no current higher than the PATIENT LEAKAGE CURRENT allowable in SINGLE FAULT CONDITION flows if an unintended voltage originating from an external source is connected to the PATIENT, and thereby applied between the APPLIED PART and earth. F-type APPLIED PARTS are either TYPE BF APPLIED PARTS or TYPE CF APPLIED PARTS.	NG.01.07	IEC 60601-1:1998 IEC 60601-1/A2:1995 IEC 60601-2-47:2001 IEC 60601-2-51:2003
FULL SOFTWARE CONTROL OF ACOUSTIC OUTPUT	Means by which the EQUIPMENT establishes values of the acoustic output quantities independent of direct OPERATOR control.		IEC 60601-2-37:2001
FULLWIDTH AT HALF MAXIMUM (FWHM)	For a bell shaped curve, distance parallel to the abscissa axis between the points where the ordinate has half of its maximum value.	rm-73-02	IEC 60601-2-44:2002 IEC 60789:1992 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998
FULL WIDTH AT TENTH MAXIMUM (FWTM)	For a bell shaped curve, distance parallel to the abscissa axis between the points where the ordinate has one tenth of its maximum value.	rm-73-03	IEC 60789:1992
FUNCTION (OF AN EQUIPMENT OR SYSTEM)	Clinically significant feature that the EQUIPMENT or SYSTEM is intended to provide.		IEC 60601-1-2:2001
FUNCTIONAL EARTH CONDUCTOR	Conductor to be connected to a FUNCTIONAL EARTH TERMINAL.	NG.06.03	IEC 60601-1:1988 IEC 60601-1/A2:1995
FUNCTIONAL EARTH TERMINAL	Terminal directly connected to a point of a measuring supply or control circuit or to a screening part which is intended to be earthed for functional purposes.	NG.06.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
GAMMA CAMERA	EQUIPMENT for scintigraphy, which produces an image by simultaneous detection of radiation emitted from the object.	rm-34-03	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998
GAMMA CAMERA BASED WHOLEBODY IMAGING SYSTEM	EQUIPMENT for scintigraphy, employing one or two DETECTOR HEAD(S), in which the image is formed by moving the DETECTOR HEAD(S) and the object relative to each other and relating output information of the RADIOLOGICAL IMAGE.		IEC 61675-3:1998
GANTRY	That part of the EQUIPMENT supporting the RADIATION HEAD.	rm-30-04	IEC 60601-2-1/A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
GANTRY	That part of the EQUIPMENT supporting and allowing possible movements of the RADIATION HEAD. **Recommended replacement: IEC 60601-2-1:2002**		IEC 60601-2-11:1997
GANTRY	In EQUIPMENT for RADIOTHERAPY, part of the EQUIPMENT supporting and allowing possible movements of the RADIATION HEAD. **Recommended replacement: IEC 60601-2-1:2002**		IEC 60601-2-29:1999 IEC 60976/A1:2000 IEC 61217:2002
GAS CONCENTRATION	Volume fraction of the gas expressed as a percentage referred to dry conditions and constant barometric pressure.		IEC 60601-3-1:1996
GAS EXHAUST PORT	That port of a VENTILATOR from which gas is discharged to the atmosphere either directly or via a gas scavenging system. [ISO 4135:1995, definition 4.2.7]		IEC 60601-2-12:2001
GAS INTAKE PORT	Port through which gas is drawn into the VENTILATOR BREATHING SYSTEM.		IEC 60601-2-12:2001
GAS OUTPUT PORT	Port through which gas is delivered at RESPIRATORY PRESSURES via the inspiratory limb to the PATIENT CONNECTION PORT. [ISO 4135:1995, definition 4.2.8 modified]		IEC 60601-2-12:2001
GAS RETURN PORT	Port through which gas is returned at RESPIRATORY PRESSURES via the expiratory limb from the PATIENT CONNECTION PORT. [ISO 4135:1995, definition 4.2.9 modified]		IEC 60601-2-12:2001
GEOMETRICAL FIELD SIZE	Geometrical PROJECTION as seen from the centre of the front surface of the RADIATION SOURCE on a plane perpendicular to the axis of the beam of the distal end of the BEAM LIMITING DEVICE. The field is thus of the same shape as the aperture of the BEAM LIMITING DEVICE. The GEOMETRICAL FIELD SIZE may be defined at any distance from the VIRTUAL SOURCE.		IEC 60976/ A1:2000
GEOMETRICAL FIELD SIZE	Geometrical projection of the distal end of the BEAM LIMITING DEVICE on a plane orthogonal to the RADIATION BEAM AXIS, as seen from the centre of the front surface of the RADIATION SOURCE. The RADIATION FIELD is thus of the same shape as the aperture of the BEAM LIMITING DEVICE. The GEOMETRICAL FIELD SIZE may be defined at any distance from the RADIATION SOURCE. **Recommended replacement: IEC 60976**		IEC 60601-2-11:1997
GEOMETRICAL RADIATION FIELD	Geometrical projection of the distal end of the BEAM LIMITING DEVICE on a plane orthogonal to the REFERENCE AXIS, as seen from the centre of the front surface of the TARGET/ELECTRON radiation window. The geometrical RADIATION FIELD may be defined at any distance from the front surface of the TARGET for X-RADIATION, or from the ELECTRON radiation window for ELECTRON radiation.		IEC 60601-2-1/A1:2002
GRADIENT OUTPUT	Parameter characterizing gradient performance such as rate of change of the magnitude of the magnetic field, or electric field induced by one or more GRADIENT UNITS under specified conditions and at a specified position.		IEC 60601-2-33:2002
GRADIENT UNIT	All gradient coils and amplifiers that together generate a magnetic field gradient along one of the axes of the coordinate system of the MR EQUIPMENT.		IEC 60601-2-33:2002
GRID EXPOSURE FACTOR	Letter symbol: *B*. For an ANTI-SCATTER GRID, ratio of the INDICATED VALUE of the rate of total RADIATION without the ANTI-SCATTER GRID in a specified beam to that with the ANTI-SCATTER GRID placed in the beam, under specific measuring conditions.	rm-32-26	IEC 61223-3-3:1996

Term	Definition	Reference	Used in IEC
GRID EXPOSURE FACTOR	Letter symbol: *B*. Characteristic of an ANTI-SCATTER GRID, evaluated as the ratio of the MEASURED VALUE of the quantity or rate of total RADIATION without the ANTI-SCATTER GRID in a RADIATION BEAM to that with the ANTI-SCATTER GRID placed in the beam, under specific measuring conditions. **Recommended replacement: rm-32-26**		IEC 60627:2001
GRID RATIO	Letter symbol: *r*. Ratio between the height of the absorbing strips and the distance between the absorbing strips in the centre of a LINEAR GRID.		IEC 60627:2001
GRID SELECTIVITY	Letter symbol: Σ. Characteristic of an ANTI-SCATTERED GRID, evaluated as the ratio of the TRANSMISSION OF PRIMARY RADIATION to the TRANSMISSION OF SCATTERED RADIATION, under specific measuring conditions.		IEC 60627:2001
HAEMODIALYSIS, HAEMODIAFILTRATION AND/OR HAEMOFILTRATION EQUIPMENT	A system or combination of units used to perform HAEMODIALYSIS, HAEMODIAFILTRATION and/or HAEMOFILTRATION (also refer to 2.2.15).		IEC 60601-2-16:1998
HAEMODIALYSIS (HD)	Process whereby solute imbalances in a PATIENT'S blood are corrected, mainly by diffusion across a semi-permeable membrane. NOTE This process normally includes fluid removal.		IEC 60601-2-16:1998
HAEMOFILTRATION (HF)	A process whereby solute imbalances of a PATIENT'S blood are corrected, mainly by FILTRATION across a semi-permeable membrane. NOTE This process includes fluid exchange and normally fluid removal.		IEC 60601-2-16:1998
HAEMODIAFILTRATION (HDF)	A process whereby solute imbalances in a PATIENT'S blood are corrected by means of simultaneous FILTRATION and diffusion across a semi-permeable membrane. NOTE This process includes fluid exchange and normally fluid removal.		IEC 60601-2-16:1998
HALF VALUE LAYER TEST DEVICE	Device of known X-RAY ATTENUATION properties, normally shaped as foil or plate, which, when applied in the proper thickness, attenuates AIR KERMA RATE to one half of the value that is measured without the device.		IEC 61267:1994
HALF-VALUE LAYER	Thickness of a specified material which attenuates under NARROW BEAM CONDITIONS X- radiation or gamma radiation with a particular RADIATION ENERGY or with a particular spectrum to an extent such that the KERMA RATE, EXPOSURE RATE or ABSORBED DOSE RATE is reduced to one half of the value that is measured without the material. The HALF-VALUE LAYER is expressed in suitable submultiples of the metre together with the material.	rm-13-42	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994

Term	Definition	Reference	Used in IEC
HALF-VALUE LAYER	Thickness of a specified material which under NARROW BEAM CONDITIONS attenuates PHOTON radiation according to its energy spectrum to an extent such that the AIR KERMA RATE is reduced to one half of the value that is measured without the material. **Recommended replacement: rm-13-42**		IEC 60580:2000
HAND-HELD EQUIPMENT	EQUIPMENT intended to be supported by the hand during NORMAL USE.	NG.02.13	IEC 60601-1:1988 IEC 60601-1/A2:1995
HARD COPY CAMERA	Device producing non-erasable images on a sheet of material from an input signal provided by an imaging system. NOTE Definition from IEC 61223-2-5: IMAGE display device: Device capable of displaying images from an input signal provided by an imaging system.	rm-80-07	IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-3:1996
HARD-WIRED	Term used where the features of a system can be modified only by physically removing and re-routing wires.		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
HARM	Physical injury or damage to the health of people, or damage to property or the environment. [ISO/IEC Guide 51:1999, definition 3.1]		ISO 14971:2000
HAZARD	Potential source of HARM. [ISO/IEC Guide 51:1999, definition 3.5]		ISO 14971:2000
HAZARD ANALYSIS	Identification of hazards and their initiating causes. NOTE The quantification of hazard is not a part of the HAZARD ANALYSIS.		IEC 60601-1-4:2000
HAZARDOUS SITUATION	Circumstance in which people, property or the environment are exposed to one or more hazard(s). [ISO/IEC Guide 51:1999, definition 3.6]		ISO 14971:2000
HEAD/FOOT PANEL ASSEMBLY	Assemblies mounted to BED end which may be used as handles to push the BED.		IEC 60601-2-38 /A1:1999
HEAD RF TRANSMIT COIL	A VOLUME RF TRANSMIT COIL suitable for use in MR EQUIPMENT for a MAGNETIC RESONANCE EXAMINATION of the head of PATIENTS.		IEC 60601-2-33:2002
HEAD SAR	SAR averaged over the mass of the PATIENTS head and over a specified time.		IEC 60601-2-33:2002
HEATING DEVICE	EQUIPMENT intended to supply heat to the whole or part of the body of a PATIENT by means of heated BLANKETS, PADS, MATTRESSES, and fluid-filled MATTRESSES.		IEC 60601-2-35:1996
HIGH FREQUENCY SURGICAL EQUIPMENT; HF SURGICAL EQUIPMENT	MEDICAL ELECTRICAL EQUIPMENT including its associated ACCESSORIES intended for the performance of surgical operations, such as the CUTTING or COAGULATION of biological tissue by means of high frequency (HF) currents.		IEC 60601-2-2:1998 IEC 60601-2-18/A1:2000
HIGH HEAT TRANSFER	Thermal characteristic of a HEATING DEVICE as determined according to Annex CC or Annex DD.		IEC 60601-2-35:1996
HIGH PRESSURE GAS INPUT PORT	Input port to which gas may be supplied at a PRESSURE greater than 100 kPa. [ISO 4135:1995, definition 4.2.10 modified]		IEC 60601-2-12:2001

Term	Definition	Reference	Used in IEC
HIGH VOLTAGE	Any voltage over 1 000 V a.c. or over 1 500 V d.c. or 1 500 V peak value.	NG.04.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
HIGH-CONTRAST RESOLUTION	See SPATIAL RESOLUTION		IEC 61223-2-6:1994
HIGH-VOLTAGE CABLE CONNECTION	EQUIPMENT designed for use in RADIOLOGY.	rm-20-18	IEC 60601-2-7:1998
HIGH-VOLTAGE GENERATOR	In an X-RAY GENERATOR, combination of all components for control and production of the electrical energy to be supplied to an X-RAY TUBE, usually consisting of a HIGH-VOLTAGE TRANSFORMER ASSEMBLY and a control assembly.	rm-21-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
HIGH-VOLTAGE TRANSFORMER ASSEMBLY	In a HIGH-VOLTAGE GENERATOR, assembly of the high-voltage transformer and other high-voltage circuit components.	rm-21-15	IEC 60601-2-8:1999
HYDRAULIC TEST PRESSURE	PRESSURE applied to test a vessel or part of it for compliance with Clause 45 of IEC 60601-1:1988.	NG.11.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
IEC 60601 TEST LEVEL	IMMUNITY TEST LEVEL specified in 36.202 by this standard or a Particular Standard.		IEC 60601-1-2:2001
IMAGE DISPLAY DEVICE	Device capable of displaying images from an input signal provided by an imaging system. NOTE Definition from IEC 61223-2-4: HARD COPY CAMERA: Device producing non-erasable images on a sheet of material from an input signal provided by an imaging system.	rm-80-08	IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996
IMAGE DISTORTION	As a characteristic of an XRII, variation of the magnification of the image of an object. IMAGE DISTORTION is expressed with respect to a reference magnification (CENTRAL MAGNIFICATION) and as a function of either position (DIFFERENTIAL RADIAL IMAGE DISTORTION) or size (INTEGRAL IMAGE DISTORTION) of the object.		IEC 61262-4:1994
IMAGE MATRIX	Arrangement of MATRIX ELEMENTS in a preferentially Cartesian coordinate system.	rm-32-55	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001

Term	Definition	Reference	Used in IEC
IMAGE PLANE	A plane assigned to a plane in the OBJECT SLICE. NOTE Usually, the IMAGE PLANE is the mid-plane of the corresponding OBJECT SLICE.		IEC 61675-1:1998 IEC 61675-2:1998
IMAGE RECEPTION AREA	In RADIOLOGY, surface on which an X-RAY PATTERN is received.	rm-37-16	IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 61217:2002 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-2:1994
IMAGE RECEPTION PLANE	Plane containing the greatest dimensions of the IMAGE RECEPTION AREA.	rm-37-15	IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61217:2002 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
IMAGE RECEPTOR PLANE IN X-RAY IMAGE INTENSIFIER TUBES	The image receptor plane of an X-RAY IMAGE INTENSIFIER TUBE is taken in this collateral standard IEC 60601-1-3:1994 to be the plane containing the largest selectable IMAGE RECEPTION AREA. NOTE In accordance with this convention, the position of the image receptor plane and thus also the FOCAL SPOT TO IMAGE RECEPTOR DISTANCE, are considered to be unaffected by the selection of different magnification modes.		IEC 60601-1-3:1994
IMMUNITY (to a disturbance)	The ability of an EQUIPMENT and/or system to perform without DEGRADATION in the presence of an electromagnetic disturbance (IEV 161-01-20, modified).		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
IMMUNITY (TO A DISTURBANCE)	Ability of an EQUIPMENT or SYSTEM to perform without DEGRADATION in the presence of an ELECTROMAGNETIC DISTURBANCE [IEV 161-01-20, modified]		IEC 60601-1-2:2001
IMMUNITY LEVEL	Maximum level of a given ELECTROMAGNETIC DISTURBANCE incident on a particular device, EQUIPMENT or system for which it remains capable of operating at a required degree of performance. [IEV 161-03-14]	IEV 161-03-14	IEC 60601-1-2:2001
IMMUNITY TEST LEVEL	Level of a test signal used to simulate an ELECTROMAGNETIC DISTURBANCE when performing an IMMUNITY test. [IEV 161-04-41]		IEC 60601-1-2 2001

Term	Definition	Reference	Used in IEC
IN VITRO COUNTING SYSTEM	Instrument designed to estimate the ACTIVITY of radioactive substances in a sample. NOTE IN VITRO COUNTING SYSTEMS are usually equipped with a scintillation or semi-conductor detector.		IEC 61948-1:2001
IN VIVO COUNTING SYSTEM	Instruments designed to directly measure the ACTIVITY of radioactive substances in the body.		IEC 61948-1:2001
INCUBATOR	An EQUIPMENT having a BABY COMPARTMENT which is provided with the means to control the environment of the baby primarily by heated air within the BABY COMPARTMENT.		IEC 60601-2-19/A1:1996
INCUBATOR TEMPERATURE	Temperature of the air at a point 10 cm above the centre of the mattress surface in the BABY COMPARTMENT (see Figure 102, point A).		IEC 60601-2-19/A1:1996
INDICATED VALUE	Value of a quantity derived from the SCALE READING of an instrument after applying scale factors.	rm-73-10	IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-9:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
INDICATED VALUE	The value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. **Recommended replacement: rm-73-10**		IEC 61676:2002
INDICATED VALUE	The value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. NOTE The INDICATED VALUE is equivalent to the “uncorrected observations” shown in Figure 1 of IEC 60731. **Recommended replacement: rm-73-10**		IEC 60731/A1:2002
INDICATED VALUE	Value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. **Recommended replacement: rm-73-10**		IEC 60580:2000 IEC 61674 /A1:2002
INDIRECT RADIOGRAM	RADIOGRAM obtained after TRANSFER of the information.	rm-32-04	IEC 60601-2-1/A1:2002 IEC 61223-2-9:1999
INDIRECT RADIOGRAPHY	RADIOGRAPHY in which the recording is effected after TRANSFER of the information obtained at an IMAGE RECEPTION AREA.	rm-41-08	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-9:1999 IEC 61223-3-1:1999
INDIRECT RADIOSCOPY	RADIOSCOPY in which the images are presented after TRANSFER of the information so that they can be viewed from outside the RADIATION BEAM.	rm-41-03	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
INDUCED RADIOACTIVITY	RADIOACTIVITY of material caused by IRRADIATION.	rm-12-14	IEC 60601-2-1/A1:2002
INFANT PHOTOTHERAPY EQUIPMENT	IRRADIATION EQUIPMENT which emits in the main RADIATION SPECTRUM in the range between 400 nm to 550 nm for reducing the concentration of bilirubin in the body of infants.		IEC 60601-2-50:2000
INFANT RADIANT WARMER	An electrically powered device with a radiant heating source intended to maintain the thermal balance of an infant PATIENT by direct radiation of energy in the infra-red region of the electromagnetic spectrum.		IEC 60601-2-21/ A1:1996
INFLATING GAS	FRESH GAS that may also power the VENTILATOR.		IEC 60601-2-12:2001
INFLATING GAS INPUT PORT	Input port to which INFLATING GAS is supplied. [ISO 4135:1995, definition 4.2.11] NOTE An input port is a port to which gas is supplied under positive pressure and through which the gas is driven by this pressure. The gas may be supplied either at a controlled pressure or at a controlled flow.		IEC 60601-2-12:2001
INFLOW	The phase during which the peritoneal cavity is filled. NOTE The term fill is commonly used as a synonym for inflow.		IEC 60601-2-39:1999
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument. **Recommended replacement: IEC 60580**		IEC 60731/A1:2002
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument (e. g. ambient temperature, RADIATION QUALITY etc.).		IEC 60580:2000
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument (e.g. ambient temperature etc.) and any property of the X-RAY EQUIPMENT under test that needs to be taken into account in using the instrument FOR NON-INVASIVE MEASUREMENT of X-RAY TUBE VOLTAGE (e.g. range of X-RAY TUBE VOLTAGE, ANODE ANGLE, ANODE material, TOTAL FILTRATION etc.). **Recommended replacement: IEC 60580**		IEC 61676:2002
INFORMATION TECHNOLOGY EQUIPMENT (ITE)	EQUIPMENT designed for the purpose of: a) receiving data from an external source (such as a data input line or via a keyboard); b) performing some processing functions on the received data (such as computation, data transformation or recording, filing, sorting, storage, TRANSFER of data); c) providing a data output (either to other EQUIPMENT or by the reproduction of data or images). NOTE This definition includes electrical or electronic units or systems which predominently generate a multiplicity of periodic binary PULSED electrical or electronic WAVEFORMS and are designed to perform data processing functions such as word processing, electronic computation, data transformation, recording, filing, sorting, storage, retrieval and TRANSFER, and reproduction of data as images. [IEV 161-05-04]	rm-80-09	IEC 60601-1-2:2001 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999 IEC 62083:2000
INFREQUENT USE DEFIBRILLATOR	Term used to describe a DEFIBRILLATOR designed to endure less than 2 500 discharges.		IEC 60601-2-4:2002
INFUSION CONTROLLER	EQUIPMENT intended to regulate the flow of liquid into the PATIENT under positive pressure generated by gravitational force.		IEC 60601-2-24:1998

Term	Definition	Reference	Used in IEC
INFUSION PUMP	EQUIPMENT intended to regulate the flow of liquids into the PATIENT under positive pressure generated by the pump. The INFUSION PUMP may be of: – type 1: continuous infusion flow only; – type 2: non-continuous flow only; – type 3: discrete delivery of a BOLUS; – type 4: type 1 combined with type 3 and/or type 2 in the same EQUIPMENT; – type 5: PROFILE PUMP.		IEC 60601-2-24:1998
INFUSION PUMP FOR AMBULATORY USE	EQUIPMENT intended for the controlled infusion of liquids into the PATIENT and intended to be carried continuously by the PATIENT.		IEC 60601-2-24:1998
INHERENT FILTRATION	QUALITY EQUIVALENT FILTRATION due to the irremovable materials through which the RADIATION BEAM passes before emerging from a RADIATION SOURCE ASSEMBLY or from components thereof. For an X-RAY TUBE ASSEMBLY, the INHERENT FILTRATION is expressed in thickness of a reference material which, at a specified voltage and WAVEFORM, gives the same RADIATION QUALITY in terms of first HALF-VALUE LAYER.	rm-13-46	IEC 61223-3-1:1999 IEC 61267:1994
INHIBITION	Disabling or SILENCING and disabling an ALARM until revoked intentionally.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
INHIBITION (DISABLED)	State in which an ALARM SYSTEM or part of an ALARM SYSTEM can not annunciate ALARM SIGNALS. NOTE 1 INHIBITION may apply to an individual ALARM CONDITION, to a group of ALARM CONDITIONS, or to the entire ALARM SYSTEM of the EQUIPMENT. NOTE 2 INHIBITION may be invoked by the OPERATOR or by the EQUIPMENT (for instance, in a warm-up mode or when no PATIENT is connected). NOTE 3 The duration of inhibition is always indefinite. Only direct action by the OPERATOR or a change in the EQUIPMENT caused by the OPERATOR (for instance, the end of a warm-up mode or when a PATIENT is connected) will revoke INHIBITION.		IEC 60601-2-12:2001
INITIAL CONSTANCY TEST FILM	Film containing the RADIOGRAM of the step wedge part of the TEST DEVICE.		IEC 61223-2-7:1999
INITIAL REFERENCE FILM	Film with an optical density resulting from processing a non-irradiated film under specific conditions prepared during the initial CONSTANCY TEST.		IEC 61223-2-7:1999
INITIAL X-RAY TUBE VOLTAGE	In a capacitor discharge X-RAY GENERATOR, X-RAY TUBE VOLTAGE at the beginning of the LOADING of the X-RAY TUBE.	rm-36-05	IEC 60601-1-3:1994
INITIATION	In RADIOTHERAPY, commencing IRRADIATION from the READY STATE when the READY STATE has been attained by carrying out selection and confirming the operating conditions and not by INTERRUPTION OF IRRADIATION.		IEC 60601-2-17/A1:1996
INPUT APERTURE	The aperture that determines the cross-sectional area of a RADIATION BEAM.		IEC 61262-5:1994
INPUT SCREEN	In an electro-optical vacuum device, layer forming the IMAGE RECEPTION AREA.	rm-32-47	IEC 60601-1-3:1994 IEC 61223-3-1:1999 IEC 61262-5:1994

Term	Definition	Reference	Used in IEC
INSTRUCTIONS FOR USE	Those parts of ACCOMPANYING DOCUMENTS giving the necessary information for safe and proper use and operation of the EQUIPMENT.	rm-82-02	IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/ A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60731/A1:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61331-3:1998 IEC 61674 /A1:2002 IEC 62083:2000
INSTRUMENT ACCURACY	Ratio of the most probable MEASURED VALUE over the TRUE VALUE.		IEC 61303:1994
INSTRUMENT PARAMETER	Any internal property of an instrument that may affect the performance of this instrument.	rm-80-03	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002
INSTRUMENT PARAMETER	Any INTERNAL property of an instrument that may affect the performance of the instrument.		IEC 61676:2002
INTEGRAL IMAGE DISTORTION	IMAGE DISTORTION for a circular TEST DEVICE placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS. Integral image distortion is a function of the radius of this circular TEST DEVICE.		IEC 61262-4:1994

Term	Definition	Reference	Used in IEC
INTEGRAL MAGNIFICATION	As a characteristic of XRIIs, the ratio of the diameter in the OUTPUT IMAGE to the actual diameter of a circular TEST DEVICE placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS. INTEGRAL MAGNIFICATION is a function of the radius of this circular TEST DEVICE.		IEC 61262-4:1994
INTEGRATED PATIENT MONITORING/COMMUNICATIONS SYSTEMS CONTROL SIDE RAIL	See 2.1.103. CONTROL SIDE RAIL with the addition of PATIENT/OPERATOR station communication control, and/or PATIENT television/radio entertainment control, and/or PATIENT room lighting control, and/or PATIENT egress detection system, etc.		IEC 60601-2-38 /A1:1999
INTENDED USE / INTENDED PURPOSE	Use of a product, process or service in accordance with the specifications, instructions and information provided by the MANUFACTURER.		ISO 14971:2000
INTENSIFYING SCREEN	Layer of material used in DIRECT RADIOGRAPHY to convert the incident X-RADIATION or gamma radiation into radiation more suitable for the radiation-sensitive emulsion of the RADIOGRAPHIC FILM.	rm-32-38	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61331-2:1994
INTERCHANGEABLE ANAESTHETIC VAPOUR DELIVERY DEVICE	OPERATOR detachable ANAESTHETIC VAPOUR DELIVERY DEVICE designed to be used with specific EQUIPMENT from different MANUFACTURERS.		IEC 60601-2-13:2003
INTERCONNECTION CONDITIONS	Conditions that shall be fulfilled for safe use when an energized ENDOSCOPE or energized ENDOSCOPICALLY-USED ACCESSORY is used with an ENDOSCOPE.		IEC 60601-2-18 /A1:2000
INTERCONNECTION TERMINAL DEVICE	TERMINAL DEVICE by which internal connections within EQUIPMENT or between EQUIPMENT parts are made.	NG.07.09	IEC 60601-1:1988 IEC 60601-1/A2:1995

Term	Definition	Reference	Used in IEC
INTERLOCK	Device preventing the start or the continued operation of EQUIPMENT unless certain predetermined conditions prevail.	rm-83-05	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17/ A1:1996 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001
INTERMEDIATE RATE	– For VOLUMETRIC INFUSION PUMPS and VOLUMETRIC INFUSION CONTROLLERS, set the rate to 25 ml/h; – for drip-rate INFUSION PUMPS and drip-rate infusion controllers, set the rate to 20 drops/minute; – for SYRINGE PUMPS, set the rate to 5 ml/h; – for SPECIAL USE EQUIPMENT and INFUSION PUMPS for ambulatory use, set the rate specified by the MANUFACTURER as typical for the EQUIPMENT.		IEC 60601-2-24:1998
INTERMITTENT MODE	For an X-RAY GENERATOR, mode of LOADING an X-RAY TUBE where the electric energy is supplied to the tube in single, intermittent or pulsed LOADINGS, as for example in RADIOGRAPHY, CINERADIOGRAPHY.	rm-36-41	IEC 60601-1-3:1994 IEC 60601-2-7:1998
INTERMITTENT OPERATION	Operation in a series of specified identical cycles, each cycle being composed of a period of operation under normal load, without the specified limits of temperature being exceeded, following by a rest period with the EQUIPMENT running idle or switched off.	NG.10.06	IEC 60601-1:1988 IEC 60601-1/A2:1995
INTERNAL ELECTRICAL POWER SOURCE	Power source intended to provide the electrical power necessary to operate EQUIPMENT and which is incorporated in that EQUIPMENT.	NG.01.09	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-12:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
INTERNAL DISCHARGE CIRCUIT	Circuit within the DEFIBRILLATOR which discharges the ENERGY STORAGE DEVICE without energizing the DEFIBRILLATOR ELECTRODES.		IEC 60601-2-4:2002
INTERNALLY POWERED EQUIPMENT	EQUIPMENT able to operate from an INTERNAL ELECTRICAL POWER SOURCE.	NG.02.29	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-26:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
INTERRUPTION	In RADIOTHERAPY, stopping IRRADIATION prior to TERMINATION (of IRRADIATION) with the possibility of CONTINUATION without re-confirmation of operating conditions (i.e. return to READY STATE).		IEC 60601-2-17 /A1:1996

Term	Definition	Reference	Used in IEC
INTERRUPTION (of IRRADIATION)/to interrupt (IRRADIATION)	Stopping of/to stop IRRADIATION and movements with the possibility of continuing without reselecting operating conditions (i.e. a return to the READY STATE).	rm-33-18	IEC 60601-2-11:1997 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
INTERSTITIAL RADIOTHERAPY	RADIOTHERAPY with SEALED RADIOACTIVE SOURCES implanted within the TARGET VOLUME.	rm-42-53	IEC 60601-2-17 /A1:1996
INTERVENTIONAL REFERENCE POINT	For INTERVENTIONAL X-RAY EQUIPMENT, specified point on the REFERENCE AXIS used as a reference location for the indication of PATIENT-incident AIR KERMA and AIR KERMA RATE.	rm-73-19	IEC 60601-2-43:2000
INTERVENTIONAL X-RAY EQUIPMENT	X-RAY EQUIPMENT for RADIOSCOPICALLY GUIDED INTERVENTIONAL PROCEDURES.	rm-31-11	IEC 60601-2-43:2000
INTRACAVITARY RADIOTHERAPY	RADIOTHERAPY in which a RADIATION BEAM or one or more RADIOACTIVE SOURCES, with or without BEAM APPLICATORS or SOURCE APPLICATORS, are introduced into a body cavity through a natural or artificial opening.	rm-42-04	IEC 60601-2-17 /A1:1996
INTRINSIC ENERGY RESOLUTION	The FWHM of the full energy ABSORPTION peak in the INTRINSIC ENERGY SPECTRUM for a specified RADIONUCLIDE.		IEC 60789:1992
INTRINSIC ENERGY SPECTRUM	The measured histogram of PULSE heights for the DETECTOR HEAD without COLLIMATOR (the PULSE height should be expressed as corresponding energy).		IEC 60789:1992
INTRINSIC ERROR	Deviation of the MEASURED VALUE (i.e. the INDICATED VALUE, corrected to REFERENCE CONDITIONS) from the CONVENTIONAL TRUE VALUE under STANDARD TEST CONDITIONS.	rm-73-16	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002 IEC 61676:2002
INTRINSIC LINE SPREAD FUNCTION	The LSF measured with a collimated LINE SOURCE in front of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992
INTRINSIC NON-UNIFORMITY OF RESPONSE	The NON-UNIFORMITY OF RESPONSE of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992 IEC 61948-2:2001
INTRINSIC SPATIAL NON-LINEARITY	The spatial non-LINEARITY of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992
INVASIVE MEASUREMENT	Measurement of the X-RAY TUBE VOLTAGE by external connection of a suitable meter or a high resistance divider.		IEC 61676:2002
IONIZATION CHAMBER	Ionization detector consisting of a CHAMBER filled with a suitable gas, in which an electric field, insufficient to induce gas multiplication, is provided for the collection at the ELECTRODES of charges associated with ions and the ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION.	rm-51-03	IEC 60601-2-9:1996 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61267:1994 IEC 61303:1994

Term	Definition	Reference	Used in IEC
IONIZATION CHAMBER	Detector consisting of a CHAMBER filled with a suitable medium, usually gaseous, in which an electric field, insufficient to induce charge multiplication, is provided for the collection at the ELECTRODES of charges associated with ions and the ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION. NOTE For use with DOSE AREA PRODUCT METERS, IONIZATION CHAMBERS are constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere. Sealed CHAMBERS are not suitable for use with DOSE AREA PRODUCT METERS, because the necessary wall thickness of a sealed CHAMBER may cause an unacceptable energy dependence of the RESPONSE and because the long term stability of sealed CHAMBERS is not guaranteed. **Recommended replacement: rm-51-03**		IEC 60580:2000
IONIZATION CHAMBER TEST SOURCE	RADIOACTIVE SOURCE used for the determination of the long-term stability of an IONIZATION CHAMBER. The half-life of the source shall be greater than five years and the effects of any radioactive contaminants shall be such that the indication by the device over a period of five years would not deviate by more than 0,5 % after decay correction for the known half-life of the principal RADIONUCLIDE.		IEC 61303:1994
IONIZING RADIATION	Radiation consisting of directly or indirectly ionizing particles of a mixture of both. By convention ultraviolet radiation is excluded.	rm-11-02	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000 IEC 61223-2-7:1999 IEC 61262-1:1994 IEC 61303:1994 IEC 61331-1:1994
IONIZING RADIATION SHIELD	Component designed to attenuate the passage of IONIZING RADIATION.		IEC 61303:1994

Term	Definition	Reference	Used in IEC
IRRADIATION	Exposing of a living being or matter to radiation. In RADIOLOGY, exposing of a living being or matter to IONIZING RADIATION. Thus: – X-IRRADIATION; – gamma IRRADIATION; – ELECTRON IRRADIATION; – NEUTRON IRRADIATION.	rm-12-09	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-3:1994 IEC 61331-3:1998 IEC 62083:2000
IRRADIATION	Actual TREATMENT of the PATIENT, it is regarded as commencing when the RADIOACTIVE SOURCES reach their intended positions in the SOURCE APPLICATORS and as ceasing when they leave at the end of TREATMENT. These transit times are explicitly from the TREATMENT TIME. **Recommended replacement: rm-12-09**		IEC 60601-2-17/ A1:1996
IRRADIATION FIELD SIZE	In RADIOTHERAPY, dimensions of an area in a plane perpendicular to the RADIATION BEAM AXIS at a specified distance from the RADIATION SOURCE or at a specified depth in the irradiated object and defined by specified isodose lines.	rm-37-11	IEC 60601-2-11:1997
IRRADIATION SWITCH	In RADIOLOGICAL EQUIPMENT, control device provided to initiate and/or stop IRRADIATION.	rm-30-03	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000

Term	Definition	Reference	Used in IEC
IRRADIATION TIME	Duration of an IRRADIATION determined according to specific methods, usually the time a rate of a RADIATION QUANTITY exceeds a specified level.	rm-36-11	IEC 60336:1993 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-4:2000 IEC 62083:2000
IRRADIATION TIME	Generally the IRRADIATION TIME is measured in terms of LOADING TIME as the time interval between: – the instant that the X-RAY TUBE VOLTAGE has risen for the first time to a value of 75 % of the peak value, and – the instant at which it finally drops below the same value. For systems in which LOADING is controlled by electronic switching of the HIGH VOLTAGE, using a grid in an electronic tube or in the X-RAY TUBE, the LOADING TIME may be determined as the time interval between the instant when the TIMING DEVICE generates the signal to start the IRRADIATION and the instant when it generates the signal to terminate the IRRADIATION. For systems in which LOADING is controlled by simultaneous switching in the primaries of both the high-voltage circuit and the heating supply for the filament of the X-RAY TUBE, the LOADING TIME shall be determined as the time interval between the instant when the X-RAY TUBE CURRENT first rises above 25 % of its maximum value and the instant when it finally falls below the same value. **Recommended replacement: rm-36-11**		IEC 60601-2-7:1998
IRRADIATION TIME	Generally the IRRADIATION TIME is measured in terms of LOADING TIME as the time interval between: – the instant that the X-RAY TUBE VOLTAGE has risen for the first time to a value of 75 % of the peak value, and – the instant at which it finally drops below the same value. **Recommended replacement: rm-36-11**		IEC 60601-2-45:2001
IRRADIATION TIME	Duration of IRRADIATION determined according to specific methods, usually the time during which the rate of a RADIATION QUANTITY exceeds a specified level. **Recommended replacement: rm-36-11**		IEC 60580:2000
IRRADIATION TREATMENT PRESCRIPTION	Quantitative description of all the TREATMENT PARAMETERS that determine the IRRADIATION to be delivered.		IEC 60601-2-17/ A1:1996
ISOCENTRE	In RADIOLOGICAL EQUIPMENT with several modes of movement of the REFERENCE AXIS around a common centre, centre of the smallest sphere through which the RADIATION BEAM AXIS passes.	rm-37-32	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60976 /A1:2000 IEC 61217:2002

Term	Definition	Reference	Used in IEC
ISOCENTRIC	When used in combination with RADIOLOGICAL techniques or EQUIPMENT, refers to the use or presence of an ISOCENTRE.		IEC 60976 /A1:2000
ISOCENTRIC EQUIPMENT	EQUIPMENT for RADIOTHERAPY designed and constructed in such a manner that it has an ISOCENTRE.		IEC 60976/A1:2000
ISOCENTRIC TREATMENT	In RADIOTHERAPY, TREATMENT of a PATIENT in which the position of the TARGET VOLUME is referred to the ISOCENTRE.		IEC 60976/A1:2000
ISOPLANATIC REGION	Region where the form of the POINT SPREAD FUNCTION is constant within specified accuracy.		IEC 61262-7:1995
KEEP OPEN RATE (KOR)	Low predetermined rate(s) to which the EQUIPMENT reverts under specified conditions with the object of keeping the PATIENT LINE open. NOTE The abbreviation KVO (Keep-Vein-Open Rate) is commonly used as a synonym of KOR.		IEC 60601-2-24:1998
KERMA	Letter symbol: *K*. Kinetic energy released in material by IONIZING RADIATION. KERMA is determined as the quotient of dE_{tr} by d*m*, where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in a material of mass d*m*: $K = \frac{dE_{tr}}{dm}$ The unit of KERMA is the joule per kilogram (J.kg^{-1}). The special name of the unit of KERMA is the gray (Gy). The earlier unit of KERMA was the rad, 1 rad being equal to 10^{-2} J.kg^{-1}.	rm-13-10	IEC 60601-2-17/ A1:1996 IEC 60601-2-9:1996 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996
KERMA RATE	Letter symbol: $\dot{K}$. KERMA per unit time. KERMA RATE is determined as the quotient of d*K* by d*t*, where d*K* is the increment of KERMA in the time interval d*t*: $\dot{K} = \frac{dK}{dt}$ A unit of KERMA RATE is any quotient of the gray or its multiples or submultiples by a suitable unit of time (Gy·s^{-1}, mGy·h^{-1}, etc.). Thus: – AIR KERMA RATE.	rm-13-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17/A1:1996 IEC 60806:1984 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 61331-1:1994
LARGE EQUIPMENT OR SYSTEM	EQUIPMENT or SYSTEM that cannot fit within a 2 m x 2 m x 2,5 m volume, excluding cables; this includes distributed SYSTEMS.		IEC 60601-1-2:2001
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the parameter returns to a value which no longer exceeds the ALARM LIMIT or when the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-23:1999 IEC 60601-2-34:2000

Term	Definition	Reference	Used in IEC
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the parameter (which caused the ALARM) returns to a value which no longer exceeds the ALARM LIMIT or if the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-30:1999
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the ALARM CONDITION no longer exists.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
LEAD	ELECTRODE and LEAD WIRE combination(s) used for a certain recording of ECG. Examples: Einthoven limb lead II, Unipolar chest lead V5. [IEC 60601-2-25:1999, definition 2.103, modified]		IEC 60601-2-47:2001
LEAD(S)	ELECTRODE combination used for a certain ECG recording.		IEC 60601-2-25 /A1:1999 IEC 60601-2-26:2002 IEC 60601-2-27:1994 IEC 60601-2-51:2003
LEAD(S)	Combination(s) of ELECTRODES and LEAD WIRES used for a certain ECG recording (see also Table 110).		IEC 60601-2-51:2003
LEAD EQUIVALENT	Letter symbol: δ_{Pb}. ATTENUATION EQUIVALENT expressed in thickness of lead as reference material. NOTE For protection against IONIZING RADIATION it is unnecessary for a material containing a significant amount of lead to specify the RADIATION QUALITY.	rm-13-38	IEC 61331-1:1994 IEC 61331-3:1998
LEAKAGE CURRENT	Current that is not functional. The following LEAKAGE CURRENTS are defined: EARTH LEAKAGE CURRENT, ENCLOSURE LEAKAGE CURRENT and PATIENT LEAKAGE CURRENT.	NG.05.03	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-26:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
LEAD SELECTOR	System to select certain LEADS and TEST.		IEC 60601-2-25 /A1:1999
LEAD SELECTOR	System to select LEADS.		IEC 60601-2-27:1994
LEAD SELECTOR	System to select certain LEADS and CAL.		IEC 60601-2-51:2003
LEAD WIRE(S)	Cable connected between the ELECTRODE and the AMBULATORY RECORDER.		IEC 60601-2-47:2001
LEAD WIRE(S)	Cable(s) connected between ELECTRODE(S) and the ELECTROCARDIOGRAPH.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
LEAKAGE CURRENT	Any current in the signal path arising in the detector and/or MEASURING ASSEMBLY which is not produced by ionization in the RADIATION DETECTOR. Recommended replacement: NG.05.03		IEC 61674/A1:2002
LEAKAGE CURRENT	Any current in the signal path arising in the detector and/or MEASURING ASSEMBLY which is not produced by ionization in the IONIZATION CHAMBER. Recommended replacement: NG.05.03		IEC 60580:2000
LEAKAGE CURRENT (CHAMBER ASSEMBLY)	Any current in the signal path arising in the CHAMBER ASSEMBLY which is not produced by ionization in the measuring volume. NOTE It is distinguished from ZERO DRIFT or ZERO SHIFT which arise in the MEASURING ASSEMBLY.		IEC 60731/A1:2002
LEAKAGE RADIATION	IONIZING RADIATION which has passed through the PROTECTIVE SHIELDING of a RADIATION SOURCE as well as that which, for some types of X-RAY GENERATORS, has passed through the RADIATION APERTURE before and after LOADING (for example one containing a grid controlled X-RAY TUBE).	rm-11-15	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993
LEGIBLE	Displayed qualitative or quantitative information, values, functions, and/or markings discernible or identifiable to an OPERATOR with 6-6 (20/20) vision (corrected if necessary) from a distance of 1 m at a light level of 215 lux, when viewing the information, markings, etc perpendicular to and including 15° above, below, left and right of the normal line of sight of the OPERATOR.		IEC 60601-2-13:2003
LIFE-SUPPORTING EQUIPMENT or SYSTEM	EQUIPMENT or SYSTEM that includes at least one FUNCTION that is intended to actively keep alive or resuscitate PATIENTS and the failure of which to comply with the requirements of 36.202.1 j) is likely to lead to serious injury or death of a PATIENT.		IEC 60601-1:1988
LIFTING POLE	Device suspended above the BED intended to allow the PATIENT to change position by gripping it.		IEC 60601-2-38 /A1:1999
LIGHT DETECTOR	RADIATION DETECTOR sensitive to visible radiation (light).		IEC 61262-7:1995
LIGHT EMISSION PART	That part of the insertion portion of an ENDOSCOPE surrounding the light emission window, delineated as follows: The area of the surface of the insertion portion within three times the maximum diameter of the insertion portion, measured at the tip (distal cover removed) for forward viewing ENDOSCOPES or the centre of the light emission window for side viewing ENDOSCOPES, measured in both longitudinal directions from the centre of the light emission window, but with a minimum of 10 mm and a maximum of 25 mm.		IEC 60601-2-18 /A1:2000
LIGHT FIELD	In EQUIPMENT emitting IONIZING RADIATION, area illuminated by light, being the locus of points at which the illumination exceeds a specific or specified level, simulating the RADIATION FIELD.	rm-37-09	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
LIGHT FIELD CENTRE	(lfc) Point of maximum illuminance in the light field (lighted area). It is the reference point for light field size and distribution measurements.		IEC 60601-2-41:2000
LIGHT FIELD DIAMETER	(d_{10}) Diameter of a circle around the LIGHT FIELD CENTRE (point of CENTRAL ILLUMINANCE) where the illuminance reaches 10 % of E_c.		IEC 60601-2-41:2000
LIGHT FIELD-INDICATOR	In RADIOLOGICAL EQUIPMENT, device to delineate by means of visible light the extent of the field to be irradiated.	rm-37-31	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61331-3:1998
LIMITED X-RAY TUBE VOLTAGE	In an X-ray installation, a NOMINAL X-RAY TUBE VOLTAGE limited for a particular combination.	rm-36-04	IEC 60613:1989
LIMITS OF VARIATION	Maximum VARIATION of a PERFORMANCE CHARACTERISTIC y, permitted by this standard. If LIMITS OF VARIATION are stated as ± L %, the VARIATION $\Delta y/y$, expressed as a percentage, shall remain in the range from – L % to + L %.	rm-73-17	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 A1:2002
LIMITS OF VARIATION	The maximum VARIATION of a PERFORMANCE CHARACTERISTIC y, permitted by this standard. If the LIMITS OF VARIATION are stated as ± L % the VARIATION $\Delta y/y$, expressed as a percentage, shall remain in the range from – L % to + L %.		IEC 61676:2002
LINE OF RESPONSE (LOR)	The axis of the PROJECTION BEAM. NOTE In PET, it is the line connecting the centres of two opposing detector elements operated in coincidence.		IEC 61675-1:1998
LINE PAIR RESOLUTION	Highest spatial frequency of the specified line-group test pattern imaged under specified conditions which is distinguishable in the image. The unit is lp/mm. NOTE Another term for LINE PAIR RESOLUTION used in literature is SPATIAL RESOLUTION. **Recommended replacement: SPATIAL RESOLUTION rm-32-65**		IEC 61223-3-4:2000
LINE PAIR RESOLUTION	Highest spatial frequency of the specified line-group test pattern imaged under specified conditions which is distinguishable in the image. The unit is lp/mm. NOTE LINE PAIR RESOLUTION is used here as a practical substitute for SPATIAL RESOLUTION. **Recommended replacement: SPATIAL RESOLUTION rm-33-56**		IEC 61223-3-1:1999
LINE SOURCE	Straight RADIOACTIVE SOURCE approximating a δ-function in two dimensions and being constant (uniform) in the third dimension.	rm-33-09	IEC 61675-1:1998 IEC 61675-2:1998
LINE SPREAD FUNCTION (ABBREVIATION LSF)	Normalized distribution of irradiance in the image of an incoherently radiating LINE SOURCE. The LINE SPREAD FUNCTION only exists in an ISOPLANATIC REGION, see ISO 9334. NOTE The Fourier transform of the line function is the ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION for the orientation perpendicular to the direction of the LINE SOURCE. **Recommended replacement: rm-73-01**		IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
LINE SPREAD FUNCTION (LSF)	Letter symbol L. In an imaging system, distribution of the intensity from a LINE SOURCE along a straight line in a specified IMAGE PLANE where the straight line is normal to the image of the LINE SOURCE.	rm-73-01	IEC 60789:1992 IEC 61675-1:1998 IEC 61675-3:1998
LINEAR GRID	ANTI-SCATTER GRID composed of highly absorbing strips and highly transmitting interspaces which are parallel in their longitudinal direction.		IEC 60627:2001
LINEAR RANGE	Range of input signals within which the imaging system exhibits LINEARITY within specified accuracy, see ISO 9334. NOTE The range of input signals indicating the LINEAR RANGE of the imaging system should be specified by minimum and maximum levels.		IEC 61262-7:1995
LINEARITY	Property of an imaging system in that the image of a weighted sum of objects is identical to the similarly weighted sum of images of individual objects.		IEC 61262-7:1995
LIQUID SCINTILLATION COUNTER	Counting system utilizing a liquid scintillator in which the radioactive material is distributed. NOTE Usually the LIQUID SCINTILLATION COUNTER is used for measuring samples with β-emitting RADIONUCLIDES.		IEC 61948-1:2001
LITHOTRIPSY	Comminution or fragmentation of calculi.		IEC 60601-2-36:1997
LIVE	State of a part which, when connection is made to that part, can cause a current exceeding the allowable LEAKAGE CURRENT (specified in NG.19.03) for the part concerned to flow from that part to earth or from that part to an ACCESSIBLE PART of the same EQUIPMENT.	NG.01.10	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-51:2003
LOADING	In an X-RAY GENERATOR, act of supplying electrical energy to the ANODE of an X-RAY TUBE.	rm-36-09	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60806:1984 IEC 61223-2-6:1994 IEC 61223-2-10:1999

Term	Definition	Reference	Used in IEC
LOADING FACTOR	Factor influencing by its value the X-RAY TUBE LOAD, for example X- ray tube current, LOADING TIME, equivalent ANODE INPUT POWER, X-RAY TUBE VOLTAGE and PERCENTAGE RIPPLE.	rm-36-01	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
LOADING STATE	For an X-RAY GENERATOR, state from the end of the READY STATE, when the intended function of the generator is initiated, until the end of the LOADING of the X-RAY TUBE.	rm-36-40	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
LOADING TIME	Time, determined according to a specific method, during which the ANODE INPUT POWER is applied to the X-RAY TUBE.	rm-36-10	IEC 60336:1993 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
LOCAL RADIAL MAGNIFICATION	As a characteristic of XRIIs, the ratio of the length in the OUTPUT IMAGE to the actual length of a small TEST DEVICE placed in the ENTRANCE PLANE symmetrically about a given point and oriented radially to the CENTRAL AXIS. LOCAL RADIAL MAGNIFICATION is a function of position of this TEST DEVICE in the ENTRANCE PLANE.		IEC 61262-4:1994
LOCAL RF TRANSMIT COIL	An RF transmit coil other than a VOLUME RF TRANSMIT COIL. The LOCAL RF TRANSMIT COIL can be a coil for spectroscopy.		IEC 60601-2-33:2002
LOCAL SAR	SAR averaged over any 10 g of tissue of the PATIENT body and over a specified time.		IEC 60601-2-33:2002
LOCALIZATION DEVICE	Device used to determine the position of the calculi in (three-dimensional) space.		IEC 60601-2-36:1997
LONG TERM AUTOMATIC MODE	A mode in which a timer, set by the OPERATOR, initiates the measurements.		IEC 60601-2-30:1999
LOW CONTRAST RESOLUTION	Lowest contrast detail object of a specified shape and area that can be resolved from an uniform background.	rm-32-56	IEC 61223-3-1:1999
LOW CONTRAST RESOLUTION	The lowest contrast detail object of a specified object that can be resolved from an uniform background. **Recommended replacement: IEC 61223-3-1**		IEC 61223-3-4:2000
LOW HEAT TRANSFER	Thermal characteristic of a HEATING DEVICE as determined according to Annex CC or Annex DD.		IEC 60601-2-35:1996
LOW POWER EQUIPMENT	EQUIPMENT having a RATED OUTPUT POWER not exceeding 10 W.		IEC 60601-2-3/A1:1998
LOW VOLTAGE	Line-to-line or line-to-neutral voltage that is less than or equal to 1 000 V a.c. or 1 500 V d.c.		IEC 60601-1-2:2001
LOW-FREQUENCY DROP (abbreviation LFD)	Difference between unity and the value of the MODULATION TRANSFER FUNCTION close to zero spatial frequency. NOTE With currently known XRIIs, significant veiling glare is present. This is apparent as a steep drop in the MTF curve slightly above zero spatial frequency. For the purpose of this international standard IEC 61262-7:1995 the spatial frequency at which the LFD is to be determined, is chosen to be 0,1 mm^{-1}.		IEC 61262-7:1995
LOW-PRESSURE GAS INPUT PORT	Input port to which gas is supplied at a pressure not exceeding 100 kPa. [ISO 4135:1995, definition 4.2.14]		IEC 60601-2-12:2001
LUMINAIRE FOR DIAGNOSIS	Luminaire to illuminate the body of the PATIENT locally in order to support diagnosis or TREATMENT which could be interrupted without any hazard for the PATIENT in case of failure of the light. It is not intended to be used in operating rooms. See Table 101.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
LUMINANCE DISTRIBUTION	In an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, spatial VARIATION of luminance over the area of the OUTPUT IMAGE under specific conditions.	rm-32-45	IEC 61262-3:1994
LUMINANCE NON-UNIFORMITY	For an XRII, the difference of luminance between the CENTRE OF THE OUTPUT IMAGE and locations near the periphery of the OUTPUT IMAGE under specific conditions, expressed as a percentage of the luminance at the CENTRE OF THE OUTPUT IMAGE.		IEC 61262-3:1994
MAGNETIC RESONANCE (MR)	Resonant absorption of electromagnetic energy by an ensemble of atomic particles situated in a magnetic field.		IEC 60601-2-33:2002
MAGNETIC RESONANCE EQUIPMENT (MR EQUIPMENT)	MEDICAL ELECTRICAL EQUIPMENT which is intended for in-vivo MAGNETIC RESONANCE EXAMINATION of a PATIENT. The MR EQUIPMENT comprises all parts in hardware and software from the SUPPLY MAINS to the display monitor. The MR EQUIPMENT is a Programmable Electrical Medical System (PEMS).		IEC 60601-2-33:2002
MAGNETIC RESONANCE EXAMINATION (MR EXAMINATION)	Process of acquiring data by MAGNETIC RESONANCE from a PATIENT.		IEC 60601-2-33:2002
MAGNETIC RESONANCE SYSTEM (MR SYSTEM)	Ensemble of MR EQUIPMENT, ACCESSORIES including means for display, control, energy supplies, and the CONTROLLED ACCESS AREA, where provided.		IEC 60601-2-33:2002
MAINS CONNECTOR	Part of an APPLIANCE COUPLER integral with or intended to be attached to a flexible cord which is intended to be connected to the SUPPLY MAINS. A MAINS CONNECTOR is intended to be inserted into the APPLIANCE INLET of EQUIPMENT.	NG.07.10	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS PART	Entirety of all parts of EQUIPMENT intended to have a CONDUCTIVE CONNECTION with the SUPPLY MAINS. For the purpose of this definition, the PROTECTIVE EARTH CONDUCTOR is not regarded as a part of the MAINS PART.	NG.01.12	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001
MAINS PLUG	Part integral with or intended to be attached to a power SUPPLY CORD of EQUIPMENT, to be inserted into a FIXED MAINS SOCKET OUTLET.	NG.07.11	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS TERMINAL DEVICE	TERMINAL DEVICE by which the electrical connection to the SUPPLY MAINS is made.	NG.07.12	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS VOLTAGE	Voltage of a SUPPLY MAINS between two line conductors of a polyphase system or voltage between the line conductor and the neutral conductor of a single-phase system.	NG.04.02	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
MAJOR SURGICAL LUMINAIRE	Single luminaire in the PATIENT environment which is FAIL SAFE and provides an adequate CENTRAL ILLUMINANCE to illuminate locally the body of the PATIENT. It is intended to support the TREATMENT and diagnosis, and to be used in operating rooms. See Table 101.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
MAMMOGRAPHIC ANTI-SCATTER GRID	FOCUSED GRID specially designed for mammography. NOTE In this Standard the term "general purpose ANTI-SCATTER GRID" is used to describe any ANTI-SCATTER GRID not specially designed for mammography.		IEC 60627:2001
MAMMOGRAPHIC STEREOTACTIC DEVICE	Device for three-dimensional localization of a point within the breast, and for mechanically guided placement of a needle or position marker for such purposes as fine-needle aspiration, core biopsy and pre-surgical localization. The localization is based on radiographic images of an immobilized breast acquired at different known angles. Such a device may be a dedicated system or an ACCESSORY for mammographic X-RAY EQUIPMENT.	rm-35-20	IEC 60601-2-45:2001
MANUAL DEFIBRILLATOR	DEFIBRILLATOR capable of being manually operated by the OPERATOR for selection of energy, charging and discharging.		IEC 60601-2-4:2002
MANUAL MODE	A mode of operation in which the heater is either at a fixed level or a proportion of its maximum output set by the USER.		IEC 60601-2-21/A1:1996
MANUAL MODE	A mode in which the OPERATOR has full control of the INITIATION of each measurement.		IEC 60601-2-30:1999
MANUAL VENTILATION PORT	Port to which a device may be connected for manual inflation of the lungs. [ISO 4135:1995, definition 4.2.15 modified]		IEC 60601-2-12:2001

Term	Definition	Reference	Used in IEC
MANUFACTURER	Organization or individual who produces an EQUIPMENT. (Term without definition in IEC 60788)	MR-121-01 (rm-85-03)	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1 /A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60731/A1:2002 IEC 61217:2002 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61674/A1:2002 IEC 62083:2000
MANUFACTURER	Natural or legal person with responsibility for the design, manufacture, packaging or labelling of a medical device, assembling a system, or adapting a medical device before it is placed on the market and/or put into service, regardless of whether these operations are carried out by that person himself or on his behalf by a third party.		ISO 14971:2000
MATCHED LOAD	Resistive load normally in the range 50 Ω to 75 Ω, which, when replacing the APPLICATOR, results in a voltage standing wave ratio (VSWR) not exceeding 1,5 in the APPLICATOR connecting cable or waveguide.		IEC 60601-2-6:1984

Term	Definition	Reference	Used in IEC
MATRIX ELEMENT	Smallest unit of an IMAGE MATRIX, which is assigned in location and size to a certain volume element of the object (VOXEL).	rm-32-58	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
MATTRESS	HEATING DEVICE providing resilient support to the whole body of a PATIENT.		IEC 60601-2-35:1996
MATTRESS SUPPORT PLATFORM	Structural surface on which the PATIENT sleeping surface (for example mattress) rests in NORMAL USE. The MATTRESS SUPPORT PLATFORM articulates or changes positions to facilitate various therapeutic, diagnostic and convenience positions. (See Figures 101 and 112.)		IEC 60601-2-38/A1:1999
MAXIMUM ANODE HEAT CONTENT	Maximum permissible ANODE HEAT CONTENT.	rm-36-27	IEC 60601-2-28:1993 IEC 60613:1989
MAXIMUM CONTINUOUS HEAT DISSIPATION	Highest value of the X-RAY TUBE ASSEMBLY INPUT POWER which can be applied to an X-RAY TUBE ASSEMBLY continuously under specified conditions without exceeding the MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT.	rm-36-34	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-44:2002 IEC 60613:1989
MAXIMUM ENERGY	Highest RADIATION ENERGY contained in a beam of polyenergetic radiation.	rm-13-32	IEC 60601-1-3:1994 IEC 60601-2-45:2001
MAXIMUM GRADIENT SLEW RATE	The rate of change of the gradient obtained by switching the GRADIENT UNIT between its maximum specified gradient strengths G_{+max} and G_{-max} in the shortest possible ramp time obtainable under normal scan conditions.		IEC 60601-2-33:2002
MAXIMUM INFUSION PRESSURE	Maximum PRESSURE which can be generated by the EQUIPMENT under conditions of total occlusion at the end of the PATIENT LINE.		IEC 60601-2-24:1998
MAXIMUM LIMITED PRESSURE ($P_{LIM}max$)	Highest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE and under a SINGLE FAULT CONDITION.		IEC 60601-2-12:2001
MAXIMUM PEAK VOLTAGE	Maximum value of the X-RAY TUBE VOLTAGE in a specified time interval. The unit of this quantity is the volt (V).		IEC 61676:2002
MAXIMUM PERMISSIBLE WORKING PRESSURE	PRESSURE specified by the MANUFACTURER or by the inspection authority or competent person(s) in the report of the most recent examination.	NG.11.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAXIMUM TOLERABLE RISK	Value of RISK which is specified as the maximum which may be permitted. NOTE The value may be specified for the PEMS as a whole or for a particular hazard.		IEC 60601-1-4:2000
MAXIMUM TRACKING RATE	Maximum PULSE RATE at which the PULSE GENERATOR will respond on a 1:1 basis to a triggering signal.		IEC 60601-2-31/A1:1998
MAXIMUM TRACKING RATE	Maximum ventricular pacing rate in response to sensed arterial ACTIVITY.		IEC 60601-2-31/A1:1998
MAXIMUM WORKING PRESSURE ($P_w$max)	Highest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE, irrespective of the setting of controls, other than the control intended to adjust this PRESSURE. NOTE Even if not adjustable, this maximum is equal to or less than the MAXIMUM LIMITED PRESSURE.		IEC 60601-2-12:2001
MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT	Maximum permissible X-RAY TUBE ASSEMBLY HEAT CONTENT under specific ambient conditions.	rm-36-31	IEC 60601-2-28:1993 IEC 60613:1989
MEAN CT NUMBER	Mean value of the COMPUTED TOMOGRAPHY NUMBERS of all PIXELS within a certain defined region of interest.		IEC 61223-2-6:1994

Term	Definition	Reference	Used in IEC
MEAN PEAK VOLTAGE	Mean value of all X-RAY TUBE VOLTAGE peaks during a specified time interval. The unit of this quantity is the volt (V).		IEC 61676:2002
MEASURED VALUE	Estimate of the TRUE VALUE of a quantity, derived from the INDICATED VALUE of a meter after applying all relevant CORRECTION FACTORS.	rm-73-08	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61303:1994
MEASURED VALUE	The best estimate of the TRUE VALUE of a quantity, being derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS and the CALIBRATION FACTOR. NOTE The MEASURED VALUE is the "final result of measurement" shown in Figure 1 of IEC 60731:2002. **Recommended replacement: rm-73-08**		IEC 60731:2002
MEASURED VALUE	Best estimate of the TRUE VALUE of a quantity, derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS.		IEC 61674/A1:2002
MEASURED VALUE	Value of a physical quantity derived by applying all relevant corrections to an INDICATED VALUE. **Recommended replacement: rm-73-08**		IEC 60580:2000
MEASURED VALUE	The best estimate of the CONVENTIONAL TRUE VALUE of a quantity, being derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS. NOTE The CONVENTIONAL TRUE VALUE will usually be the value determined by the WORKING STANDARD with which the instrument under test is being compared. **Recommended replacement: rm-73-08**		IEC 61676:2002
MEASURING ASSEMBLY	Device to convert the output from the IONIZATION CHAMBER into a form suitable for the display of the value(s) of DOSE AREA PRODUCT or DOSE AREA PRODUCT RATE.		IEC 60580:2000
MEASURING ASSEMBLY	A device to convert the output from the RADIATION DETECTOR into a form suitable for display, control or storage of the values of ABSORBED DOSE, ABSORBED DOSE RATE or any dose-related quantities. It includes all electrical circuits in use during the period of PATIENT contact up to and including any SEPARATION DEVICE(S).		IEC 60601-2-9:1996
MEASURING ASSEMBLY	A device to measure the charge (or current) from the IONIZATION CHAMBER and convert it into a form suitable for displaying the values of dose or KERMA (or their corresponding rates). **Recommended replacement: IEC 60601-2-9:1996**		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
MEASURING ASSEMBLY	Device to convert the output from the DETECTOR ASSEMBLY into a form suitable for the display of the value(s) of AIR KERMA, AIR KERMA LENGTH or AIR KERMA RATE. **Recommended replacement: IEC 60601-2-9:1996**		IEC 61674/A1:2002
MECHANICAL INDEX	MECHANICAL INDEX is given by $MI \equiv \frac{p_{ra} f_{awf}^{-1/2}}{C_{MI}}$ where C_{MI} = 1 MPa MHz$^{-1/2}$; p_{ra} is the ATTENUATED PEAK-RAREFACTIONAL PRESSURE in megapascals; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz. Symbol: *MI*. Unit: None.		IEC 60601-2-37:2001
MEDICAL DEVICE	Any instrument, apparatus, appliance, material or other article, whether used alone or in combination, including the software necessary for its proper application, intended by the MANUFACTURER to be used for human beings for the purpose of – diagnosis, prevention, monitoring, TREATMENT or alleviation of disease, – diagnosis, monitoring, TREATMENT, alleviation of, or compensation for, an injury or handicap, – investigation, replacement or modification of the anatomy or of a physiological process, – control of conception, and which does not achieve its principal intended action in or on the human body by pharmacological, immunological or metabolic means, but which may be assisted in its function by such means. [ISO 13485:1996, definition 3.1]		ISO 14971:2000
MEDICAL DIAGNOSTIC RADIOLOGY	Medical diagnosis using IONIZING RADIATION.	rm-40-04	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 60806:1984 IEC 61223-2-1:1993

Term	Definition	Reference	Used in IEC
MEDICAL ELECTRICAL EQUIPMENT (hereinafter referred to as EQUIPMENT)	Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT. The EQUIPMENT includes those accessories as defined by the MANUFACTURER which are necessary to enable the NORMAL USE of the EQUIPMENT.	NG.02.15	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-13:2003 IEC 60601-2-33:2002 IEC 60601-2-51:2003 IEC 60731 /A1:2002 IEC 61217:2002 IEC 61674/A1:2002 IEC 62083:2000
MEDICAL ELECTRICAL EQUIPMENT	Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT. Under the scope of this Particular Standard EQUIPMENT means HAEMODIALYSIS, HAEMODIAFILTRATION and/or HAEMOFILTRATION EQUIPMENT.		IEC 60601-2-16:1998
MEDICAL ELECTRICAL EQUIPMENT	Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT. Under the scope of this Particular Standard EQUIPMENT means PERITONEAL DIALYSIS EQUIPMENT.		IEC 60601-2-39:1999
MEDICAL ELECTRICAL EQUIPMENT	Electrical EQUIPMENT, provided with one or more connections to particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT. See Figure 101 describing the possible SUPPLY MAINS for SURGICAL LUMINAIRES.		IEC 60601-2-41:2000
MEDICAL ELECTRICAL SYSTEM		NG-2.203	IEC 60601-1-4:2000
MEDICAL ELECTRICAL SYSTEM	Totality of more than one item of MEDICAL ELECTRICAL EQUIPMENT or of MEDICAL ELECTRICAL EQUIPMENT in combination with other non-medical electrical EQUIPMENT that by COUPLING behaves as a unit with specified functions.		IEC 60601-2-13:2003
MEDICAL ELECTRICAL SYSTEM	Combination of items of EQUIPMENT, at least one of which must be MEDICAL ELECTRICAL EQUIPMENT and interconnected by FUNCTIONAL CONNECTION or use of a MULTIPLE PORTABLE SOCKET-OUTLET. NOTE EQUIPMENT when mentioned in connection with a SYSTEM, should be taken to include EQUIPMENT.		IEC 60601-1 /A2:1995 IEC 60601-1-2:2001
MEDICAL RADIOLOGICAL EXAMINATION	Medical examination using effects of IONIZING RADIATION.	rm-41-24	IEC 60580:2000

Term	Definition	Reference	Used in IEC
MEDICAL RADIOLOGY	Branch of RADIOLOGY applied to human and veterinary medicine as well as to dentistry and chiropractic.	rm-40-03	IEC 60601-2-43:2000
MEDICAL SUPERVISION	Adequate medical management of PATIENTS who may be at risk from some parameters of EXPOSURE to the MR EQUIPMENT, either because of the medical condition of the PATIENT, the levels of EXPOSURE or a combination,		IEC 60601-2-33:2002
MICROWAVE THERAPY EQUIPMENT	EQUIPMENT for the TREATMENT of the PATIENT by means of a propagated electromagnetic field in the frequency range of more than 300 MHz but not exceeding 30 GHz.		IEC 60601-2-6:1984
MID POINT AVERAGE TEMPERATURE	(T_M) The TEST DEVICE AVERAGE TEMPERATURE of the TEST DEVICE positioned at the mid point of the EQUIPMENT mattress. (See Figure 102.)		IEC 60601-2-21/A1:1996
MINIMUM BREAKING LOAD	Maximum load where Hooke's Law is applicable.	NG.11.03	IEC 60601-1/A2:1995
MINIMUM EFFECTIVE RANGE	The MINIMUM EFFECTIVE RANGE is the smallest permitted range of INDICATED VALUES for which an instrument complies with a stated performance.		IEC 61676:2002
MINIMUM LIMITED PRESSURE (P_{LIM}min)	Lowest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE and under a SINGLE FAULT CONDITION. NOTE This PRESSURE may be sub-atmospheric.		IEC 60601-2-12:2001
MINIMUM RATE	Lowest rate selectable by the OPERATOR, but not less than 1 ml/h. NOTE For INFUSION PUMPS FOR AMBULATORY USE it is the lowest selectable rate.		IEC 60601-2-24:1998
MINIMUM RATED RANGE	Least range of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER over which the instrument shall operate within the specified LIMITS OF VARIATION in order to comply with this standard.		IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002
MINOR SURGICAL LUMINAIRE (TREATMENT luminaire)	Single luminaire in the PATIENT environment which provides an adequate CENTRAL ILLUMINANCE to illuminate the body of the PATIENT locally. It is intended to be used in operating rooms for diagnosis and TREATMENT which can be interrupted without any hazard for the PATIENT in case of failure of the light. See Table 101.		IEC 60601-2-41:2000
MINUTE VOLUME ($\dot{V}$)	Volume of gas per minute entering or leaving the lungs of the PATIENT.		IEC 60601-2-12:2001
MOBILE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another between periods of use while supported by its own wheels or equivalent means.	NG.02.16	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001
MOBILE OPERATING TABLE	An OPERATING TABLE intended to be moved from one location to another.		IEC 60601-2-46:1998
MODE OF OPERATION	For INTERVENTIONAL X-RAY EQUIPMENT, the technical state defined by a configuration of several predetermined LOADING FACTORS, technique factors or other settings for RADIOSCOPY or RADIOGRAPHY, selectable simultaneously by the operation of a single control. NOTE 1 Selection of a particular mode does not necessarily define the values of all the parameters affecting its use. NOTE 2 Values defined by selection of a particular mode are not necessarily invariable during its use.		IEC 60601-2-43:2000

Term	Definition	Reference	Used in IEC
MODEL OR TYPE REFERENCE	Combination of figures, letters or both used to identify a particular model of EQUIPMENT.	NG.12.02	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000
MODES OF OPERATION WITH CONTINUED DISPLAY	An X-RAY IMAGING ARRANGEMENT operating with continued display is regarded in this collateral standard IEC 60601-1-3:1994 as an X-RAY IMAGING ARRANGEMENT for RADIOSCOPY if means are provided for automatic repetition of irradiation.		IEC 60601-1-3:1994
MODULATION TRANSFER FUNCTION (abbreviation MTF)	Modulus of the ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION. NOTE The MTF is defined in ISO 9334 as the modulus of the OPTICAL TRANSFER FUNCTION. For the purpose of this international standard IEC 61262-7:1995, this definition is more appropriate. **Recommended replacement: rm-73-05**		IEC 61262-7:1995
MODULATION TRANSFER FUNCTION (MTF)	Letter symbol: M. Fourier transform of the LINE SPREAD FUNCTION. For a symmetrical line spread function, the MODULATION TRANSFER FUNCTION is the normalized Fourier transform using the equation: $$M(v) = \frac{\int_{-\infty}^{+\infty} L(x) \cos 2\pi v x dx}{\int_{-\infty}^{+\infty} L(x) x dx}$$ where: v is the spatial frequency, L is the LINE SPREAD FUNCTION, x is the abscissa.	rm-73-05	IEC 60336:1993 IEC 60789:1992 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
MOMENTARY CONTACT SWITCH	Control device which initiates and maintains operation of operating elements only as long as the control (actuator) is actuated. The manual control (actuator) returns automatically to the stop position when released. MOMENTARY CONTACT SWITCHES are also known as “hold-to-run control devices”.		IEC 60601-2-38/ A1:1999
MONITOR	Part of a DEFIBRILLATOR providing a visual display of the electrical ACTIVITY of the PATIENT’S heart. NOTE The term is used within this Particular Standard to distinguish such a monitor from one which forms a separate EQUIPMENT in its own right even in cases where the separate stand-alone monitor is able to provide synchronization signals to the DEFIBRILLATOR, used as basis for AED rhythm recognition detection or providing control signals to the DEFIBRILLATOR.		IEC 60601-2-4:2002
MONITORING DEVICE	Device which continuously or repeatedly measures and indicates the value of a variable to the OPERATOR.		IEC 60601-2-13:2003

Term	Definition	Reference	Used in IEC
MOVING BEAM RADIOTHERAPY	RADIOTHERAPY with continuous displacement of the RADIATION SOURCE relative to the PATIENT during the IRRADIATION.	rm-42-41	IEC 60601-2-11:1997 IEC 60976/A1:2000 IEC 61217:2002
MOVING BEAM RADIOTHERAPY	RADIOTHERAPY with any planned displacement of the RADIATION FIELD or PATIENT relative to each other or with any planned change of ABSORBED DOSE distribution. **Recommended replacement: rm-42-41**		IEC 60601-2-1/A1:2002
MOVING GRID	ANTI-SCATTER GRID used in an ACCESSORY that enables that ANTI-SCATTER GRID to be moved, when irradiated by a RADIATION BEAM, in order to avoid the imaging of the absorbing strips and the consequent loss of information.	rm-32-15	IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-2:1996
MOVING GRID	ANTI-SCATTER GRID used in an ACCESSORY that enables the ANTI-SCATTER GRID to be moved, when irradiated by a RADIATION BEAM, in order to avoid the imaging of the absorbing strips and the consequent loss of information.		IEC 60627:2001
MTF ANALYZER	Instrument, including relay optics and software, capable of performing measurements of the MODULATION TRANSFER FUNCTION.		IEC 61262-7:1995
MULTI-DETECTOR COUNTER	Instrument consisting of an array of WELL-TYPE DETECTORS to determine the ACTIVITY in multiple samples simultaneously.		IEC 61948-1:2001
MULTI-PURPOSE ULTRASONIC EQUIPMENT	Ultrasonic EQUIPMENT which is intended for more than one clinical application.		IEC 60601-2-37:2001
MULTICHANNEL ELECTROCARDIOGRAPH	EQUIPMENT for the simultaneous recording of several ECG LEADS. This EQUIPMENT may also provide facilities for phonocardiography and PULSE recording, etc.		IEC 60601-2-25 A1:1999
MULTICHANNEL ELECTROCARDIOGRAPH	EQUIPMENT for the simultaneous recording of two or more ECG LEADS. This EQUIPMENT may also provide facilities for phonocardiography and PULSE recording, etc.		IEC 60601-2-51:2003
MULTIFUNCTION PATIENT MONITORING EQUIPMENT	A modular or pre-configured device including more than one PHYSIOLOGICAL MONITORING UNIT designed to collect information from a single PATIENT and process it for monitoring purposes and to generate ALARMS.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
MULTIPLE FUNCTION	Measurement of more than one physiological parameter.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
MULTIPARAMETER PATIENT MONITORING EQUIPMENT	Stationary or MOBILE EQUIPMENT powered by an electrical power source and including one or more physiological monitoring units designed to collect information from a PATIENT, process it and generate ALARMS.		IEC 60601-2-23:1999
MULTIPLE WINDOW SPATIAL REGISTRATION	The measured position of a source as a function of the PULSE amplitude analyzer window setting.		IEC 60789:1992
NARROW BEAM	RADIATION BEAM of a solid angle as small as possible for measuring a desired RADIATION QUANTITY thus minimizing the contribution of SCATTERED RADIATION and ensuring, if relevant, the lateral electronic equilibrium.	rm-37-22	IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
NARROW BEAM CONDITION	Arrangement for the measurement of a RADIATION QUANTITY in a NARROW BEAM of IONIZING RADIATION.	rm-37-23	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994
NATIONAL STANDARD	A standard recognized by an official national decision as the basis for fixing the value in that country of all other standards of the given quantity.		IEC 60731/A1:2002
NET OPTICAL DENSITY	Density above FILM BASE PLUS FOG DENSITY.		IEC 61223-2-10:1999
NEUTRAL ELECTRODE	Electrode of a relatively large area for connection to the body of the PATIENT, intended to provide a return path for the high frequency current with such a low current density in the body tissue that physical effects such as unwanted burns are avoided. NOTE The NEUTRAL ELECTRODE is also known as plate, plate electrode, passive, return or dispersive electrode.		IEC 60601-2-2:1998
NEUTRAL ELECTRODE	Reference point for differential amplifiers and/or interference suppression circuits, not forming part of any ELECTROCARDIOGRAPH LEAD. [IEC 60601-2-25:1999, definition 2.107]		IEC 60601-2-25:1993 IEC 60601-2-27:1994 IEC 60601-2-47:2001
NEUTRAL ELECTRODE	ELECTRODE used as a common mode reference for differential amplifiers and/or interference suppression which is not involved in an EQUIPMENT ELECTRODE combination.		IEC 60601-2-26:2002
NEUTRAL ELECTRODE	Reference point for differential amplifiers and/or interference suppression circuits. Any ELECTROCARDIOGRAPHIC LEAD is independent of the potential of this reference point.		IEC 60601-2-51:2003
NEUTRON	Elementary particle having no electric charge, a rest mass of 1,67492 x 10^{-27} kg, and a mean life of about 1 000 s.	rm-11-17	IEC 60601-2-1/A1:2002
NOISE	VARIATION OF COMPUTED TOMOGRAPHY NUMBERS from a mean value in a defined area in the image of a uniform substance. The magnitude of NOISE is indicated by the standard deviation of the COMPUTED TOMOGRAPHY NUMBERS of a uniform substance in the region of interest.		IEC 61223-2-6:1994
NOISE	Unwanted signals of any frequency present in the ELECTROCARDIOGRAM.		IEC 60601-2-51:2003
NOMINAL (value)	Value quoted for reference purposes which is subject to agreed tolerances, for example, NOMINAL MAINS VOLTAGE, NOMINAL diameter of a screw.	NG.12.03	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-44:2002
NOMINAL ANODE INPUT POWER	Highest constant ANODE INPUT POWER that can be applied for a single X-RAY TUBE LOAD in a specific LOADING TIME.	rm-36-23	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989

Term	Definition	Reference	Used in IEC
NOMINAL ELECTRIC POWER	For a HIGH-VOLTAGE GENERATOR, highest constant electric power which can be delivered for a single X-RAY TUBE LOAD in a specific LOADING TIME.	rm-36-19	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001
NOMINAL ENERGY	for ELECTRON radiation, energy stated by the MANUFACTURER to characterize the RADIATION BEAM. This energy is approximately equal to the most probable energy at the surface of the measuring PHANTOM, $E_{p,0}$ (see ICRU Report 35; Section 3.3; Energy, $E_{p,0}$); for X-RADIATION, the energy stated by the MANUFACTURER to characterize the RADIATION BEAM.	rm-13-56	IEC 60601-2-1/A1:2002 IEC 62083:2000
NOMINAL ENERGY	As a characteristic of medical ELECTRON accelerators, RADIATION ENERGY describing: – for X-RADIATION the energy of the ELECTRONS striking the TARGET, and for ELECTRON radiation the energy of the ELECTRONS in the USEFUL BEAM at the PHANTOM surface in the NORMAL TREATMENT DISTANCE. **Recommended replacement: rm-13-56**		IEC 60976/ A1:2000
NOMINAL ENTRANCE FIELD SIZE	For an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, ENTRANCE FIELD SIZE that would be achieved with a parallel beam of IONIZING RADIATION.	rm-32-44	IEC 61223-3-1:1999
NOMINAL ENTRANCE FIELD SIZE	The ENTRANCE FIELD SIZE of the XRII that would be achieved with a parallel beam of IONIZING RADIATION with the RADIATION SOURCE approaching infinity. **Recommended replacement: rm-32-44**		IEC 61262-1:1994
NOMINAL FOCAL SPOT VALUE	Dimensionless numerical value having a specific relation to the dimensions of the effective spot of an X-RAY TUBE, measured under specific conditions.	rm-20-14	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-6:1994 IEC 61262-7:1995
NOMINAL IMAGE SIZE	The product of the linear dimension of a small OBJECT in the ENTRANCE PLANE and the CENTRAL MAGNIFICATION.		IEC 61262-6:1994
NOMINAL SHORTEST IRRADIATION TIME	For HIGH-VOLTAGE GENERATORS with AUTOMATIC CONTROL SYSTEMS which vary the IRRADIATION TIME, shortest IRRADIATION TIME for which a required constancy of the controlled RADIATION QUANTITY is maintained.	rm-36-12	IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-3-1:1999
NOMINAL TOMOGRAPHIC SECTION THICKNESS	In CT SCANNERS the TOMOGRAPHIC SECTION THICKNESS which is selected and indicated on the CONTROL PANEL.		IEC 60601-2-44:2002
NOMINAL TOMOGRAPHIC SECTION THICKNESS	In CT SCANNERS the TOMOGRAPHIC SECTION THICKNESS which is selected and indicated on the CONTROL PANEL. NOTE In helical scanning the thickness of a reconstructed image depends on the helical reconstruction algorithm and pitch, and hence this thickness may not equal the NOMINAL TOMOGRAPHIC SECTION THICKNESS. The thickness of the reconstructed image may be indicated or selected prior to the helical scan.		IEC 60601-2-44:2002

Term	Definition	Reference	Used in IEC
NOMINAL SENSITIVITY	The ratio of the change in TRANSDUCER output to a change of the value of the PRESSURE at any selected pressure range.		IEC 60601-2-34:2000
NOMINAL TOMOGRAPHIC SLICE THICKNESS	In EQUIPMENT for COMPUTED TOMOGRAPHY, SLICE THICKNESS selected and indicated at the CONTROL PANEL. **Recommended replacement: NOMINAL TOMOGRAPHIC SECTION THICKNESS**		IEC 61223-2-6:1994
NOMINAL X-RAY TUBE VOLTAGE	Highest permitted X-RAY TUBE VOLTAGE for specific operating conditions.	rm-36-03	IEC 60336:1993 IEC 60522:1999 IEC 60601-2-7:1998 IEC 60601-2-8,1999 IEC 60601-2-28:1993 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60806:1984 IEC 61267:1994
NON-FLAMMABLE ANAESTHETIC AGENTS	(IEC 60601-1)		IEC 60601-2-13:2003
NON-INTERCHANGEABLE ANAESTHETIC VAPOUR DELIVERY DEVICE	ANAESTHETIC VAPOUR DELIVERY DEVICE designed to be used only with EQUIPMENT specified by the MANUFACTURER. NOTE These devices may or may not be OPERATOR-detachable.		IEC 60601-2-13:2003
NON-ISOCENTRIC	When used in combination with RADIOLOGICAL techniques or EQUIPMENT, refers to conditions without the use of, or to the absence of, an ISOCENTRE.		IEC 60976/ A1:2000
NON-LATCHED ALARM	An ALARM, the visual and auditory manifestation of which stops when the parameter (which caused the ALARM) returns to a value which no longer exceeds the ALARM LIMIT or if the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-23:1999
NON-LATCHED ALARM	An ALARM, the auditory or visual and auditory manifestations of which stop when the ALARM CONDITION no longer exists.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
NON-LATCHING ALARM SIGNAL	ALARM SIGNAL that automatically stops ANNUNCIATING when its associated ALARM CONDITION no longer exists		IEC 60601-2-13:2003
NON-LINEARITY	Deviation from LINEARITY, quantified as follows: on each range the half full SCALE READING M is taken as a reference; the input signal Q required to produce this REFERENCE SCALE READING is measured. At another SCALE READING m produced by an input signal q, the percentage deviation from LINEARITY is given by: $100 \cdot ((m \cdot Q / M \cdot q) - 1)$ NOTE 1 For a MEASURING ASSEMBLY set to the “dose” mode, the input signal is electric charge; NOTE 2 For a MEASURING ASSEMBLY set to the “dose rate” mode, the input signal is electric current.		IEC 60731/A1:2002
NON-IMPLANTABLE PULSE GENERATOR	MEDICAL ELECTRICAL EQUIPMENT with an INTERNAL ELECTRICAL POWER SOURCE which is intended for use outside the body and which produces a periodic electrical PULSE intended to stimulate the heart through a LEAD (or combination of a LEAD and PATIENT CABLE).		IEC 60601-2-31/ A1:1998

Term	Definition	Reference	Used in IEC
NON-INVASIVE MEASUREMENT	Measurement of X-RAY TUBE VOLTAGE by analysis of the emitted radiation.		IEC 61676:2002
NON-IRRADIATED CONSTANCY TEST FILM	Film with an optical density resulting from processing a non-irradiated film under specific conditions.		IEC 61223-2-7:1999
NON-SCANNING MODE	Mode of operation of an ULTRASONIC DIAGNOSTIC EQUIPMENT that involves a sequence of ultrasonic PULSES which give rise to ultrasonic scan lines that follow the same acoustic path.		IEC 60601-2-37:2001
NON-SCREEN FILM	In DIRECT RADIOGRAPHY, RADIOGRAPHIC FILM to be used without an INTENSIFYING SCREEN.	rm-32-35	IEC 60336:1993 IEC 60806:1984 IEC 61223-2-1:1993 IEC 61223-3-4:2000 IEC 61262-3:1994
NON-UNIFORMITY OF RESPONSE	In a RADIONUCLIDE imaging device, differences in COUNT RATE between small areas of specified dimensions within the DETECTOR FIELD OF VIEW when a uniform plane source parallel to the detector face and of dimensions larger than its ENTRANCE FIELD is used.	rm-34-26	IEC 60789:1992 IEC 61948-2:2001
NORMAL CONDITION	Condition in which all means provided for protection against SAFETY HAZARDS are intact.	NG.10.07	IEC 60601-1/ A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17 A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
NORMAL OPERATING MODE	Mode of operation of the MR EQUIPMENT in which none of the outputs have a value that may cause physiological stress to PATIENTS.		IEC 60601-2-33:2002
NORMAL POSITION	The position of the OPERATING TABLE top with all sections set in the horizontal position.		IEC 60601-2-46:1998
NORMAL SENSITIVITY	SENSITIVITY of 10 mm per mV.		IEC 60601-2-25/A1:1999 IEC 60601-2-51:2003
NORMAL TREATMENT DISTANCE	For ELECTRON IRRADIATION, specified distance measured along the axis of the beam from the VIRTUAL SOURCE of ELECTRONS to the ENTRANCE SURFACE. For X-IRRADIATION, specified distance measured along the axis of the beam from the VIRTUAL SOURCE of X-RADIATION to the ISOCENTRE or, in EQUIPMENT without an ISOCENTRE, to a specified plane.	rm-33-16	IEC 60601-2-8,:1999 IEC 60976 /A1:2000 IEC 61217:2002
NORMAL TREATMENT DISTANCE	A specified distance measured along the RADIATION BEAM AXIS from the RADIATION SOURCE to the ISOCENTRE or, for EQUIPMENT without an ISOCENTRE, to a specified plane. **Recommended replacement: IEC 60976, IEC 61217:2002**		IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
NORMAL TREATMENT DISTANCE (abbreviation: NTD)	For ELECTRON IRRADIATION, specified distance measured along the REFERENCE AXIS from the ELECTRON radiation window to the distal end of the ELECTRON beam APPLICATOR or to a specified plane; FOR X-IRRADIATION, specified distance measured along the REFERENCE AXIS from the front surface of the TARGET to the ISOCENTRE or, for EQUIPMENT without an ISOCENTRE, to a specified plane. **Recommended replacement: IEC 60976, IEC 61217:2002**		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
NORMAL USE	Use and operation, as well as transport and storage between periods of use, according to the INSTRUCTIONS FOR USE or for the obvious intended purpose.	rm-82-04	IEC 60336:1993 IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61331-3:1998 IEC 62083:2000
NORMAL USE	Operation, including routine inspection and adjustments by the OPERATOR, and STAND-BY, according to the INSTRUCTIONS FOR USE.	NG.10.08	IEC 60601-1/A2:1995 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17/A1:1996 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
NORMALIZED SLICE SENSITIVITY	SLICE SENSITIVITY divided by the AXIAL SLICE WIDTH (EW) for that slice.		IEC 61675-1:1998
NORMALIZED VOLUME SENSITIVITY	VOLUME SENSITIVITY divided by the AXIAL FIELD OF VIEW of the tomograph or the PHANTOM length, whichever is the smaller.		IEC 61675-2:1998
NUCLEAR MEDICINE	Use of unsealed RADIONUCLIDES for diagnostic and therapeutic purposes.	rm-40-06	IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61303:1994
OBJECT PROGRAMMED CONTROL	In an X-RAY GENERATOR, mode of operation in which (a) semi-permanently pre-set combination(s) of LOADING FACTORS is (are) pre-selected depending upon the object to be irradiated, usually for diagnostic purposes.	rm-36-44	IEC 60601-2-7:1998
OBJECT SLICE	A slice in the object. The physical property of this slice that determines the measured information is displayed in the tomographic image.	rm-32-59	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
OBJECTIVE EVIDENCE	Information which can be proven true, based on facts obtained through observation, measurement, TEST or other means. [ISO 8402:1994, definition 2.19]		ISO 14971:2000
OBLIQUE CROSS GRID	CROSS GRID in which the directions of the absorbing strips form an angle other than 90°.		IEC 60627:2001
OCCLUSION ALARM THRESHOLD (PRESSURE)	Value of the physical quantity at which the occlusion ALARM is activated.		IEC 60601-2-24:1998
OFFSET	Deviation of the position of the PROJECTION of the COR (X'_p) from $X_p = 0$.		IEC 61675-2:1998 IEC 61948-2:2001
ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION (abbreviation 1-OTF)	Section of the OPTICAL TRANSFER FUNCTION through the origin in a given orientation.		IEC 61262-7:1995
ONE-PEAK HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR for operation on a single-phase supply that delivers an unrectified output voltage, or a rectified output voltage with one peak during each cycle of the supply.	rm-21-02	IEC 60601-2-7:1998 IEC 60613:1989
OPERATING CABLE	A PATIENT supporting table for general, surgical/medical procedures.		IEC 60601-2-46:1998
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this collateral standard, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NOMINAL use of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item.	rm-36-49	IEC 60601-1-3:1994
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this standard, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NOMINAL USE of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item.		IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this standard IEC 60601-2-7:1998, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NORMAL USE of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item. **Recommended: Definition from IEC 60601-1-3**		IEC 60601-2-7:1998
OPERATING FREQUENCY	Fundamental frequency of a signal, electrical or non-electrical, that is set in an EQUIPMENT or SYSTEM intended to control a physiological parameter.		IEC 60601-1-2:2001
OPERATOR	Person utilizing an EQUIPMENT individually with or without the aid of an assistant, who controls some or all functions of the EQUIPMENT in his presence.	rm-85-02	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60731/A1:2002 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61674 /A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
OPERATOR	Person handling EQUIPMENT. **Recommended replacement: rm-85-02**	NG.12.17	IEC 60601-1/ A2:1995 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-26:2002 IEC 60601-2-32:1994 IEC 60601-2-47:2001 IEC 60601-2-51:2003
OPERATOR'S POSITION	Intended location and orientation of the OPERATOR with respect to the EQUIPMENT for NORMAL USE according to the instructions for use.		IEC 60601-2-12:2001
OPTICAL TRANSFER FUNCTION (abbreviation OTF)	Two-dimensional Fourier transform of the imaging system's POINT SPREAD FUNCTION, see ISO 9334. NOTE For the OPTICAL TRANSFER FUNCTION to have significance, it is essential that the imaging system is working in its LINEAR RANGE, and that an ISOPLANATIC REGION is considered.		IEC 61262-7:1995
ORGAN COUNTING SYSTEM	Instrument used for radiation detection of incorporated radioactive substances in specific organs or regions of the body.		IEC 61948-1:2001
ORTHOGONAL CROSS GRID	CROSS GRID in which the directions of the absorbing strips form an angle of 90°.		IEC 60627:2001
OUTFLOW	The phase during which the peritoneal cavity is emptied. NOTE The term drain is commonly used as a synonym for outflow.		IEC 60601-2-39:1999
OUTPUT CIRCUIT	All conductive parts used to couple radio-frequency power from the generator to the APPLICATORS, including conductive (inaccessible) parts of the APPLICATORS and their connecting cables.		IEC 60601-2-3 /A1:1998
OUTPUT IMAGE	In an electro-optical vacuum device, light image generated in the OUTPUT SCREEN.	rm-32-49	IEC 61223-2-1:1993 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
OUTPUT POWER	Time-average ultrasonic power radiated by a TREATMENT HEAD of EQUIPMENT into an approximately free field under specified conditions in a specified medium, preferably in water (see 3.5 of IEC 61161). [IEC 61689, definition 3.31]		IEC 60601-2-5:2000
OUTPUT POWER	Time-average power radiated by an ULTRASONIC TRANSDUCER into an approximately free-field under specified conditions in a specified medium, preferably water. Symbol: *P*. Unit: milliwatts, mW.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
OUTPUT SCREEN	In an electro-optical vacuum device, layer in which the ELECTRON pattern is converted into a light image.	rm-32-48	IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-7:1995
OVARY SHIELD	PROTECTIVE DEVICE intended to protect the gonads of a female PATIENT.	rm-64-07	IEC 61331-3:1998
OVERALL UNCERTAINTY	Uncertainty associated with the MEASURED VALUE, i.e. it represents the bounds within which the ERROR OF MEASUREMENT is estimated to lie. NOTE For the purpose of this standard IEC 60731/A1:2002 the OVERALL UNCERTAINTY may be taken as the EXPANDED UNCERTAINTY corresponding to a confidence level of 95 %.		IEC 60731/A1:2002
OVERALL UNCERTAINTY	Quadrature combination of the random and non-random uncertainties at the 68 % confidence limits. **Recommended replacement: IEC 61674**		IEC 61303:1994
OVERALL UNCERTAINTY	Uncertainty associated with the MEASURED VALUE, i.e. representing the bounds within which the ERROR OF MEASUREMENT is estimated to lie.		IEC 61674/ A1:2002
OVERLOAD TOLERANCE	Maximum input-circuit voltage which does not alter the functioning of the ELECTROCARDIOGRAPH.		IEC 60601-2-51:2003
OVER-BLANKET	BLANKET to be used over a PATIENT.		IEC 60601-2-35:1996
OVER-CURRENT RELEASE	PROTECTIVE DEVICE which causes a circuit to open with or without delay, when the current in the device exceeds a predetermined value.	NG.09.07	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-45:2001
OXYGEN RICH ENVIRONMENT	An environment in which partial pressure of oxygen is greater than 275 hPa.		IEC 60601-2-13:2003
PAD	HEATING DEVICE which can be bent but not folded.		IEC 60601-2-35:1996
PARALLEL GRID	LINEAR GRID in which the planes of the absorbing strips are parallel to each other and perpendicular to the incident face.		IEC 60627:2001
PARALLEL HOLE COLLIMATOR	COLLIMATOR with a number of apertures, the axes of which are parallel.		IEC 60789:1992
PART LEAKAGE CURRENT	Current flowing from a SINGLE FUNCTION through the PATIENT to the remaining SINGLE FUNCTION(S) of the same APPLIED PART under NORMAL CONDITION.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
PARTIAL BODY SAR	SAR averaged over the mass of the PATIENT'S body that is exposed by the VOLUME RF TRANSMIT COIL and over a specified time.		IEC 60601-2-33:2002
PARTICLE ACCELERATOR	EQUIPMENT for accelerating charged particles such as ELECTRONS, protons, deuterons and alpha particles to kinetic energies higher than corresponding to the voltage applied. Thus: – ELECTRON accelerator.	rm-23-01	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000 IEC 61217:2002 IEC 62083:2000
PASSWORD	For EQUIPMENT under the control of a PROGRAMMABLE ELECTRONIC SUBSYSTEM (PESS), sequence of keystrokes that permits OPERATOR access for NORMAL USE or to reset INTERLOCKS and, with a different sequence of keystrokes, permits access for adjustment and maintenance.		IEC 60601-2-1/A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
PATIENT	Living being (person or animal) undergoing medical or dental investigation or TREATMENT.	NG.12.04	IEC 60580:2000 IEC 60601-1/A2:1995 IEC 60601-1-4:2000 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-26:2002 IEC 60601-2-32:1994 IEC 60601-2-47:2001 IEC 60601-2-51:2003 IEC 60731/A1:2002 IEC 61674/A1:2002
PATIENT	Person or animal undergoing medical examination or TREATMENT. For purposes of RADIOLOGICAL PROTECTION, a person or animal is a PATIENT only during the intentional application of IONIZING RADIATION to that person or animal. **Recommended replacement: NG.12.04**	rm-62-03	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 672083:2000

Term	Definition	Reference	Used in IEC
PATIENT	An infant who is being treated by means of visible radiation. Recommended replacement: NG 12.04		IEC 60601-2-50:2000
PATIENT ANATOMY MODEL/ANATOMY MODELLING	All physical and anatomical parameters required to plan a course of RADIOTHERAPY for a particular PATIENT. The process of establishing the PATIENT ANATOMY MODEL is referred to as "ANATOMY MODELLING".		IEC 62083:2000
PATIENT AUXILIARY CURRENT	Current flowing in the PATIENT in NORMAL USE between parts of the APPLIED PART and not intended to produce a physiological effect, for example, bias current of an amplifier, current used in impedance plethysmography.	NG.05.04	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
PATIENT CABLE	Multiwire cable and associated connector(s) to connect the ELECTRODES to the ELECTROCARDIOGRAPH. **Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE**		IEC 60601-2-25 /A1:1999 IEC 60601-2-51:2003
PATIENT CABLE	Multiwire cable and associated connector(s) to connect the ELECTRODES to the AMBULATORY RECORDER. [IEC 60601-2-25:1999, definition 2.109] **Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE**		IEC 60601-2-26:2002 IEC 60601-2-47:2001
PATIENT CABLE	Device attached to the terminals of a non-implantable PULSE GENERATOR so that the distance between it and the pacing LEAD can be increased. **Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE**		IEC 60601-2-31 /A1:1998
PATIENT CIRCUIT	Any electrical circuit which contains one or more PATIENT CONNECTIONS. PATIENT CIRCUITS include all conductive parts which are not insulated from the PATIENT CONNECTIONS to the extent necessary to comply with the dielectric strength requirements or which are not separated from the PATIENT CONNECTIONS to the extent necessary to comply with the CREEPAGE DISTANCE and AIR CLEARANCE requirements.	NG.01.15	IEC 60601-1/A2:1995
PATIENT CONNECTION	Every individual part of the APPLIED PART through which current can flow between the PATIENT and the EQUIPMENT in NORMAL CONDITION or SINGLE FAULT CONDITION.	NG.01.23	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-51:2003
PATIENT CONNECTION PORT (OF THE VENTILATOR BREATHING SYSTEM)	Port of the VENTILATOR BREATHING SYSTEM to which the PATIENT can be connected. [ISO 4135:1995, definition 4.2.16] NOTE Interface between the VENTILATOR BREATHING SYSTEM and the PATIENT.		IEC 60601-2-12:2001
PATIENT ELECTRODE	Means in contact with a specified part of the body to detect heart action voltage in combination with another means. [IEC 60601-2-25:1999, definition 2.104]		IEC 60601-2-47:2001
PATIENT END	That end of the PATIENT LINE where connection to the PATIENT takes place.		IEC 60601-2-24:1998
PATIENT ENVIRONMENT	IEC 601-1-1 2.202		IEC 60601-2-9:1996

Term	Definition	Reference	Used in IEC
PATIENT EXTRAPMENT	The ability for a PATIENT to insert his / her head, neck or chest cavity into a permanent opening in the BED and/or its ACCESSORIES or a temporary opening created during NORMAL USE and from which the PATIENT cannot remove that portion of his/her anatomy.		IEC 60601-2-38 /A1:1999
PATIENT LEAKAGE CURRENT	Current flowing from the APPLIED PART via the PATIENT to earth or flowing from the PATIENT via an F-type APPLIED PART to earth originating from the unintended appearance of a voltage from an external source on the PATIENT.	NG.05.06	IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-51:2003
PATIENT LINE	That part of the ADMINISTRATION SET between the EQUIPMENT and the PATIENT.		IEC 60601-2-24:1998
PATIENT SUPPORT	In RADIOLOGICAL EQUIPMENT, component such as a table top or arm rest, serving to support the PATIENT in order to allow the part of his body which is to be irradiated to be positioned or to be displaced.	rm-30-02	IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61217:2002 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61267:1994
PATIENT SUPPORT	The assembly of EQUIPMENT that supports the PATIENT. **Recommended replacement: rm-30-02**		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
PATIENT SURFACE	In RADIOLOGY, surface through which the radiation enters the body of the PATIENT.	rm-37-18	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-3:1998
PEAK-RAREFACTIONAL ACOUSTIC PRESSURE	Maximum of the modulus of the negative instantaneous acoustic pressure in an acoustic field during an acoustic repetitions period. Symbol: p_r. Unit: megapascals, MPa.		IEC 60601-2-37:2001
PENDANT CONTROL	Means, used by either PATIENT or OPERATOR, to control the drives that activate various BED functions.		IEC 60601-2-38 A1:1999

Term	Definition	Reference	Used in IEC
PENETRATIVE QUALITY	Depth in a PHANTOM most distant from its surface at which the ABSORBED DOSE is 80 % of the maximum ABSORBED DOSE both measured on the radiation axis in a specified RADIATION FIELD and with the surface of the PHANTOM at a specified distance.		IEC 60976/A1:2000
PENUMBRA	In RADIOLOGY, spatial region around the RADIATION BEAM where the value of radiation flux is between two specified or specific fractions of the value that is measured in the RADIATION BEAM AXIS, these two values being measured in a same cross-section. NOTE The existence of such spatial regions can be due to one or more of the following phenomena: – EXTRA-FOCAL RADIATION; – SCATTERED RADIATION; – absence of lateral electronic equilibrium; – pair production; – geometry of the RADIATION SOURCE and of the BEAM LIMITING SYSTEM.	rm-37-08	IEC 60976/A1:2000 IEC 62083:2000
PERCENTAGE RIPPLE	For a HIGH-VOLTAGE GENERATOR, ratio of the difference between the highest and the lowest values of a rectified voltage WAVEFORM during a cycle of the supply to the highest value, expressed as a percentage.	rm-36-17	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 60601-2-45:2001 IEC 60613:1989 IEC 61267:1994 IEC 61331-1:1994
PERCENTAGE RIPPLE IN CONSTANT POTENTIAL HIGH-VOLTAGE GENERATORS	Unless otherwise stated, it is to be assumed that for a HIGH-VOLTAGE GENERATOR to be regarded as a CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR, the PERCENTAGE RIPPLE of its output voltage (under the relevant conditions) does not exceed 4. **Recommended replacement: rm-36-17**		IEC 60601-2-7:1998 IEC 60601-2-45:2001
PERFORMANCE CHARACTERISTIC	One of the quantities used to define the performance of an instrument (e.g. RESPONSE, LEAKAGE CURRENT).	rm-72-05	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
PERFORMANCE CHARACTERISTIC	One of the quantities used to define the performance of an instrument (e.g. RESPONSE). **Recommended replacement: IEC 60731, IEC 61674**		IEC 61676:2002
PERITONEAL DIALYSIS	A process whereby DIALYSING SOLUTION is introduced into the peritoneal cavity of the PATIENT and is subsequently removed.		IEC 60601-2-39:1999
PERITONEAL DIALYSIS EQUIPMENT	EQUIPMENT used to perform PERITONEAL DIALYSIS.		IEC 60601-2-39:1999
PERMANENT FILTRATION	The QUALITY EQUIVALENT FILTRATION effected in an X-RAY TUBE ASSEMBLY by permanently fixed materials intercepting the X-ray beam, that are not intended to be removed for any application and are not provided with means for removal in NORMAL USE.		IEC 60522:1999

Term	Definition	Reference	Used in IEC
PERMANENTLY INSTALLED EQUIPMENT	EQUIPMENT that is electrically connected to the SUPPLY MAINS by means of a permanent connection which can only be detached by the use of a TOOL.	NG.02.17	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PHANTOM	In MEDICAL RADIOLOGY, object behaving in essentially the same manner as tissue, with respect to ABSORPTION or SCATTERING of the IONIZING RADIATION in question. PHANTOMS are used, for example, for simulating practical conditions of measurement: – for purposes of RADIATION PROTECTION; – for evaluation the performances of diagnostic systems with respect to the radiation or to the object; – for dosimetry.	rm-54-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994
PHANTOM	Device, intended to simulate parts of the PATIENT for test purposes.		IEC 60601-2-6:1984
PHOTON	Stable elementary particle, quantum of electromagnetic radiation.	rm-11-19	IEC 61223-2-10:1999
PHYSIOLOGICAL ALARM	Signal which either indicates that a monitored physiological parameter is out of the specified limits or indicates an abnormal PATIENT condition.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
PHYSIOLOGICAL MONITORING UNIT	A part of the EQUIPMENT whose purpose is to collect information relating to (a) physiological function(s) and to process it for monitoring and summary diagnostic purposes.		IEC 60601-2-49:2001 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
PHYSICAL POINT SPREAD FUNCTION	For tomographs, a two-dimensional point function in planes perpendicular to the PROJECTION BEAM at specified distances from the detector. NOTE The PHYSICAL POINT SPREAD FUNCTION characterizes the purely physical imaging performance of the tomographic device independent from, e.g. sampling, image reconstruction and image processing, but dependent on the COLLIMATOR. A PROJECTION BEAM is characterized by the entirety of all PHYSICAL POINT SPREAD FUNCTIONS as a function of distance along its axis.		IEC 61675-1:1998 IEC 61675-2:1998
PHYSIOLOGICAL SIMULATION FREQUENCY	Fundamental frequency of a signal, electrical or non-electrical, used to simulate a physiological parameter such that the EQUIPMENT or SYSTEM will operate in a manner consistent with use on a PATIENT.		IEC 60601-1-2:2001
PILE UP EFFECT	False measurement of the PULSE amplitude, due to the ABSORPTION of two or more gamma rays, reaching the same RADIATION DETECTOR within the RESOLVING TIME.		IEC 61675-1:1998
PINHOLE CAMERA	Assembly of EQUIPMENT used to obtain a FOCAL SPOT PINHOLE RADIOGRAM on RADIOGRAPHIC FILM.	rm-71-02	IEC 60336:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000
PIN-HOLE COLLIMATOR	COLLIMATOR with one small aperture in a plane in front of the RADIATION DETECTOR ASSEMBLY.		IEC 60789:1992
PIXEL	MATRIX ELEMENT in a two-dimensional IMAGE MATRIX.	rm-32-60	IEC 61675-1:1998 IEC 61675-2:1998
PLAYBACK EQUIPMENT	EQUIPMENT for monitoring and documenting functions into which data from the RECORDER is fed. NOTE This EQUIPMENT is usually stationary and commonly includes computing facilities.		IEC 60601-2-47:2001
POINT SOURCE	RADIOACTIVE SOURCE approximating a δ-function in all three dimensions.	rm-34-36	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-2:2001
POINT SPREAD FUNCTION (PSF)	Normalized distribution of irradiance in the image of a POINT SOURCE, see ISO 9334.		IEC 61262-7:1995
POINT SPREAD FUNCTION (PSF)	Scintigraphic image of a POINT SOURCE. **Recommended replacement: IEC 61262-7**		IEC 61675-1:1998 IEC 61675-2:1998
PORTABLE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another while used or between periods of use while being carried by one or more persons.	NG.02.18	IEC 60601-1/A2:1995 IEC 60601-2-32:1994 IEC 60601-2-51:2003
PORTABLE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another while in use of between periods of use, by one or more persons or by other means. Recommended replacement: NG.02.18		IEC 60601-2-24:1998
POSITIONING DEVICE	Device which brings the calculi into coincidence with the TARGET LOCATION.		IEC 60601-2-36:1997
POSITIONING TIME	((see DETECTOR POSITIONING TIME))		IEC 61675-2:1998
POSITRON EMISSION TOMOGRAPH	Tomographic device, which detects the ANNIHILATION RADIATION of positron emitting RADIONUCLIDES by COINCIDENCE DETECTION.		IEC 61675-1:1998

Term	Definition	Reference	Used in IEC
POSITRON EMISSION TOMOGRAPHY (PET)	EMISSION COMPUTED TOMOGRAPHY utilizing the ANNIHILATION RADIATION of positron emitting RADIONUCLIDES by COINCIDENCE DETECTION.		IEC 61675-1:1998
POST-VENTRICULAR ATRIAL REFRACTORY PERIOD (PVARP)	Period after a ventricular event (whether sensed or paced), in which there is no sensing in the atrium.		IEC 60601-2-31/A1:1998
POST-VENTRICULAR ATRIAL REFRACTOR PERIOD (PVARP)	Period after a ventricular event (whether sensed or paced), during which synchronous ventricular pacing is disabled, regardless of any atrial event.		IEC 60601-2-31/A1:1998
POTENTIAL EQUALIZATION CONDUCTOR	Conductor providing a connection between EQUIPMENT and the potential equalization busbar of the electrical installation.	NG.06.06	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
POWER SUPPLY	Any source of energy, other than that generated directly by the human body or by gravity, that makes the device function.		IEC 60601-2-13:2003
POWER SUPPLY CORD	Flexible cord, fixed to or assembled with EQUIPMENT for mains supply purposes	NG.07.17	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
PRACTICAL PEAK VOLTAGE (PPV)	The PRACTICAL PEAK VOLTAGE $\hat{U}$ is defined as: $\hat{U} = \frac{\int_{U_{min}}^{U_{max}} p(U) \cdot w(U) \cdot U dU}{\int_{U_{min}}^{U_{max}} p(U) \cdot w(U) dU}$ with $\int_{U_{min}}^{U_{max}} p(U) dU = 1$ where *p(U)* is the distribution function for the voltage *U* and *w(U)* is a weighting function. U_{max} is the highest voltage in the interval, and U_{min} is the lowest voltage in the interval. The unit of the quantity PRACTICAL PEAK VOLTAGE is the volt (V). NOTE Additional information on the PRACTICAL PEAK VOLTAGE, the weighting function *w(U)* and the distribution function *p(U)* is provided in Annex B. Using this weighting function *w(U)* the PRACTICAL PEAK VOLTAGE will be defined as the constant potential which produces the same AIR KERMA contrast behind a specified PHANTOM as the non-dc voltage under test.		IEC 61676:2002
PRACTICAL RANGE	For ELECTRON radiation, depth in a PHANTOM with its surface at the NORMAL TREATMENT DISTANCE, for which on the DEPTH DOSE chart the extrapolation of the steepest fall-off section of the ABSORBED DOSE distribution along the RADIATION BEAM AXIS intercepts the extrapolated tail of the ABSORBED DOSE distribution.		IEC 60976/ A1:2000

Term	Definition	Reference	Used in IEC
PREPARATORY STATE	State of EQUIPMENT for setting essential operating conditions, if in the STAND-BY STATE the setting of these conditions is not possible.	rm-84-04	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999
PRESSURE (overpressure)	PRESSURE above atmospheric (gauge pressure).	NG.11.04	IEC 60601-1/A2:1995 IEC 60601-2-28:1993 IEC 60601-2-33:2002 IEC 60601-2-44:2002
PRESSURE PULSE	Acoustic wave emitted by the LITHOTRIPSY EQUIPMENT.		IEC 60601-2-36:1997
PRESSURE PULSE COUPLING	Any means allowing transition of the PRESSURE PULSE from the EQUIPMENT into the PATIENT.		IEC 60601-2-36:1997
PRIMARY DOSE MONITORING SYSTEM	DOSE MONITORING SYSTEM which is intended to terminate IRRADIATION when a pre-selected value is reached.	rm-33-03	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000
PRIMARY PROTECTIVE SHIELDING	PROTECTIVE SHIELDING for attenuating RESIDUAL RADIATION.	rm-64-02	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-45:2001
PRIMARY RADIATION	IONIZING RADIATION emitted directly by the TARGET or by a RADIOACTIVE SOURCE.	rm-11-06	IEC 60601-2-44:2002 IEC 60627:2001 IEC 61223-2-11:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
PRIMARY TIMER	The CONTROLLING TIMER which is intended to terminate IRRADIATION at the pre-selected time.		IEC 60601-2-11:1997
PRIMARY/SECONDARY (timer) COMBINATION	Combination of two timers in which one is arranged to be the PRIMARY TIMER and the other is to be the SECONDARY TIMER.	rm-21-11	IEC 60601-2-8:1999 IEC 60601-2-11:1997
PRIMARY/SECONDARY DOSE MONITORING COMBINATION	Utilization of two DOSE MONITORING SYSTEMS where one is arranged to be the PRIMARY and the other the SECONDARY DOSE MONITORING SYSTEM.	rm-33-17	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
PRIMARY-SECONDARY DOSE MONITORING SYSTEM	Combination of two DOSE MONITORING SYSTEMS in which one is arranged to be the PRIMARY DOSE MONITORING SYSTEM and the other is to be the SECONDARY DOSE MONITORING SYSTEM. **Recommended replacement: PRIMARY/SECONDARY DOSE MONITORING COMBINATION**		IEC 60976/A1:2000
PROCEDURE	Specific way to perform an ACTIVITY. [ISO 8402:1994, definition 1.3]		ISO 14971:2000
PROCESS	Set of inter-related resources and activities which transform inputs into outputs. [ISO 8402:1994, definition 1.2]		ISO 14971:2000
PROFILE PUMP	EQUIPMENT intended for controlled infusion of liquids into the PATIENT by means of a programmed sequence of delivery rates.		IEC 60601-2-24:1998

Term	Definition	Reference	Used in IEC
PROGRAMMABLE ELECTRICAL MEDICAL SYSTEM (PEMS)	MEDICAL ELECTRICAL EQUIPMENT or MEDICAL ELECTRICAL SYSTEM containing one or more PROGRAMMABLE ELECTRONIC SUBSYSTEM.	rm-80-04	IEC 60601-1-4:2000 IEC 62083:2000
PROGRAMMABLE ELECTRONIC SUBSYSTEM (PESS)	System based on one or more central processing units, including their software and interfaces.	rm-80-05	IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
PROGRAMMABLE ELECTRONIC SYSTEM (abbreviation: PES)	Term used to cover systems incorporating a wide range of programmable devices including microprocessors, programmable controllers, programmable logic controllers and other computer based devices. These devices may contain one or more central processing units connected to sensors and/or actuators, for the purpose of control, protection or monitoring.		IEC 60601-2-11:1997
PROJECTION	Transformation of a three-dimensional object into its two-dimensional image or of a two-dimensional object into its one-dimensional image, by integrating the physical property which determines the image along the direction of the PROJECTION BEAM. NOTE This process is mathematically described by line integrals in the direction of PROJECTION and called the Radon-transform.	rm-32-61	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
PROJECTION ANGLE	Angle at which the PROJECTION is measured or acquired.	rm-32-62	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
PROJECTION BEAM	Determines the smallest possible volume in which the physical property which determines the image is integrated during the measurement process. Its shape is limited by the SPATIAL RESOLUTION in all three dimensions. NOTE The PROJECTION BEAM mostly has the shape of a long thin cylinder or cone. In POSITRON EMISSION TOMOGRAPHY, it is the SENSITIVE VOLUME between two detector elements operated in coincidence.		IEC 61675-1:1998
PROJECTION BEAM	Determines the smallest possible volume in which the physical property which determines the image is integrated during the measurement process. Its shape is limited by the SPATIAL RESOLUTION in all three dimensions. NOTE In SPECT the PROJECTION BEAM usually has the shape of a long thin diverging cone. **Recommended replacement: IEC 61675-1:1998**		IEC 61675-2:1998
PROPERLY INSTALLED	Condition in which at least the relevant instructions concerning installation given by the MANUFACTURER in the ACCOMPANYING DOCUMENTS are observed.	NG.10.09	IEC 60601-1/A2:1995
PROTECTED AREA	Defined area within an area under surveillance or within a CONTROLLED AREA which is protected by STRUCTURAL SHIELDING or by distance so that the level of radiation is lower than is required for the total area of which it is a part.	rm-63-06	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-43:2000
PROTECTIVE BARRIER	PROTECTIVE SHIELDING in the form of attenuating material provided for RADIOLOGICAL PROTECTION.	rm-64-04	IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
PROTECTIVE COVER	Part of an ENCLOSURE or guard provided to prevent accidental access to parts which might be hazardous if contacted.	NG.01.17	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE DEVICE	In RADIOLOGY, device for the purpose of RADIOLOGICAL PROTECTION. Thus: – protective clothing: – protective apron; – protective skirt; – protective glove; – mobile protective barrier.	rm-64-05	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-1:1993 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998
PROTECTION DEVICE	No definition - **Recommended replacement: rm-64-05**	NG.09.08	IEC 60601-2-8:1999
PROTECTION DEVICE	Device which, without intervention of the OPERATOR, protects the PATIENT from hazardous output due to incorrect delivery of energy or substances. **Recommended replacement: rm-64-05**		IEC 60601-2-13:2003
PROTECTIVE EARTH CONDUCTOR	Conductor to be connected between the PROTECTIVE EARTH TERMINAL and an external protective earthing system.	NG.06.07	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE EARTH TERMINAL	Terminal connected to conductive parts of CLASS I EQUIPMENT for SAFETY purposes. This terminal is intended to be connected to an external protective earthing system by a PROTECTIVE EARTH CONDUCTOR.	NG.06.08	IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE GLASS PLATE	PROTECTIVE DEVICE of an optical quality suitable for transmitting visual images.		IEC 61331-2:1994
PROTECTIVE GLASS PLATE TYPE SC	PROTECTIVE GLASS PLATE of high optical quality with specified ATTENUATION properties used in DIRECT RADIOSCOPY for observation of the image in the FLUORESCENT SCREEN.		IEC 61331-2:1994
PROTECTIVE GLASS PLATE TYPE VI	PROTECTIVE GLASS PLATE of low optical quality with specified ATTENUATION properties used to provide optically clear and transparent PROTECTIVE SHIELDING.		IEC 61331-2:1994

Term	Definition	Reference	Used in IEC
PROTECTIVE GONAD APRON	Protective apron worn by the PATIENT to protect the region of the gonads as an alternative to the use of a SCROTUM SHIELD or an OVARY SHIELD; see rm-64-05 of IEC 60788.		IEC 61331-3:1998
PROTECTIVE MITTEN	Protective glove with open palm and separated thumb used where full perception of touch is essential.		IEC 61331-3:1998
PROTECTIVE SHIELDING	In RADIOLOGY, material that limits the extent of the RADIATION BEAM or attenuates STRAY RADIATION. NOTE PROTECTIVE SHIELDING may include materials provided for RADIOLOGICAL PROTECTION, or devices or materials provided for other purposes, which attenuate IONIZING RADIATION.	rm-64-01	IEC 60580:2000 IEC 60601-1-3:1994 IEC 61331-2:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997
PROTECTIVE SYSTEM	An automatic system which senses a specified parameter (or parameters), or a constructional feature, specifically designed to protect the PATIENT against SAFETY HAZARDS which may arise.		IEC 60601-2-16:1998 EC 60601-2-39:1999
PROTECTIVELY EARTHED	Connected to the PROTECTIVE EARTH TERMINAL for protective purposes by means complying with the requirements of this standard IEC 60601-1:1988.	NG.06.09	IEC 60601-1/A2:1995 IEC 60601-2-51:2003
PRUDENT-USE STATEMENT	Affirmation of the principle advising avoidance of primarily high EXPOSURE levels and secondarily long EXPOSURE times while acquiring necessary clinical information.		IEC 60601-2-37:2001
PUBLIC MAINS NETWORKS	LOW VOLTAGE electricity power lines to which all categories of consumers have access.		IEC 60601-1-2:2001
PULSE AMPLITUDE ANALYZER PULSE WINDOW	Range of input signal amplitudes for which the analyzer delivers an output signal.	rm-34-23	IEC 60789:1992 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998
PULSE BEAM-WIDTH	Distance between two points, on a specified surface in a specified direction passing through the point of maximum PULSE-PRESSURE-SQUARED INTEGRAL (p_i) in that surface, at which the PULSE-PRESSURE-SQUARED INTEGRAL is the specified fraction of the maximum value in that surface. Symbol: d_{-6} (for PULSE BEAM-WIDTH defined at –6 dB). Unit: centimetres, cm.		IEC 60601-2-37:2001
PULSE DURATION	Time interval beginning at the first time the pressure amplitude exceeds a REFERENCE VALUE and ending at the last time the pressure amplitude returns to that value. The REFERENCE VALUE is equal to the sum of the minimum pressure amplitude and 10 % of the difference between the maximum and minimum pressure amplitude. [IEC 61689, definition 3.35] NOTE The above definition from IEC 61689 differs from that of 3.30 of IEC 61102 to account for incomplete modulation.		IEC 60601-2-5:2000
PULSE DURATION	The duration of the output PULSE WAVEFORM at 50 % of the maximum amplitude.		IEC 60601-2-10 /A1:2001
PULSE DURATION	1,25 times the interval between the time when the time integral of intensity in an acoustic PULSE at a point reaches 10 % and when it reaches 90 % of the PULSE-INTENSITY INTEGRAL. Symbol: t_d. Unit: seconds, s.		IEC 60601-2-37:2001
PULSE DURATION	The duration of the electrical stimulus pulse WAVEFORM at 50 % of the peak amplitude.		IEC 60601-2-40:1998
PULSE REPETITION PERIOD	Absolute value of the time interval after which the same characteristics of a periodic WAVEFORM recur (see 5.3.2.1 of IEC 60469-1). [IEC 61689, definition 3.36]		IEC 60601-2-5:2000
PULSE REPETITION RATE	Inverse of the time interval between two successive acoustic PULSES. Symbol: p_{rr}. Unit: hertz, Hz.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
PULSE-AVERAGE INTENSITY	Ratio of the PULSE-INTENSITY INTEGRAL I_{pi} to the PULSE DURATION t_d. Symbol: I_{pa}. Unit: watts per square centimetre, W cm^{-2}.		IEC 60601-2-37:2001
PULSE-INTENSITY INTEGRAL	Time integral of instantaneous intensity at a particular point in an acoustic field integrated over the acoustic PULSE WAVEFORM. Symbol: I_{pi}. Unit: millijoules per centimetre squared, mJ/cm^2.		IEC 60601-2-37:2001
PULSE-PRESSURE-SQUARED INTEGRAL	Time integral of the square of the instantaneous acoustic pressure at a particular point in an acoustic field integrated over the acoustic PULSE WAVEFORM. Symbol: p_i. Unit: Pascal squared second, Pa^2s.		IEC 60601-2-37:2001
QUALIFIED PERSON	Person recognized by a competent authority as having the requisite knowledge and training to perform specified duties.	rm-85-04	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 62083:2000
QUALIFIED PERSON	Person competent in any relevant discipline by virtue of his training, knowledge and experience to perform required duties.		IEC 60601-2-17 /A1:1996
QUALITY ASSURANCE	Planned and systematic actions necessary to provide adequate confidence by ensuring that a product or service will satisfy given requirements for quality.	rm-70-05	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999
QUALITY ASSURANCE PROGRAMME	Detailed instruction for carrying out actions of QUALITY ASSURANCE for individual items of EQUIPMENT, systems of EQUIPMENT or facilities, including quality administrative elements and quality control techniques.	rm-70-06	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
QUALITY CONTROL	Operational techniques and activities that are used to fulfil requirements for quality.	rm-70-07	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999
QUALITY CONTROL	Part of the QUALITY ASSURANCE in nuclear medicine including tests of instruments with appropriate test methods. NOTE Includes both ACCEPTANCE TESTING and ROUTINE TESTING.		IEC 61948-1:2001

Term	Definition	Reference	Used in IEC
QUALITY EQUIVALENT FILTRATION	Quantitative indication of the FILTRATION effected by one or several layer(s) of reference material(s) which, if substituted in a beam of specified RADIATION QUALITY under NARROW BEAM CONDITION for the material under consideration, give(s) the same RADIATION QUALITY as gives the material under consideration. The QUALITY EQUIVALENT FILTRATION is expressed in suitable submultiples of the metre together with the reference material(s) and the RADIATION QUALITY of the incident beam.	rm-13-45	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994
QUALITY EQUIVALENT FILTRATION	Quantity indicating for a material or an object the effect of its FILTRATION, expressed as the thickness of a particular reference material, whose FILTRATION is found to have the same effect on RADIATION QUALITY under specific conditions of measurement. **Recommended replacement: rm-13-45**		IEC 60580:2000
QUANTITY INDEX	For X-RADIATION, the ratio of the ABSORBED DOSE measured at a depth of 20 cm to that measured at a depth of 10 cm. The detector is at the NORMAL TREATMENT DISTANCE. The measurement is made in a PHANTOM on the RADIATION BEAM AXIS for a RADIATION FIELD of 10 cm x 10 cm.		IEC 60976 /A1:2000
QUANTUM ABSORPTION EFFICIENCY	The number of PHOTONS incident at the input of a RADIATION DETECTOR that yield a signal at the output of the RADIATION DETECTOR divided by the total number of incident PHOTONS.		IEC 61262-5:1994
QUENCH	Transition of the electrical conductivity of a coil that is carrying a current from a superconducting state to normal conductivity, resulting in rapid boil-off of fluid cryogen and decay of the magnetic field.		IEC 60601-2-33:2002
RADIATION SOURCE TO SKIN DISTANCE	In RADIOTHERAPY, distance from the surface of the RADIATION source to the ENTRANCE SURFACE.	rm-37-14	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997
RADIATION SPECTRUM	Distribution of a RADIATION QUANTITY with respect to RADIATION energy. Thus: – X-ray spectrum; – gamma-ray spectrum.	rm-13-34	IEC 60601-2-28:1993 IEC 60627:2001 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994
RADIATION TYPE	Nature of the waves or corpuscles comprising the RADIATION, for example whether the RADIATION is X-RADIATION or ELECTRON RADIATION.	rm-11-23	IEC 60601-2-1/A1:2002 IEC 60976 /A1:2000
RADIAL RESOLUTION	TRANSVERSE RESOLUTION along a line passing through the position of the source and the SYSTEM AXIS.	rm-34-37	IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
RADIATION	Propagation of emitted energy through space or through a material medium in the form of waves or in the form of kinetic energy of particles. NOTE When unqualified, the term RADIATION usually refers – to electromagnetic radiations according to frequency or origin such as: radiofrequency radiation, infra-red radiation, visible radiation (light), ultraviolet radiation, X-radiation, gamma radiation; – to corpuscular radiations according to particles or origin such as: alpha radiation, beta radiation, ELECTRON radiation, NEUTRON radiation.	rm-11-01	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-3:1998 IEC 62083:2000
RADIATION APERTURE	Aperture in the PROTECTIVE SHIELDING of a RADIATION SOURCE or in a beam limiting device, that is intended to give passage to the RADIATION BEAM.	rm-37-26	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
RADIATION BEAM	In RADIOLOGY, spatial region limited in solid angle and containing a flux of IONIZING RADIATION originating from a RADIATION SOURCE that is considered as a POINT SOURCE. Leakage radiation and SCATTERED RADIATION are considered not to form a RADIATION BEAM. Thus: – X-ray beam; – gamma-ray beam; – ELECTRON beam; – NEUTRON beam.	rm-37-05	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-32:1994 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-3:1998 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIATION BEAM AXIS	For a symmetrical RADIATION BEAM, line through the centre of the RADIATION SOURCE and half way between the effective edges of the beam limiting device. Usually, the RADIATION BEAM AXIS coincides within required tolerances with the REFERENCE AXIS of the RADIATION SOURCE. Thus: – X-ray beam axis; – gamma-ray beam axis; – NEUTRON beam axis; – ELECTRON beam axis.	rm-37-06	IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61267:1994
RADIATION CONDITION	Description of RADIATION FIELDS by a set of electrical and geometrical parameters like X-RAY TUBE VOLTAGE, TOTAL FILTRATION and geometrical arrangements. NOTE The term RADIATION CONDITION refers to a description of RADIATION FIELDS and not to a particular set-up for testing of EQUIPMENT.	rm-13-59	IEC 60627:2001 IEC 61267:1994
RADIATION DETECTOR	EQUIPMENT, generally sub-assembly, or substance which, in the presence of radiation, provides by either direct or indirect means a signal or other indication suitable for use in measuring one or more quantities of the incident radiation.	rm-51-01	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
RADIATION DETECTOR	Element which transduces AIR KERMA, AIR KERMA length or AIR KERMA RATE into a measurable electrical signal. It may be either an IONIZATION CHAMBER or a semi-conductor detector: 1) IONIZATION CHAMBER: Ionization detector consisting of a CHAMBER filled with air, in which an electric field insufficient to induce gas multiplication is provided for the collection, at the ELECTRODES, of charges associated with the ions and ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION. The CHAMBER is constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere so that corrections to the RESPONSE for changes in air density need to be made. 2) Vented CHAMBER: An IONIZATION CHAMBER constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere so that corrections to the RESPONSE for changes in air density need to be made. NOTE Sealed CHAMBERS are not suitable, because the necessary wall thickness of a sealed CHAMBER may cause an unacceptable energy dependence of the RESPONSE and because the long term stability of sealed CHAMBERS is not guaranteed. 3) Semi-conductor detector: Either a) and/or b): a) semi-conductor device operating in the shorted junction mode that utilizes the production and motion of excess free charge carriers in the semi-conductor for the detection and measurement of incident IONIZING RADIATION; b) scintillator material optionally coupled to a semi-conductor photodiode operating in the shored junction mode, in which assembly incident IONIZING RADIATION is first converted to light and then to an electrical signal. **Recommended replacement: rm-51-01**		IEC 61674 /A1:2002
RADIATION DETECTOR	For this standard IEC 60601-2-9:1996 this is defined as the electrically operated element which directly transduces ABSORBED DOSE, ABSORBED DOSE RATE or any other dose related quantity into a measurable electrical signal. **Recommended replacement: rm-51-01**		IEC 60601-2-9:1996
RADIATION DETECTOR ASSEMBLY	In a RADIONUCLIDE imaging device, assembly with one or more RADIATION DETECTORS the electrical output signals of which are used to form a RADIOLOGICAL IMAGE .	rm-34-11	IEC 60601-2-9:1996 IEC 60789:1992 IEC 61675-3:1998
RADIATION ENERGY	In RADIOLOGY, quantity indicating the energy that a PHOTON or other particle is carrying, except its rest energy. The unit of RADIATION ENERGY is the ELECTRONvolt (eV), 1 eV being equal to 1,60219 x 10^{-19} J. Thus: – X-ray energy; – gamma ray energy.	rm-13-29	IEC 60613:1989 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
RADIATION FIELD	Area on a surface intersected by a RADIATION BEAM within which the radiation intensity exceeds a specific or specified level. Thus: – X-ray field; – gamma-ray field; – ELECTRON field; – NEUTRON field.	rm-37-07	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 62083:2000
RADIATION HEAD	Structure from which the RADIATION BEAM emerges.	rm-20-06	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61217:2002

Term	Definition	Reference	Used in IEC
RADIATION METER	In RADIOLOGY, assembly designed to measure quantities concerned with IONIZING RADIATION (ACTIVITY, EXPOSURE RATE, etc.), and including one or several RADIATION DETECTORS and associated sub-assemblies or basic function units. Thus: – kermameter; – KERMA ratemeter; – area KERMA product meter; – EXPOSURE METER; – EXPOSURE ratemeter; – area EXPOSURE product meter.	rm-50-01	IEC 60601-2-9:1996 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
RADIATION OUTPUT	AIR KERMA per CURRENT TIME PRODUCT (mGy/mAs) at a given distance from the FOCAL SPOT in the primary X-ray beam.	rm-13-57	IEC 61223-3-1:1999 IEC 61223-3-4:2000
RADIATION PROTECTION	Limitation to an acceptable level of: – radiation hazard; – damage to material attributable to radiation.	rm-60-02	IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 61331-2:1994
RADIATION QUALITY	Characteristic of IONIZING RADIATION determined by the spectral distribution of a RADIATION QUANTITY with respect to RADIATION ENERGY. NOTE For various purposes concerning X-RADIATION, practical approximations of RADIATION QUALITY are expressed in terms of variables such as: a) HIGH VOLTAGE with PERCENTAGE RIPPLE and TOTAL FILTRATION; b) first HALF-VALUE LAYER for specified HIGH VOLTAGE with its PERCENTAGE RIPPLE; c) first HALF-VALUE LAYER and TOTAL FILTRATION; d) the first HALF-VALUE LAYER and the quotient of the first HALF-VALUE LAYER by the second HALF-VALUE LAYER; e) equivalent energy.	rm-13-28	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61331-1:1994 IEC 61331-2:1994 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIATION QUALITY	RADIATION CONDITION whereby the RADIATION FIELD only comprises an insignificant amount of SCATTERED RADIATION. NOTE This definition takes preference over that given in IEC 60788.		IEC 60627:2001 IEC 61267:1994
RADIATION QUALITY	For a specific type of radiation, the description of any characteristic that depends on its energy spectrum. NOTE For the purposes of this international standard, a practical approximation of RADIATION QUALITY is expressed as the quotient of the first HALF-VALUE LAYER and the second HALF-VALUE LAYER. **Recommended replacement: rm-13-28**		IEC 60580:2000
RADIATION QUANTITIES AND UNITS	This collateral standard IEC 60601-1-3:1994 uses the quantity AIR KERMA in preference to EXPOSURE. The unit of AIR KERMA is the gray (Gy). An AIR KERMA of 1 Gy corresponds to an EXPOSURE of 2,97 x 10^{-2} C kg^{-1}.		IEC 60601-1-3:1994
RADIATION QUANTITY	Letter symbol: Φ. At a given point of space, the number dN of particles incident during a given time interval on a suitably small sphere centred at that point divided by the cross-sectional area da of the sphere. $\Phi = \frac{dN}{da}$	rm-13-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61331-1:1994
RADIATION QUANTITY FOR NOMINAL SHORTEST IRRADIATION TIME	The definition of NOMINAL SHORTEST IRRADIATION TIME refers to a required constancy of a RADIATION QUANTITY. In this standard the RADIATION QUANTITY concerned is AIR KERMA.	rm-13-58	IEC 60601-2-7:1998 IEC 60601-2-45:2001
RADIATION SOURCE	RADIOACTIVE SOURCE or part of EQUIPMENT capable of emitting IONIZING RADIATION.	rm-20-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-3:1998 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIATION SOURCE ASSEMBLY	Assembly of components comprising: – the RADIATION SOURCE, – the means providing protection against IONIZING RADIATION and, where applicable, against electric shock, – the BEAM LIMITING SYSTEM. Thus: – X-ray source assembly; – gamma-ray source assembly; – RADIONUCLIDE source assembly.	rm-20-05	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994
RADIO FREQUENCY (RF)	Frequency in the portion of the electromagnetic spectrum that is between the audio-frequency portion and the infrared portion; frequency useful for radio transmission. NOTE The limits are generally accepted to be 9 kHz to 3 000 GHz.		IEC 60601-1-2:2001
RADIOACTIVE HALF-LIFE	Letter symbol: *T*. For a single radioactive decay process, the time required for the ACTIVITY to decrease to half its value. NOTE For a RADIONUCLIDE, the RADIOACTIVE HALF-LIFE *T* is related to the decay constant λ by the expression: $T = \frac{L_n 2}{\lambda} = \frac{0{,}693}{\lambda}$	rm-13-20	IEC 61675-1:1998 IEC 62083:2000
RADIOACTIVE IMPURITY	RADIONUCLIDES in a RADIOACTIVE SOURCE other than the principal RADIONUCLIDE.		IEC 61303:1994
RADIOACTIVE SOURCE	Quantity of radioactive material having both an ACTIVITY and a specific ACTIVITY above specific levels.	rm-20-02	IEC 60601-2-17/A1:1996 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 62083:2000
RADIOACTIVE SOURCE TRAIN	A sequence of SEALED RADIOACTIVE SOURCES, possibly separated by non-radioactive spacers, either permanently combined or selected prior to each IRRADIATION, and used in AFTERLOADING EQUIPMENT. The RADIOACTIVE SOURCE TRAIN is usually selected to give a specified dose distribution.		IEC 60601-2-17/A1:1996

Term	Definition	Reference	Used in IEC
RADIOACTIVE STANDARD SOURCE	General term used to refer to the standard sources listed below.		IEC 61303:1994
RADIOACTIVITY	Property of certain nuclides of spontaneously emitting particles or gamma radiation, or of emitting X-RADIATION following orbital ELECTRON capture or of undergoing spontaneous fission.	rm-12-13	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 61303:1994
RADIOGRAM	In RADIOLOGY, RECORD of an X-RAY PATTERN.	rm-32-02	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIOGRAPHIC CASSETTE	Light-tight receptacle with a radiation-transparent front cover, intended to house one or more stationary RADIOGRAPHIC FILMS, usually with one or more INTENSIFYING SCREENS.	rm-35-14	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994
RADIOGRAPHIC CASSETTE HOLDER	**Recommendation: Do not use as defined term** Reason: Self-explaining, in none of the 4 standards applying the term is a definition missed by the reader.	rm-35-18	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 61217:2002 IEC 61223-2-10:1999

Term	Definition	Reference	Used in IEC
RADIOGRAPHIC FILM	Sheet or roll material consisting of a transparent carrier covered with radiation-sensitive emulsion on one or usually both sides and designed for use in DIRECT RADIOGRAPHY.	rm-32-32	IEC 60336:1993 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994
RADIOGRAPHIC RATING	For the operation of an X-RAY TUBE, specified combination of conditions and LOADING FACTORS, under which the specified limits of loadability of the X-RAY TUBE are attained.	rm-36-36	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-45:2001 IEC 60613:1989
RADIOGRAPHY	Technique for obtaining, recording, and optionally processing directly or after TRANSFER, information contained in an X-RAY PATTERN at an IMAGE RECEPTION AREA.	rm-41-06	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000

Term	Definition	Reference	Used in IEC
RADIOLOGICAL	Referring to IONIZING RADIATION, its generation and application for scientific, medical and technical purposes.	rm-40-02	IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 61223-2-10:1999 IEC 61331-3:1998
RADIOLOGICAL EQUIPMENT	EQUIPMENT designed for use in RADIOLOGY.	rm-20-19	IEC 61331-2:1994
RADIOLOGICAL INSTALLATION	Installed RADIOLOGICAL EQUIPMENT including all means for its intended operation. Thus: – gamma-ray installation; – X-ray installation (IEC 60613:1989) (IEC 61223-1:1993).	rm-20-24	IEC 60613:1989 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61331-2:1994
RADIOLOGICAL IMAGE	Information obtained by using IONIZING RADIATION presented as an image suitable for medical diagnosis.	rm-32-05	IEC 61223-2-1:1993 IEC 61675-3:1998
RADIOLOGICAL PROTECTION	RADIATION PROTECTION with respect to IONIZING RADIATION.	rm-60-03	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001
RADIOLOGY	Science of IONIZING RADIATION and its application.	rm-40-01	IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61267:1994
RADIOMETRIC PARAMETERS	NOTE See IEC 60050(845).		IEC 60601-2-50:2000

Term	Definition	Reference	Used in IEC
RADIONUCLIDE	Radioactive nuclide.	rm-11-22	IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-1:2001 IEC 61948-2:2001 IEC 62083:2000
RADIONUCLIDE BEAM THERAPY EQUIPMENT	Thus: – gamma beam therapy EQUIPMENT.	rm-24-01	IEC 60601-2-11:1997 IEC 61217:2002 IEC 62083:2000
RADIONUCLIDE CALIBRATOR	Device for measuring the ACTIVITY of a radioactive sample.		IEC 61303:1994
RADIONUCLIDE FACTOR	Factor, dependent on the RADIONUCLIDE, by which the RESPONSE of the system must be multiplied in order to obtain the correct ACTIVITY reading of a source which has been placed in the IONIZATION CHAMBER.		IEC 61303:1994
RADIOSCOPIC SCREEN	FLUORESCENT SCREEN used for DIRECT RADIOSCOPY.	rm-32-31	IEC 60601-1-3:1994
RADIOSCOPICALLY GUIDED INVASIVE PROCEDURE	Invasive procedure (involving the introduction of a device, such as a needle or a catheter into the body of the PATIENT) using radioscopic imaging as the principal means of guidance.		IEC 60601-2-43:2000
RADIOSCOPICALLY GUIDED INTERVENTIONAL PROCEDURE	RADIOSCOPICALLY GUIDED INVASIVE PROCEDURES intended to effect TREATMENT on the medical condition of the PATIENT.	rm-31-12	IEC 60601-2-43:2000
RADIOSCOPY	Technique for obtaining continuously or periodically a sequence of X-RAY PATTERNS and presenting them simultaneously and continuously as visible images.	rm-41-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000

Term	Definition	Reference	Used in IEC
RADIOTHERAPY	Medical therapy essentially consisting of one or more TREATMENTS by IONIZING RADIATION.	rm-40-05	IEC 60522:1999 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 62083:2000
RADIOTHERAPY SIMULATOR	An EQUIPMENT which uses X-RAY EQUIPMENT to simulate physically a therapeutic RADIATION BEAM so that the TREATMENT VOLUME to be irradiated during RADIOTHERAPY can be localized and the size of the therapeutic RADIATION FIELD can be confirmed. **Recommended replacement: IEC 60601-2-29**		IEC 61217:2002
RADIOTHERAPY SIMULATOR	EQUIPMENT that uses X-RAY EQUIPMENT to simulate geometrically parameters of movements and RADIATION FIELDS of RADIOTHERAPY equipment so as to assist with the planning of PATIENT TREATMENTS.		IEC 60601-2-29:1999
RADIOTHERAPY TREATMENT PLANNING SYSTEM (RTPS)	A device, usually a PROGRAMMABLE ELECTRONIC SYSTEM including its associated peripherals, that is used to simulate the application of radiation to a PATIENT for a proposed RADIOTHERAPY TREATMENT. It usually, but not necessarily, provides estimations of ABSORBED DOSE distribution in human tissue using a particular algorithm or algorithms. These algorithms provide simulations of radiation that is typically from, but not necessarily limited to, medical ELECTRON accelerators, gamma beam therapy EQUIPMENT or RADIOACTIVE SOURCES when brachytherapy is planned.		IEC 62083:2000
RADIUS OF ROTATION	Distance between the SYSTEM AXIS and the COLLIMATOR FRONT FACE.	rm-34-38	IEC 61675-2:1998 IEC 61948-2:2001
RANDOM COINCIDENCE	Result of COINCIDENCE DETECTION in which both participating PHOTONS emerge from different positron annihilations.		IEC 61675-1:1998
RANDOM UNCERTAINTY	Observed standard deviation of a set of repeated MEASURED VALUES.		IEC 61303:1994
RATED (value)	Value assigned by the MANUFACTURER to a quantity characteristic of the EQUIPMENT.	NG.12.08	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
RATED FIELD SIZE	Size of the USEFUL BEAM at the IONIZATION CHAMBER within which the IONIZATION CHAMBER performs to its specification.		IEC 60580:2000
RATED LENGTH	Length along the axis of the CT DETECTOR within which the detector performs to its specification.		IEC 61674 /A1:2002
RATED LOAD	The value of non-reactive load resistance that results in the maximum HFOUTPUT POWER from each operating mode of the HF SURGICAL EQUIPMENT.		IEC 60601-2-2:1998

Term	Definition	Reference	Used in IEC
RATED OUTPUT POWER	The power in watts produced when the HF output is fed into the RATED LOAD.		IEC 60601-2-2:1998
RATED OUTPUT POWER	Maximum radio-frequency power assigned by the MANUFACTURER, averaged over a period of 1 s, which can be delivered to the load specified in Clause 50.		IEC 60601-2-3 /A1:1998
RATED OUTPUT POWER	Maximum OUTPUT POWER of the EQUIPMENT at any RATED MAINS VOLTAGE. [IEC 61689, definition 3.32]		IEC 60601-2-5:2000
RATED OUTPUT POWER	Value of the maximum high-frequency power averaged over at least 1 s which can be fed into a MATCHED LOAD.		IEC 60601-2-6:1984
RATED RANGE (of use)	Range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. NOTE The EFFECTIVE RANGE of use is referred to as RATED RANGE in this standard.		IEC 60580:2000
RATED RANGE (of use)	Range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. NOTE Referred to as RATED RANGE in this standard IEC 60731/A1:2002.		IEC 60731/A1:2002 IEC 61674/A1:2002
RATED RANGE (of use)	The range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. The minimum RATED RANGE is the least range of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument shall operate within the specified LIMITS OF VARIATION in order to comply with this standard IEC 61676:2002 **Recommended replacement: IEC 61674, IEC 60731**		IEC 61676:2002
READY STATE	State of EQUIPMENT in which all conditions, such as carrying out of confirming operations and any other satisfaction of INTERLOCKS are prevailing so that the intended operation of such EQUIPMENT can be initiated by a single action.	rm-84-05	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000
RECONSTRUCTIVE TOMOGRAPHY	TOMOGRAPHY in which information obtained from the object is recorded for constructing images of layers in the object by processing.	rm-41-19	IEC 60336:1993 IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-2-1:1993
RECORD	Document which furnishes objective evidence of activities performed or results achieved. [ISO 8402:1994, definition 3.15]		ISO 14971:2000
RECORDING ELECTROCARDIOGRAPH	MEDICAL ELECTRICAL EQUIPMENT intended for the production of ECG RECORDS.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
RECOVERY COEFFICIENT	Measured (image) ACTIVITY concentration of an active volume divided by the true ACTIVITY concentration of that volume, neglecting ACTIVITY CALIBRATION FACTORS. NOTE For the actual measurement, the true ACTIVITY concentration is replaced by the measured ACTIVITY concentration in a large volume.		IEC 61675-1:1998
REDUNDANT (timer) COMBINATION	Combination of two CONTROLLING TIMERS in which both are arranged to terminate IRRADIATION at the pre-selected time.	rm-33-13	IEC 60601-2-8:1999 IEC 60601-2-11:1997
REDUNDANT DOSE MONITORING SYSTEMS	Utilization of two DOSE MONITORING SYSTEMS where both systems are arranged to terminate IRRADIATION according to the pre-selected number of dose monitoring units.	rm-33-14	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
REDUNDANT DOSE MONITORING COMBINATION	Combination of two DOSE MONITORING SYSTEMS in which both systems are arranged to terminate IRRADIATION according to the preselected number of DOSE MONITOR UNITS. **Recommended replacement: REDUNDANT DOSE MONITORING COMBINATION**		IEC 60976/ A1:2000
REFERENCE AIR KERMA	AIR KERMA of the primary X-ray beam measured under specific conditions and expressed as an equivalent value at the interventional reference point. REFERENCE AIR KERMA RATE, AIR KERMA RATE expressed as above. REFERENCE AIR KERMA (rate), used for brevity where either REFERENCE AIR KERMA or REFERENCE AIR KERMA RATE apply, according to the context.		IEC 60601-2-43:2000
REFERENCE AXIS	For a RADIATION SOURCE, line in the REFERENCE DIRECTION through the centre of the RADIATION SOURCE.	rm-37-03	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60806:1984 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
REFERENCE CONDITIONS	Conditions under which all INFLUENCE QUANTITIES and INSTRUMENT PARAMETERS have their REFERENCE VALUES.	rm-70-12	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002 IEC 61676:2002
REFERENCE DATA	A set of data measured immediately after ACCEPTANCE TESTING, using test methods designed for ROUTINE TESTING.		IEC 61948-1:2001 IEC 61948-2:2001

Term	Definition	Reference	Used in IEC
REFERENCE DIRECTION	For a RADIATION SOURCE, specified direction to which characteristics such as TARGET ANGLE, RADIATION FIELD, and specifications with respect to the imaging quality of the RADIATION SOURCE, are referenced.		IEC 60336:1993 IEC 60806:1984 IEC 61223-2-11:1999 IEC 61267:1994
REFERENCE INDICATED VALUE	The INDICATED VALUE at which the CALIBRATION FACTOR of an instrument is determined.		IEC 60731/A1:2002
REFERENCE PLANE	In diagnostic X-RAY EQUIPMENT for an EFFECTIVE FOCAL SPOT, plane perpendicular to the REFERENCE DIRECTION containing the point at which the REFERENCE AXIS intersects with the ACTUAL FOCAL SPOT. By convention, the point of intersection forms the centre of the EFFECTIVE FOCAL SPOT.	rm-37-04	IEC 60336:1993 IEC 60601-2-44:2002
REFERENCE POINT ACCORDING TO GOLDBERGER	Reference point at an average potential of two limbs (e.g. average of L and F).		IEC 60601-2-51:2003
REFERENCE POINT (of a CHAMBER)	Point of an IONIZATION CHAMBER, which during the calibration of the CHAMBER, is brought to coincidence with the point at which the CONVENTIONAL TRUE VALUE is specified.		IEC 60731/A1:2002 IEC 61267:1994
REFERENCE POINT (of a RADIATION DETECTOR)	Point of a RADIATION DETECTOR which, during the calibration of the detector, is brought to coincidence with the point at which the CONVENTIONAL TRUE VALUE is specified.		IEC 61674/A1:2002
REFERENCE SCALE READING	The SCALE READING corresponding to the REFERENCE INDICATED VALUE		IEC 60731/A1:2002
REFERENCE VALUE	Particular value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) chosen for the purpose of reference, i.e. the value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) at which the CORRECTION FACTOR for dependence on that INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) is unity.	rm-72-06	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
REFERENCE VALUE	Particular value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) chosen for the purposes of reference i.e. the value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) at which the CORRECTION FACTOR for dependence on that INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) is unity. **Recommended replacement: rm-72-06**		IEC 61676:2002
REFERENCE VOLUME	Volume throughout which the RADIONUCLIDE of a RADIOACTIVE STANDARD SOURCE is distributed.		IEC 61303:1994
REFERENCE-CLASS DOSIMETER	DOSIMETER whose performance and stability are sufficient for it to be used to calibrate other DOSIMETERS.		IEC 60731/A1:2002
REGION OF CONTROL	That part of the EQUIPMENT within which flow regulation, flow shut-off or air detection occurs, within the body of the EQUIPMENT or remotely.		IEC 60601-2-24:1998
REGION OF INTEREST (ROI)	Localized part of an image, which is of particular interest at a given time.	rm-32-63	IEC 61223-2-6:1994 IEC 61223-3-1:1999
REINFORCED INSULATION	Single insulation system applied to LIVE parts which provides a degree of protection against electric shock equivalent to DOUBLE INSULATION under the conditions specified in this standard IEC 60601-1:1995.	NG.03.07	IEC 60601-1/A2:1995 IEC 60601-2-51:2003
RELATIVE INTRINSIC ERROR	Ratio of the INTRINSIC ERROR to the CONVENTIONAL TRUE VALUE.	rm-73-18	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
RELATIVE INTRINSIC ERROR	The ratio of the INTRINSIC ERROR to the CONVENTIONAL TRUE VALUE.		IEC 61676:2002

Term	Definition	Reference	Used in IEC
RELATIVE SURFACE DOSE	Ratio of the ABSORBED DOSE on the RADIATION BEAM AXIS at the depth of 0,5 mm to the maximum ABSORBED DOSE on the RADIATION BEAM AXIS, both measured in a PHANTOM with its surface at a specified distance.	rm-13-60	IEC 60601-2-11:1997 IEC 60976 /A1:2000
RELATIVE SURFACE DOSE	Ratio of the ABSORBED DOSE on the REFERENCE AXIS, at the depth of 0,5 mm, to the maximum ABSORBED DOSE on the REFERENCE AXIS, both measured in a PHANTOM with its surface at a specified distance. **Recommended replacement IEC 60601-2-11:1997, IEC 60976**		IEC 60601-2-1/A1:2002
RESERVE ELECTRICAL POWER SOURCE	Part of the MEDICAL ELECTRICAL EQUIPMENT that temporarily supplies power to the electrical system in the event of an interruption of the primary electrical supply.		IEC 60601-2-13:2003
RESIDUAL RADIATION	In MEDICAL RADIOLOGY, that part of the RADIATION BEAM which remains after having passed the plane of the IMAGE RECEPTION AREA and any relevant radiation measuring device, or, in RADIOTHERAPY, which emerges from the part of the body being intentionally irradiated.	rm-11-14	IEC 60601-1-3:1994 IEC 60601-2-29:1999
RESIDUAL RISK	RISK identified by hazard analysis which remains after RISK MANAGEMENT has been completed. **Recommended replacement: ISO/IEC Guide 51,1999, definition 3.9**		IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
RESIDUAL RISK	RISK remaining after protective measures have been taken. [ISO/IEC Guide 51:1999, definition 3.9]		ISO 14971:2000
RESOLUTION OF THE DISPLAY	Smallest change of SCALE READING to which a numerical value can be assigned without further interpolation: for an analogue display, the resolution is the smallest fraction of a scale interval that can be determined by an observer under specified conditions; for a digital display, the resolution is the smallest significant increment of the reading.	rm-32-64	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002
RESOLVING TIME	Smallest time interval which must elapse between the occurrence of two consecutive input signals to a device in order that it be capable of fulfilling its function for each of them separately.	rm-34-22	IEC 60789:1992 IEC 61675-1:1998
RESPIRATORY PRESSURE	PRESSURE at the PATIENT CONNECTION PORT.		IEC 60601-2-12:2001
RESPONSE	The quotient of the INDICATED VALUE divided by the CONVENTIONAL TRUE VALUE.		IEC 61676:2002
RESPONSE	For a CHAMBER ASSEMBLY with an associated MEASURING ASSEMBLY, it is the quotient of the INDICATED VALUE divided by the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the IONIZATION CHAMBER. For a MEASURING ASSEMBLY on its own it is the quotient of the INDICATED VALUE divided by the input charge or current. For an IONIZATION CHAMBER on its own it is the quotient of the ionization charge or current divided by the CONVENTIONAL TRUE VALUE. **Recommended replacement: IEC 60580:2000**		IEC 60601-2-9:1996 IEC 60731/A1:2002
RESPONSE	Quotient of the INDICATED VALUE by the CONVENTIONAL TRUE VALUE. **Recommended replacement: IEC 60580:2000**		IEC 60580:2000 IEC 61674 /A1:2002
RESPONSE time	The time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value, after a sudden change in the quantity being measured.	rm-13-60	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002
RESPONSE TIME	Time required to display a 10 % to 90 % RESPONSE to a change of partial pressure as measured in Clause 7. NOTE Different gases may have different RESPONSE TIME.		IEC 60601-3-1:1996